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ALESSANDRO GIURIZATTO MELANDA

**ANÁLISE TRIDIMENSIONAL DA MARCHA DE CRIANÇAS
COM PARALISIA CEREBRAL:
EFETIVIDADE DO USO DE ÓRTESES SUROPODÁLICAS,
CONFIABILIDADE E VALIDADE DE CLASSIFICAÇÕES
PREEXISTENTES E CRIAÇÃO E AVALIAÇÃO DE
PROPRIEDADES PSICOMÉTRICAS DE UMA NOVA
CLASSIFICAÇÃO DA MARCHA.**

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Tese apresentada à Universidade Estadual de Londrina, como requisito parcial para obtenção do título de Doutor em Ciências da Reabilitação (Programa Associado entre a Universidade Estadual de Londrina [UEL] e Universidade Pitágoras - UNOPAR.

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MELANDA, Alessandro Giurizatto. **Análise tridimensional da marcha de crianças com paralisia cerebral:** efetividade do uso de órteses suropodálicas, confiabilidade e validade de classificações preexistentes e criação e avaliação de propriedades psicométricas de uma nova classificação da marcha. 2020. 255 f. Tese (Doutorado em Ciências da Reabilitação) – Universidade Estadual de Londrina, Londrina, 2020.

RESUMO

Introdução: Paralisia Cerebral (PC) é a causa mais comum de distúrbio físico na infância. As crianças com PC, como efeito da lesão neurológica, comumente apresentam fraqueza, espasticidade, falta de coordenação muscular e controle postural inadequado, que juntos dificultam a mobilidade e limitam as atividades físicas. Entretanto, mais da metade das crianças identificadas com PC andam de forma independente. A avaliação criteriosa dos indivíduos auxilia na indicação, frequência, tempo ou momento no processo de tratamento que cada modalidade deve ser utilizada. A análise tridimensional da marcha (A3DM) é considerada o padrão-ouro na avaliação do andar de indivíduos com PC e foi utilizada nesta tese como principal instrumento de medida. **Objetivos:** avaliar a efetividade do uso de órteses suropodálicas (OSP) em crianças com PC, identificar a aplicabilidade de classificações preexistentes da marcha em crianças com PC espástica e construir uma nova classificação da marcha para crianças com PC para suprir deficiências das classificações atuais. **Métodos:** Quatro estudos originais retrospectivos foram desenvolvidos e contaram com a utilização do banco de dados do Laboratório de Marcha do Centro Hospitalar de Reabilitação de Curitiba – Paraná, coletados entre os anos de 2010 e 2017. O primeiro (1) estudo avaliou 24 crianças com PC espástica que foram submetidas a A3DM com e sem OSP. Foram utilizados para análise o “*Gait Profile Score*” (GPS) e dados de tempo e espaço da marcha das crianças com e sem as órteses. O segundo (2) estudo determinou utilidade da classificação publicada por Papageorgiou et al., em 2019, em avaliar uma amostra de 130 crianças com PC espástica. Também foi determinada a reprodutibilidade inter e intraobservador da referida classificação. O terceiro (3) estudo determinou a utilidade clínica e a reprodutibilidade inter e intraobservadores a partir da classificação da marcha proposta e publicada por Davids e Bagley, em 2014, em uma amostra de 131 crianças. O quarto (4) estudo propôs uma nova classificação baseada em níveis de comprometimento para a marcha de crianças com PC espástica. Foram utilizados dados da A3DM de 101 crianças para construção desta classificação. De forma inovadora, também foi considerado o uso de equipamentos auxiliares da marcha (bengalas, muletas e andadores) nesta construção. Foi determinada a reprodutibilidade inter e intraobservadores, assim como a reprodutibilidade dos observadores com o resultado do consenso da avaliação dos autores e a reprodutibilidade entre os diferentes profissionais (fisioterapeutas e cirurgiões ortopédicos). **Resultados:** O estudo (1) mostrou que o índice GPS, dos lados direito e esquerdo, não apresentaram variações estatisticamente significantes ao comparar os mesmos indivíduos deambulando com e sem órteses. Foi observado aumento das variáveis espaço-temporais (velocidade da marcha, comprimento do passo e da passada), quando os participantes estavam em uso de órtese. O estudo (2) mostrou que todos os grupos da classificação foram representados na amostra avaliada, com 95,4% dos participantes classificados. A classificação mostrou sobreposição das

características cinemáticas entre os grupos. A reprodutibilidade foi quase perfeita interobservador, com reprodutibilidade intraobservador substancial e moderada para os avaliadores um e dois, respectivamente. O terceiro estudo (3) determinou que a classificação de Davids e Bagley apresenta utilidade clínica com reprodutibilidade interobservadores e intraobservadores, moderada e moderada a substancial, respectivamente. No quarto estudo (4) foi construída uma classificação de níveis da marcha de crianças com PC, após avaliação do padrão de uma amostra de 101 participantes. A classificação proposta mostrou validade de face, critério e concorrente. A reprodutibilidade interobservadores foi substancial, tanto utilizando dados da A3DM, quanto utilizando apenas a análise observacional da marcha (AOM), por meio de vídeo bidimensional. A reprodutibilidade intraobservador foi substancial ou quase perfeita, a partir dos dados da A3DM ou somente AOM. A reprodutibilidade entre os observadores e o consenso da classificação realizado pelos autores foi substancial ou quase perfeita, assim como a reprodutibilidade entre os tipos de profissionais avaliadores mencionados. **Conclusões:** os quatro estudos científicos utilizaram a A3DM na avaliação de crianças com PC espástica e adicionaram informações relevantes na avaliação da marcha desta população. A presente tese mostrou por meio do primeiro estudo (1) que OSP prescritas por profissional sem utilização da A3DM não produzem alterações significativas no padrão global da marcha (GPS), apesar de apresentarem benefícios funcionais (parâmetros de tempo e espaço). A classificação da marcha dessa população, auxilia na comunicação e no planejamento de tratamentos. O segundo (2) e terceiro (3) estudos determinaram que as classificações estudadas são instrumentos capazes de classificar a marcha de crianças com PC, apesar de limitações terem sido observadas em ambas. O quarto estudo (4) construiu uma nova classificação que objetiva agregar benefícios às classificações existentes com validade e excelente reprodutibilidade em classificar crianças com PC.

Palavras-chave: Paralisia cerebral. Criança. Marcha. Análise da marcha. Classificações em saúde. Órteses.

MELANDA, Alessandro Giurizatto. **Three-dimensional gait analysis of children with cerebral palsy**: effectiveness of the use of ankle foot orthoses, reliability and validity of pre-existing classifications as well as the creation and assessment of psychometric properties of a new classification of gait. 2020. 255 p. Tese (Doutorado em Ciências da Reabilitação) – Universidade Estadual de Londrina, Londrina, 2020.

ABSTRACT

Introduction: Cerebral Palsy (CP) is the most common cause of physical disorders in childhood. Children with CP, as an effect of neurological injury, commonly present weakness, spasticity, lack of muscle coordination and inadequate postural control, which together hinder mobility and limit physical activities. However, more than half of the children identified with CP walk independently. The careful assessment of individuals helps in indicating, frequency, time or moment in the treatment process that each modality should be used. Three-dimensional gait analysis (3DGA) is considered the gold standard in assessing the gait of individuals with CP and was used in this thesis as a measuring instrument. **Aims:** to evaluate the effectiveness of the use of ankle foot orthoses (AFO) in children with CP, to identify the applicability of pre-existing gait classifications in children with spastic CP and to construct a new classification of gait for children with CP to supply deficiencies of the current classifications. **Methods:** Four original retrospective studies were developed and used the database of the Gait Analysis Laboratory of the Hospital Rehabilitation Center of Curitiba - Paraná, between the years 2010 and 2017. The first (1) study evaluated 24 children with spastic CP who underwent 3DGA with and without AFO. The Gait Profile Score (GPS) and spatio-temporal gait parameters of children with and without orthoses were used for analysis. The second (2) study determined the utility of the classification published by Papageorgiou et al., In 2019, in evaluating a sample of 130 children with spastic CP. The inter and intraobserver reliability of that classification was also determined. The third (3) study determined the clinical utility and inter and intrarater reliability from the classification of gait proposed and published by Davids and Bagley, in 2014, in a sample of 131 children. The fourth (4) study proposed a classification of impairment levels for the gait of children with spastic CP. 3DGA data from 101 children were used to construct the classification. In an innovative way, the use of walking aids (canes, crutches and walkers) was also considered in this construction. Inter and intrarater reliability was determined, as well as the reliability of the raters with the result of the consensus of the authors' evaluation and the reliability among the different professionals (physiotherapists and orthopedic surgeons). **Results:** The study (1) showed that the GPS index, on the right and left sides, did not show statistically significant variations when comparing the same individuals walking with and without orthoses. An increase in spatiotemporal variables (gait velocity, stride and stride length) was observed when participants were wearing orthoses. The study (2), showed that all the groups of the classification were represented in the evaluated sample, being that 95.4% of the participants were classified. The classification showed an overlap of the kinematic characteristics between the groups. The reliability interrater was almost perfect with intrarater reliability substantial and moderate for the rater one and two, respectively. The study (3) determined that the Davids and Bagley classification present clinical utility with moderate interrater reliability and moderate to substantial intrarater. In the study (4) a classification of gait levels of children with CP was

constructed, after assessing the pattern of a sample of 101 participants. The proposed classification showed face, criterion and concurrent validity. The interrater reliability was substantial both using data from the 3DGA and observational gait analysis (OGA), using 2D video. The intrarater reliability was substantial or almost perfect, using 3DGA data or only OGA. The reliability among the raters and the classification consensus made by the authors was substantial or almost perfect, as well as the reliability between the types of professional evaluators mentioned. **Conclusions:** the four scientific studies used the 3DGA in the evaluation of children with spastic CP and added relevant information to the evaluation of the gait of this population. This thesis showed through the first study (1) that AFO prescribed by a professional without using the 3DGA do not produce significant changes in the global gait pattern (GPS), despite presenting some functional benefits (spatio-temporal gait parameters). Classifying the gait of this population helps in communication and treatment planning. The second (2) and third (3) studies determined that the classifications studied are instruments capable of classifying the gait of children with CP, although limitations have been observed in both. The fourth (4) study constructed a new classification that aims to add benefits to existing classifications with validity and excellent reliability in classifying children with CP

Keywords: Cerebral palsy. Child. Gait. Gait analysis. Health classifications. Orthotic devices.

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LISTA DE ABREVIATURAS E SIGLAS

2D	Two-dimensional (bidimensional)
3DGA	Three-dimensional Gait Analysis
A3DM	Análise tridimensional da marcha
Ab-ad	Abdução - adução
ACM	Análise Computadorizada da Marcha
AD	Andar Descalço
AFO	Ankle-Foot Orthoses
Ant/post	Ântero-posterior
App. Equinus	Apparent equinus
Asym.	Asymmetrical
BF	Barefoot
CDC	Center for Disease Control and Prevention
CI	Confidence Interval
CIF	Classificação Internacional de Função
Cm	Centimeters
Cm/sec	Centimeters per second
CP	Cerebral Palsy
Df/Pf	Dorsiflexion/Plantarflexion
EIAS	Espinha Ilíaca Antero Superior
EMG	Eletromiografia
Ext-flx	Extensão – flexão
EUA	Estados Unidos da América
FMS	Functional Mobility Scale
Fx/Ext	Flexion/Extension
GCS	Gait Classification System
GDCS-CP	Gait Disruption Classification System – Cerebral Palsy
GDI	Gait Deviation Index
GMFCS	Gross Motor Function Classification System
GPS	Gait Profile Score
Genu recurv	Genu recurvatum
GVS	Gait Variable Score
Hyperext	Hyperextension

JAAOS	Journal of American Academy of Orthopaedic Surgeons
K	Kappa statistics
Kg	Kilograms
MCID	Minimal Clinically Important Difference
M	Meters
Neut/Ext/Int	Neutral/External/Internal
Not class.	Not classified
OGA	Observational Gait Analysis
OSP	Órtese Suropodálica
PC	Paralisia Cerebral
Pla-dor	Flexão plantar – flexão dorsal
POS	Pediatric Orthopedic Surgeon
Post-ant	Pósterio-anterior
PT	Physiotherapist
SD	Standard Deviation
Up/Dn	Up/Down
Var-val	Varo – valgo
Without abnorm	Without abnormalities

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1 INTRODUÇÃO

1.1 JUSTIFICATIVA

A Paralisia Cerebral (PC), é uma condição neurológica que afeta o desenvolvimento motor das crianças e persiste por toda a vida¹, constituindo a mais prevalente causa de deficiência física na infância².

A etiologia da PC é diversa e multifatorial, geralmente causada por lesão no cérebro antes, durante ou após o nascimento, até os cinco anos de idade^{3,4}. Em torno de 10% de todos os casos de PC são causados por eventos após o nascimento⁴. Entretanto, o nascimento prematuro é o fator de risco mais importante para o desenvolvimento da PC⁵.

As tendências temporais na prevalência geral da PC são mais notáveis por sua estabilidade, mas um aumento modesto ocorreu nas últimas décadas do século XX. Esse aumento na prevalência pode ser atribuído à sobrevivência de recém nascidos prematuros e de muito baixo peso (< 1000 g), resultante dos cuidados da terapia intensiva neonatal⁶. Winter *et al.* constataram que a prevalência de PC foi de 6,2 por 1.000 nascidos vivos em crianças nascidas com peso entre 1.500 a 2.499 gramas e 59,5 por 1.000 nascidos vivos em crianças nascidas com peso inferior a 1.500 gramas, em comparação com 2 por 1.000 em nascidos com peso 2.500 gramas ou mais⁷.

Segundo Gage *et al.*, as crianças nascidas prematuras, apresentam melhor potencial de reabilitação⁸. Portanto, apesar da prevalência da PC ter permanecido quase estável, número maior de casos pode ser beneficiado com programas de reabilitação.

Os indivíduos com diagnóstico de PC podem deambular de forma independente de acordo com seu nível de comprometimento neurológico. A probabilidade de crianças com PC andar aos 5 anos de idade sem auxílio é de 54% e de 16% com algum dispositivo auxiliar, segundo estudo realizado por Beckung *et al.*⁹. Um importante objetivo no tratamento dessas crianças é a melhora na habilidade motora e de marcha, devido ao impacto na autonomia e na participação social.

O Centro de Controle e Prevenção de Doenças (CDC) dos Estados Unidos da América (EUA) estimou em um milhão de dólares o custo dos cuidados durante a vida de um indivíduo com PC¹⁰. Isso porque a condição requer uma variedade de modalidades de tratamentos, que envolvem serviços e profissionais de reabilitação

(física, psicológica, comportamental, educacional), serviços médicos (pediatria, cirurgia ortopédica, neurocirurgia, psiquiatria), órteses e tutores externos, constituindo uma abordagem multidisciplinar¹¹. A avaliação criteriosa dos indivíduos auxilia na indicação, frequência e momento no processo de tratamento que cada modalidade deve ser utilizada.

Durante a reabilitação das crianças com PC, o uso de órteses é um dos recursos mais utilizados. As órteses suropodálicas (OSP) são dispositivos usados durante o dia por 21,8% das crianças com PC, segundo Sacaze *et al.*¹². As OSP são frequentemente prescritas para corrigir anormalidades na marcha e facilitar o treino de atividades funcionais¹³.

A primeira parte da tese avaliou o impacto global da utilização de órteses na marcha de indivíduos da faixa etária pediátrica com diagnóstico de PC. Para determinar o resultado funcional do uso das órteses utilizou-se a análise tridimensional da marcha (A3DM).

A A3DM é considerada o método padrão-ouro na avaliação do andar em indivíduos com PC^{14,15}. Há um aumento evidente da importância da A3DM nas decisões clínicas, repercutindo em melhores desfechos obtidos em indivíduos que tiveram seu tratamento planejado de acordo com esses resultados, quando comparados àqueles submetidos a tratamentos baseados somente na avaliação clínica^{16,17,18}.

Entretanto, devido ao grande número de informações produzidas pelos laboratórios de movimento com a A3DM, classificações da marcha foram elaboradas para doenças específicas, o que simplifica e norteia a interpretação e, ainda, facilita as decisões clínicas¹⁹. O termo "classificação de marcha" refere-se a um sistema que permite a alocação de padrões de marcha em grupos que podem ser diferenciados uns dos outros com base em um conjunto de variáveis definidas²⁰. Porém, as atuais classificações da marcha para a PC, apresentam limitações, seja na capacidade em apontar os desvios em todos os planos de movimento ou na sua reprodutibilidade²⁰.

Sendo assim, com o objetivo de determinar a aplicabilidade de classificações existentes e produzir alternativas, a segunda parte da tese avaliou a confiabilidade e a validade de duas classificações da marcha para crianças com PC e, finalmente, elaborou e propôs uma nova classificação para essa população.

2 OBJETIVOS

21 OBJETIVO GERAL

- Avaliar as características da marcha de crianças com PC por meio da A3DM, determinar a aplicabilidade de classificações preexistentes e elaborar nova classificação da marcha para essa população.

22 OBJETIVOS ESPECÍFICOS

- Avaliar a efetividade das OSPs na marcha de crianças com diagnóstico de PC bilateral, utilizando os índices “*Gait Profile Score*” (GPS) e “*Gait Variable Score*” (GVS) da A3DM, além de dados de tempo e espaço (artigo 1);
- Classificar a marcha de uma amostra de crianças com PC espástica por meio da classificação proposta por Papageorgiou *et al.*, validar e avaliar a sua reprodutibilidade (artigo 2);
- Validar e determinar a reprodutibilidade da Classificação das Alterações da Marcha em Crianças com PC, proposta por Davids e Bagley (artigo 3);
- Construir uma nova classificação que apresente características de continuidade entre os níveis de comprometimento da marcha de crianças com PC espástica e avaliar as propriedades psicométricas desse instrumento (artigo 4).

3 REVISÃO DE LITERATURA - CONTEXTUALIZAÇÃO

3.1 PARALISIA CEREBRAL

Paralisia cerebral (PC) é um termo genérico utilizado para um grupo de distúrbios de deficiência motora causados por uma lesão não progressiva no cérebro da criança em desenvolvimento durante o período intrauterino ou nos primeiros anos de vida²¹.

3.1.1 Conceitos Gerais

Os primeiros relatos sobre PC são creditados ao cirurgião inglês William Little, realizados em uma série de aulas entre os anos 1843 e 1844, e contidos no artigo para a Sociedade Obstétrica de Londres de 1861²². Dr. Little descreveu a condição como um problema obstétrico decorrente de asfixia neonatal ou lesão mecânica no feto imediatamente antes ou durante o parto. Sigmund Freud no início da sua carreira como neurologista propôs ser a PC infantil um termo “guarda-chuva” para o conceito geral de doenças infantis causadas por eventos ocorridos no período fetal ou após o nascimento²³. O limite usado para a definição de PC pós-neonatal é arbitrário, mas na maioria dos estudos é considerado até cerca de cinco anos⁴.

Rosenbaum e colaboradores, em 2007, definiram PC como “um grupo de distúrbios permanentes do desenvolvimento motor e da postura, causando limitação na atividade, que são atribuídas a distúrbios que ocorrem no desenvolvimento cerebral do feto ou da criança. As distúrbios motoras da PC são frequentemente acompanhadas por distúrbios de sensações, percepções, cognição, comunicação, comportamento, epilepsia e por problemas musculoesqueléticos”¹.

Segundo Blair e Paneth, a PC é determinada por um diagnóstico clínico, pois não há exames laboratoriais, histológicos, genéticos ou qualquer outro que demonstrem a existência ou a ausência da doença^{6,24}.

Apesar do diagnóstico de PC ocorrer principalmente com base no reconhecimento de características clínicas, como atraso nos marcos motores, alterações no tônus muscular e nos reflexos miotendíneos²⁵, a Academia Americana de Neurologia recomenda que, sempre que possível, o diagnóstico clínico de PC seja confirmado por exames de imagem³. A avaliação com neuroimagem apresenta

achados em mais de 80% das crianças com PC, enquanto que em 17% delas, os exames de imagem não detectam anormalidades^{26,27}. Estudos de neuroimagem são normais em até 50% das crianças com PC discinética²⁸.

A PC é a causa mais comum de distúrbio físico em crianças nos países desenvolvidos, com prevalência de aproximadamente 1 em cada 500 nascidos vivos, com 17 milhões de pessoas afetadas em todo o mundo⁵. A prevalência de PC na Turquia foi determinada pelo estudo de Serdaroglu *et al.*²⁹ como sendo de 4.4 por 1000 nascidos vivos com inclusão de PC adquirida pós natal. No Brasil não existem dados consistentes, mas estima-se que a incidência da PC nos países em desenvolvimento alcance valores de 7 por 1.000 nascidos vivos^{30,31}.

O tratamento de indivíduos com PC requer uma abordagem multidisciplinar¹¹, com encargos aos serviços de saúde 10 a 26 vezes maiores em relação a crianças sem PC³²⁻³⁴. Com isso, a PC e suas condições associadas representam um custo econômico significativo para as famílias, o sistema de saúde e a economia em geral, com relação diretamente proporcional entre a gravidade e os gastos da criança com PC³⁵.

3.1.2 Etiologia

Os fatores de risco mais significativos para o desenvolvimento da PC são prematuridade, baixo peso ao nascer, gemelaridade ou nascimentos múltiplos e infecção perinatal. Esses fatores de risco operam de forma independente ou em conjunto³⁶.

O dano cerebral típico da PC relacionada à prematuridade é frequentemente uma combinação de leucomalácia periventricular induzida por citocinas e dano isquêmico provocado por eventos pós-natais, como hemorragia intraventricular e hidrocefalia²⁸.

A prevalência da PC está inversamente associada ao peso ao nascer e à idade gestacional, variando de 90 casos por 1.000 nascido vivos com peso inferior a 1000 gramas e entre 1 e 5 casos por 1.000 para nascidos com peso igual ou superior a 2500 gramas^{2,21,37}. O risco para bebês nascidos antes das 28 semanas de gestação é aproximadamente 50 vezes maior que os nascidos a termo³⁷.

As malformações cerebrais são outro fator etiológico, presente em aproximadamente 10 a 15% das crianças com PC, e requerem avaliação com

neuroimagem para serem detectadas³⁸. É provável, ainda, que mutações genéticas sejam responsáveis por uma proporção substancial de casos de PC, da mesma maneira que são importantes na etiologia de outros distúrbios complexos do desenvolvimento neurológico, como autismo e dificuldades de aprendizado³⁹.

3.1.3 Fisiopatologia da PC

A PC é a causa mais frequente da síndrome do neurônio motor superior na infância, com características positivas, como espasticidade, hiper-reflexia e cocontração muscular, e características negativas, incluindo fraqueza muscular, perda do controle motor seletivo sobre o movimento, além de déficits sensoriais e de equilíbrio²⁸.

As características positivas da síndrome do neurônio motor superior em particular a espasticidade, têm recebido maior atenção dos profissionais de saúde, porque são passíveis de tratamento. Entretanto, as características negativas são as responsáveis pelo prognóstico locomotor^{28,40}. A fraqueza e a perda do controle motor seletivo determinam quando ou se uma criança caminhará, enquanto que os déficits de equilíbrio ditarão a dependência de dispositivos auxiliares para a marcha⁴¹.

Crianças com PC espástica têm músculos menores⁴² e mais fracos do que crianças saudáveis⁴³. A força muscular observada nos membros inferiores de crianças com PC é 43 a 90% menor que os valores dos controles saudáveis⁴⁰. Essas alterações funcionais são decorrentes da diminuição do volume muscular, da área de secção transversal e do comprimento do ventre muscular⁴⁴. As alterações musculares estão presentes no nível estrutural, com fibras musculares de menor diâmetro, sarcômeros alongados, alterações na matriz extracelular e no tecido conjuntivo (menor complacência). O número de células-tronco musculares (células satélites) encontra-se diminuído e com expressão gênica alterada, determinando menor capacidade de regeneração tecidual⁴⁵.

Grahan e Selber enfatizaram que apesar da PC ser, do ponto de vista neurológico, uma doença não progressiva, as alterações musculoesqueléticas podem progredir e levar ao aparecimento de deformidades nos membros e tronco, principalmente durante o crescimento⁴¹.

A lesão cerebral da PC, portanto, interfere com o andar de diversas maneiras. Inicialmente, por meio dos efeitos primários da lesão cerebral, pela perda do controle

seletivo do movimento, distúrbios de equilíbrio, alterações no tônus muscular e espasticidade e, de forma adicional, pela imposição de forças anormais ao esqueleto, produzindo mudanças no crescimento musculoesquelético secundárias à lesão cerebral⁸.

3.1.4 Classificações da PC

A PC é classificada de acordo com o tipo motor, distribuição topográfica do envolvimento dos segmentos corporais e funcionalidade.

A classificação do tipo motor ou anormalidade neuromotora é realizada de acordo com o tipo predominante, visto que muitos casos são mistos (apresentam mais de um tipo motor). Três são os grupos dessa classificação: espásticos, discinéticos (distônicos e coreoatetóticos) e atáxicos^{1,25,46}.

A classificação topográfica do acometimento motor é composta por hemiparesia, diparesia e tetraparesia⁴⁷. Uma abordagem alternativa promissora foi recomendada por Cans e diferencia comprometimento unilateral de bilateral com relação ao envolvimento topográfico motor⁴⁸.

A classificação funcional mais utilizada na PC é realizada pelo Sistema de Classificação da Função Motora Grossa (*Gross Motor Function Classification System – GMFCS*), por ser uma classificação estável e por possibilitar a definição de objetivos para os diferentes tratamentos^{49,50}. O GMFCS consiste em cinco níveis de função motora relacionadas à capacidade de locomoção do indivíduo (Figura 1).

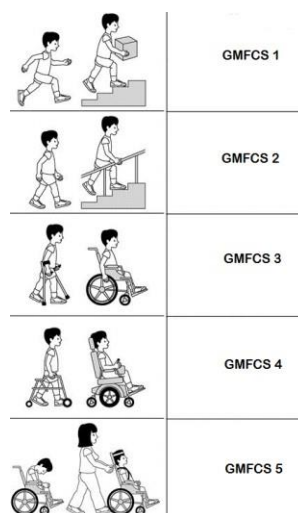


Figura 1. Sistema de Classificação da Função Motora Grossa (GMFCS) da faixa etária de 6 a 12 anos (Palisano *et al.* 1997, Graham, 2005)^{49,51}.

Em 2001, a Organização Mundial de Saúde publicou a Classificação Internacional de Funcionalidade, Incapacidade e Saúde (CIF)⁵², que descreve as disfunções em três níveis: 1) distúrbios da estrutura corporal (órgãos ou membros) ou funções (fisiológica ou psicológica), 2) limitações em atividades (execução de tarefas ou ações individuais) e 3) restrição na participação em situações da vida diária^{53,54}. Apesar da recente publicação de um instrumento com aspectos essenciais da CIF aplicáveis a crianças e jovens com PC, a classificação continua com pouca utilização na prática clínica⁵⁵.

Na mesma linha e com objetivo de caracterizar a mobilidade individual em várias distâncias, Graham *et al.* elaboraram a Escala de Mobilidade Funcional (*Functional Mobility Scale – FMS*). Nesta classificação, a capacidade habitual de andar da criança é graduada em três distâncias (5, 50 e 500 m), de acordo com a necessidade de dispositivos auxiliares, como bengalas, muletas, andadores ou cadeira de rodas⁵⁶.

3.1.5 Prognóstico motor e sobrevida nas crianças com PC

O andar é um dos principais focos da reabilitação na PC, consumindo demasiada quantidade de tempo e recursos para as crianças e seus pais ao longo de muitos anos, com envolvimento de soma significativa das finanças públicas. Apesar desses esforços, está bem estabelecido que muitas crianças com PC não adquirem ou não mantêm a marcha funcional. Dessa forma, é importante buscar parâmetros

que estabeleçam o prognóstico de deambulação de forma a não submeter os indivíduos sem capacidade neurológica a tratamentos extenuantes que não atinjam objetivos realísticos.

Alguns parâmetros clínicos são citados na literatura como marcadores prognósticos para aquisição da deambulação em crianças com PC. O controle motor de sentar entre um e dois anos de idade é fator prognóstico favorável à aquisição da marcha independente⁵⁷⁻⁵⁹. Outro parâmetro de prognóstico para a marcha é o tipo de comprometimento motor, como exemplo, as crianças hemiparéticas que deambulam independentemente e muitas daquelas com diparesia espástica que também deambulam, mas com auxílio de suportes externos. Por outro lado, aqueles com tetraparesia espástica raramente têm deambulação funcional⁴¹. Em geral, as crianças que andam independentemente o fazem por volta dos três anos de idade; quem anda com apoio pode fazê-lo até os nove anos. Já uma criança que não anda até os nove anos de idade, dificilmente andar, mesmo com apoio⁵⁷.

Durante a adolescência e na idade adulta ocorre diminuição na função e no padrão da marcha, traduzidos por diminuição na velocidade da marcha, comprimento da passada e movimentos articulares no plano sagital^{60,61}.

A maioria das crianças com PC sobrevivem até a idade adulta. Mesmo os indivíduos mais gravemente afetados, 50% deles sobreviverão até a metade da terceira década de vida. Isso é resultado de melhor nutrição e da prevenção de complicações respiratórias^{36,62}.

3.2 ANÁLISE TRIDIMENSIONAL DA MARCHA (A3DM)

Desde a década de 1970, a A3DM tem sido utilizada na avaliação de crianças com PC. A análise da marcha foi inicialmente aplicada para fins de pesquisa, mas progressivamente passou a ser utilizada para apoiar a tomada de decisão clínica e avaliar resultados de tratamentos nessa população⁶³. O desenvolvimento da tecnologia de câmeras e computadores proporcionou maior disponibilidade de sistemas de análise da marcha com *hardwares* e *softwares* complexos necessários para realizar esta tarefa com precisão e confiabilidade (Figura 2). Estes componentes da A3DM provaram ser muito desafiadores e felizmente o processo evolutivo continua até hoje⁶⁴.

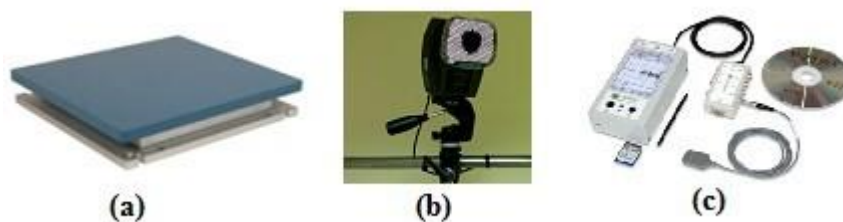


Figura 2. Equipamentos utilizados para captura do exame computadorizado da marcha : (a) Plataformas de força (*Advanced Mechanical Technology, Inc. Watertow, MA, USA*); (b) câmera com espectro de resposta sensível ao infravermelho – modelo *Hawk* (*Motion Analysis Corporation, Santa Rosa, CA*) e (c) eletromiógrafo wireless (*Delsys Incorporated, Natick, MA, USA*).

A medição acurada do movimento é central em qualquer método científico de análise da marcha⁶⁵. Atualmente, a rotina dos exames realizados nos laboratórios especializados de biomecânica são compostos pela avaliação clínica, filmagem em dois planos (sagital e coronal), coleta dos dados de cinemática e cinética tridimensional (Figura 3) e eletromiografia (EMG)⁶⁶.

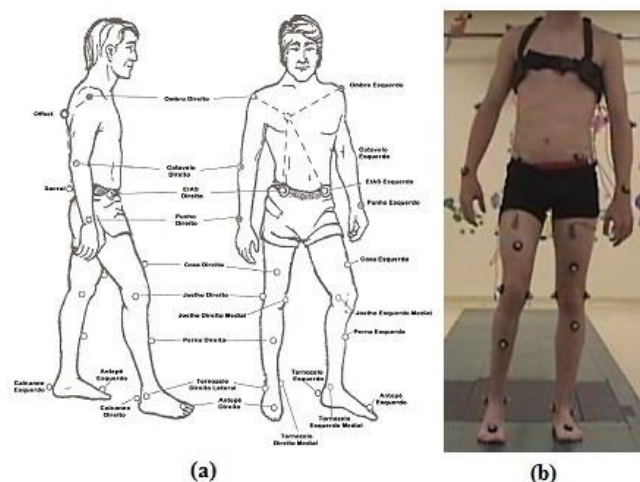


Figura 3. (a) Desenho do corpo humano nas posições lateral direita e anterior com demonstração dos pontos anatômicos segundo o modelo biomecânico Hellen Hayes (*Reference Manual OrthoTrak 6.5 Motion Analysis Corporation, Santa Rosa, CA, USA*), (b) fotografia de uma criança com marcadores reflexivos fixados aos pontos anatômicos do modelo biomecânico Hellen Hayes (arquivo do autor). EIAS: espinha íliaca ântero- superior.

Os dados da cinemática tridimensional (Figura 4) podem ser obtidos por dispositivos capazes de registrar o deslocamento realizado pelo corpo durante um

intervalo de tempo. Neste sentido, câmeras de vídeo, sistemas acústicos, sistemas eletromagnéticos, dispositivos eletromecânicos e sistemas ópticos eletrônicos podem ser utilizados. Nesta tese os dados cinemáticos tridimensionais foram obtidos por meio de um sistema óptico eletrônico com câmeras infravermelhas sincronizadas que capturam o movimento de marcadores reflexivos colocados em pontos anatômicos do sujeito em estudo⁶⁷. O futuro da captura do movimento 3D deve ser a eliminação do uso de marcadores passivos ou ativos colados ao corpo do indivíduo em estudo e a diminuição no número de câmeras⁶⁴. A força de reação ao solo e, conseqüentemente as forças atuantes no esqueleto, são capturadas por meio de plataformas de força. O padrão de atividade muscular é capturado por um sistema múltiplo de EMG⁶⁸. A EMG produz informações a respeito do recrutamento muscular promovido pela ação do sistema nervoso central. O registro dessas informações durante a marcha pode ser usado para quantificar, inclusive, o controle seletivo motor dos pacientes⁶⁹.

Apesar da aplicabilidade em várias doenças, a A3DM tem como maiores beneficiados as crianças com PC e mielomeningocele⁷⁰. Nesta população, a A3DM é utilizada para ajudar na indicação de cirurgias, de terapias físicas, nos bloqueios periféricos e na prescrição de órteses e próteses⁸.

Há um aumento crescente acerca das evidências sobre a importância da análise da marcha nas decisões clínicas. Pacientes que tem seu tratamento planejado de acordo com os resultados da A3DM apresentam resultados superiores em relação àqueles baseados somente na avaliação clínica.^{16,17 18} DeLuca *et al.* compararam as recomendações cirúrgicas feitas para sujeitos com PC oriundas da avaliação clínica e da análise de vídeo com a A3DM, e observaram mudança nas indicações em 52% dos casos⁷¹. Segundo Gough e Shortland, a análise da marcha ajudou a distinguir as crianças com PC espástica que se beneficiariam da cirurgia daquelas para as quais o manejo não-operatório era mais apropriado⁷².

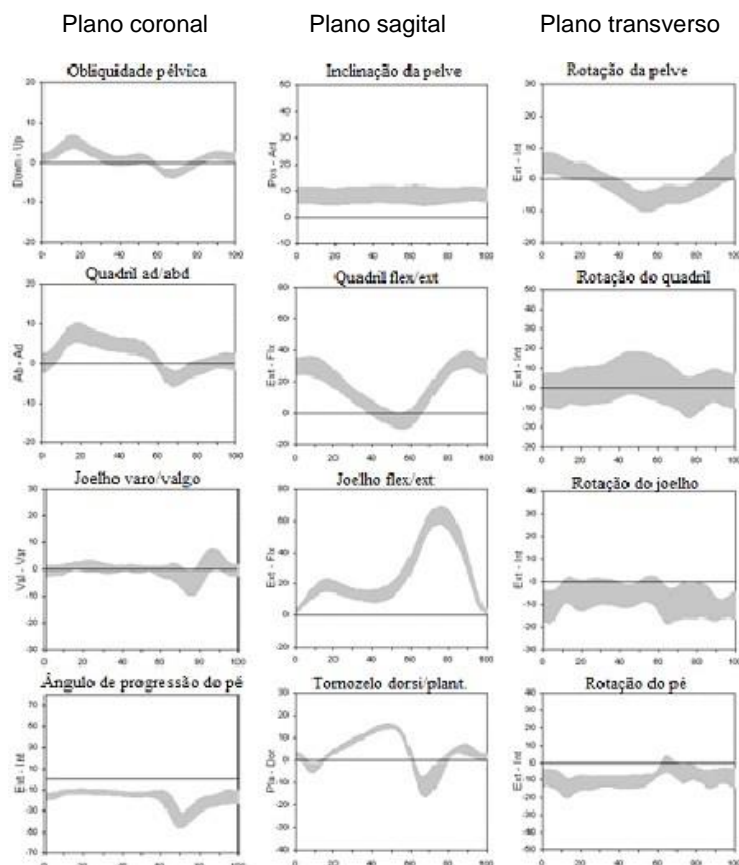


Figura 4. Gráficos de cinemática da pelve, quadril, joelho, tornozelo e pé durante o ciclo de marcha nos planos coronal, sagital e transverso. Cada quadro apresenta na vertical graus de movimento da articulação e na horizontal porcentagem do ciclo da marcha. A faixa horizontal presente em cada quadro é a marca da posição neutra. O traçado cinza representa um desvio da normalidade do movimento da articulação durante o ciclo da marcha (arquivo do Laboratório de Marcha do Centro Hospitalar de Reabilitação Ana Carolina de Moura Xavier – Curitiba – Pr.). Dow-Up: rebaixado e elevado; ab-ad: abdução e adução; var-val: varo e valgo; ext-flx: extensão e flexão; post-ant: posterior e anterior; pla-dor: plantarflexão e dorsiflexão.

Como a A3DM fornece grande quantidade de dados, que são complexos e interdependentes, foram desenvolvidos índices para descrever a qualidade do padrão da marcha de acordo com uma pontuação. Os índices pontuam o andar e podem auxiliar no entendimento de quão distante o sujeito em análise está do comportamento típico esperado^{73,74}.

As medidas de resumo mais comumente usadas são o *Gait Deviation Index* (GDI)⁷⁵ e o GPS⁷⁶, que fornecem uma única pontuação da qualidade da cinemática do paciente durante a marcha. O GDI é baseado no cálculo da distância entre os dados do paciente e a média do conjunto de dados de referência. Para esse cálculo são utilizadas 15 variáveis cinemáticas da marcha que incluem dados da pelve,

quadril, joelho e tornozelo⁷⁵. O GPS é obtido através das mesmas variáveis cinemáticas utilizadas para o cálculo do GDI. Entretanto, o GPS é calculado por meio da diferença da raiz quadrada média entre os dados do paciente e a média do conjunto de dados de referência⁷⁷. O GPS tem como vantagem poder ser decomposto nas GVS que são as variáveis cinemáticas que compõem o GPS e são representadas em um quadro chamado de “*Motion Analysis Profile*” (MAP)⁷⁸. Com isso é possível determinar quais as variáveis (que compõem o cálculo do índice) encontram-se mais distantes da normalidade.

3.3 MARCHA NORMAL

A marcha bípede de humanos é única, contrastando com os padrões de quadrúpedes e de primatas não humanos, nos quais a atividade temporal dos músculos difere significativamente^{79,80}. As pegadas deixadas nas cinzas vulcânicas de Laetoli, na África, pelos hominídeos de 3 milhões de anos atrás, indicam que eles já andavam com padrão semelhante ao homem moderno⁸¹.

O termo marcha descreve um padrão cíclico de movimentos corporais que são repetidos a cada passada⁸². A marcha humana utiliza movimentos repetitivos dos membros para avançar o corpo, mantendo simultaneamente a estabilidade no apoio⁷⁰. Isso é alcançado por padrões rigorosamente regulados de ativações musculares e geração de momentos e potências das articulações. Parte do trabalho muscular é feito para aceleração e parte é usado para controlar momentos externos resultantes da força de gravidade e da inércia do segmento em movimento⁸³.

Segundo Sutherland *et al.*, cinco determinantes são importantes indicadores de uma marcha madura: tempo de apoio simples, velocidade da marcha, cadência (número de passos dados por minuto durante a marcha), comprimento do passo e base de suporte. À medida que a maturidade avança, a cadência diminui enquanto a velocidade do andar e o comprimento do passo aumentam. Importantes fatores no desenvolvimento de um padrão maduro são o aumento do comprimento do membro e a maior estabilidade do membro, demonstrada pela duração crescente do apoio simples. Um padrão de marcha maduro, conforme determinado por esses critérios, está bem estabelecido aos três anos de idade⁸⁴.

Na marcha normal, mecanismos biomecânicos são utilizados com a finalidade de minimizar o consumo de energia pelo organismo, com mínima excursão do centro

de massa do corpo^{63,65,82}. A energia típica gasta na marcha normal (2,5 quilos de calorias por minuto) é menos que o dobro do gasto quando o indivíduo está na posição sentada ou em pé (1,5 quilos de calorias por minuto). Desvios da marcha normal aumentam muito esse custo energético⁸⁵.

A marcha humana segue um padrão constante no próprio indivíduo e muda pouco entre as pessoas, tornando possível identificar o desenvolvimento e as características maduras da marcha normal⁸⁴.

O ciclo da marcha normal (Figura 5) inicia-se pelo contato do calcâneo com o solo e termina com um novo toque do mesmo pé no solo. O ciclo da marcha é dividido em dois grandes períodos chamados de apoio e balanço. Durante o período de apoio, que corresponde a 62% do ciclo da marcha, o pé mantém contato com o solo. No balanço, responsável por 38% do ciclo, o membro inferior avança de um ponto a outro no espaço, sem contato com o solo⁸⁶.

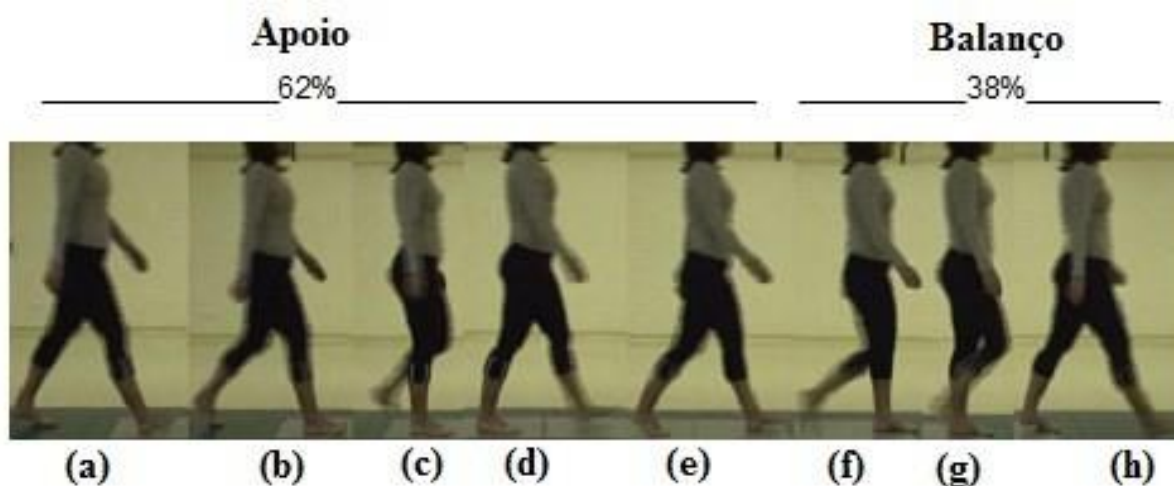


Figura 5. Ciclo da marcha (membro inferior direito) com períodos de apoio (62%) e balanço (38%). Fases do ciclo da marcha: (a) contato inicial, (b) resposta à carga, (c) médio apoio, (d) apoio terminal, (e) pré-balanço, (f) balanço inicial, (g) balanço médio, (h) balanço terminal (arquivo do autor).

Cada passada ou ciclo da marcha apresenta oito fases que correspondem aos padrões críticos do movimento sinérgico e seletivo presente no andar⁸⁶. O contato inicial e a resposta à carga são as duas primeiras fases do apoio e responsáveis pela recepção da carga pelo membro. O médio apoio e o apoio terminal representam o apoio simples, onde apenas um membro está em contato com o solo. O pré-balanço, balanço inicial, balanço médio e balanço terminal são as fases finais do ciclo da marcha normal e têm o objetivo de avançar o membro de um local a outro⁸⁷.

Parâmetros de tempo e espaço, como a velocidade e a cadência, auxiliam no entendimento da capacidade funcional da marcha do indivíduo⁸⁷.

A ação muscular produz a força necessária para promover ou restringir as articulações, podendo ser concêntrica, isométrica ou excêntrica⁷⁰. A atividade elétrica medida pela EMG determina que o músculo está ativo, mas não diferencia qual tipo de contração⁸⁸. A atividade muscular durante a deambulação é complexamente coordenada e os grupos musculares iniciam e cessam sua ação em curtos espaços de tempo. Na PC a perda da coordenação entre os grupos musculares é uma das principais causas das alterações da marcha⁸⁶.

A cinemática tridimensional, fornece uma descrição precisa dos movimentos que estão ocorrendo em uma articulação específica em todos os três planos durante o ciclo da marcha, mas as medidas são essencialmente descritivas e não fornecem a causa do movimento⁸⁵. A cinética, por outro lado, lida com as forças que produzem o movimento. Essas medidas incluem momentos e potências articulares. Momento é similar à força, exceto pelo fato de produzir um movimento de rotação⁶⁸. Momento é gerado quando uma força é exercida a alguma distância da articulação e a unidade de medida é Newton-metro por quilograma.

Por não existir uma forma direta para medir a força muscular gerada durante o andar, utiliza-se uma maneira indireta, através da força que o pé imprime durante a fase de apoio da marcha, medida por plataformas de força posicionadas no caminho a ser percorrido⁸⁹. A potência articular é medida em watts por quilograma e é o produto da multiplicação do momento articular pela velocidade angular da articulação⁹⁰.

Valores positivos para potência articular indicam que o músculo está diminuindo de tamanho (contração concêntrica) e produzindo uma aceleração. Um valor negativo indica que o músculo está alongando (contração excêntrica) e produzindo uma desaceleração⁹⁰. A potência articular é a variável que melhor descreve as fases concêntricas e excêntricas da energia mecânica que os músculos geram para realizar o movimento⁸⁵.

3.4 ASPECTOS GERAIS DA MARCHA NA PARALISIA CEREBRAL

Na PC, a lesão dos neurônios motores superiores resulta em dois tipos de efeitos. O efeito predominante e mais importante resulta da perda das conexões do trato corticoespinal com os neurônios motores inferiores e, portanto, com os

músculos esqueléticos. Isso causa paresia ou plegia, que geralmente é mais pronunciada nos músculos distais do que nos músculos proximais. Como outro efeito, supõe-se que a hipertonía e hiperreflexia sejam causadas pela perda da ação inibitória descendente aos neurônios motores inferiores, o que torna hiperativo o reflexo de estiramento no sistema neuromuscular periférico²⁸.

A alteração do controle neural dos movimentos, somado à fraqueza muscular e a uma variedade de comprometimentos osteomusculares secundários⁹¹, fazem com que indivíduos com PC usem uma estratégia de controle simplificada durante a marcha em comparação aos indivíduos não comprometidos⁹².

Segundo Perry, a marcha típica apresenta quatro pré-requisitos que são frequentemente perdidos na marcha dos indivíduos com PC. São eles: estabilidade no apoio, adequada liberação do pé para a fase de balanço, apropriado pré-posicionamento do pé no balanço e adequado comprimento do passo⁸⁶. Gage incorporou um quinto pré-requisito: a conservação de energia⁹³.

A prevalência de anormalidades específicas da marcha em crianças com PC varia com a função motora (GMFCS) e muda com a idade e com os tratamentos realizados. Após avaliar 492 indivíduos com PC, Wren *et al.* observaram como problemas mais comuns a presença de joelho rígido durante o período de balanço (80%), seguido por marcha em agachamento, caracterizada pela flexão do joelho maior que um desvio padrão da normalidade durante significativa parte do período de apoio (69%), flexão excessiva do quadril, determinada pela flexão maior que 0° no apoio terminal (65%), ângulo de progressão do pé em rotação interna (64%) e pé equino no apoio (61%)⁹⁴. A Figura 6 ilustra esses padrões de deambulação.

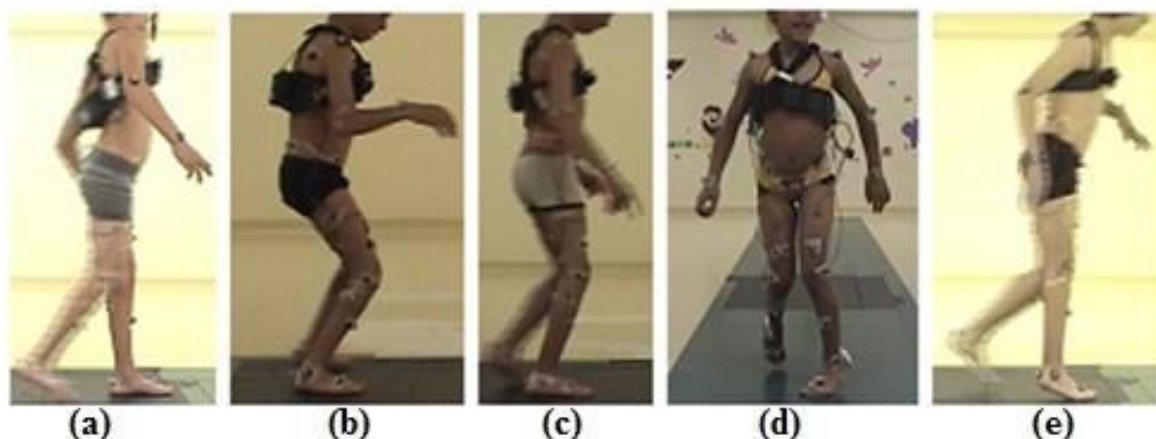


Figura 6. Padrões comuns de deambulação de crianças com PC espástica: (a) joelho rígido (flexão diminuída do joelho na fase de balanço), (b) agachamento, (c) flexão excessiva do quadril, (d) pé em rotação interna, (e) pé equino (arquivo do autor).

Note que, como os sintomas motores da PC incluem alterações relacionadas à lesão do sistema nervoso central e adaptações músculo esqueléticas, uma das características da PC é a variabilidade na apresentação clínica⁹⁵.

3.5 ÓRTESES NA MARCHA DE INDIVÍDUOS COM PC

Órtese é definida pela Organização Internacional de Padrões (ISO) como “um dispositivo aplicado externamente para modificar as características estruturais e funcionais do sistema esquelético e neuromuscular”⁹⁶.

As crianças deambuladoras com PC utilizam órteses abaixo da articulação do joelho, chamadas órteses suropodálicas (OSPs) que abrangem a articulação do tornozelo e a totalidade ou parte do pé^{8,97}.

Na marcha normal o pé e o tornozelo realizam uma série de movimentos na fase de apoio chamados rolamentos, que auxiliam a absorção do impacto do membro com o solo, promovem estabilidade no apoio e produção de potência para a marcha. Na fase de balanço, o pé e o tornozelo contribuem com dorsiflexão, para facilitar a liberação do pé do solo e auxiliar o posicionamento para a fase de apoio subsequente⁹⁸.

As crianças com PC apresentam, frequentemente, os movimentos dos pés e tornozelos alterados, devido ao desequilíbrio dinâmico entre os músculos extrínsecos da panturrilha que controlam o alinhamento desse segmento. Esse desequilíbrio pode ser consequência da espasticidade e do controle motor ou equilíbrio diminuídos⁹⁸.

Anormalidades da marcha comumente tratadas com OSPs incluem fraqueza dos flexores plantares ou dos músculos dorsiflexores, déficit no controle motor, espasticidade ou hiperatividade dos flexores plantares, instabilidade no apoio e ou problemas de equilíbrio (Figura 9). As duas categorias principais de OSPs são as fixas (rígidas) e articuladas⁹⁹.

A utilização de aparelhos ortopédicos durante o processo de reabilitação de doenças musculoesqueléticas faz parte do arsenal terapêutico. A marcha patológica de crianças com PC pode ser melhorada com o uso de órteses e a indicação do uso de OSPs deve ser feita prioritariamente após determinação da ausência de deformidades estruturadas nos tornozelos e joelhos, pois, caso contrário, a melhora funcional desejada não será alcançada.

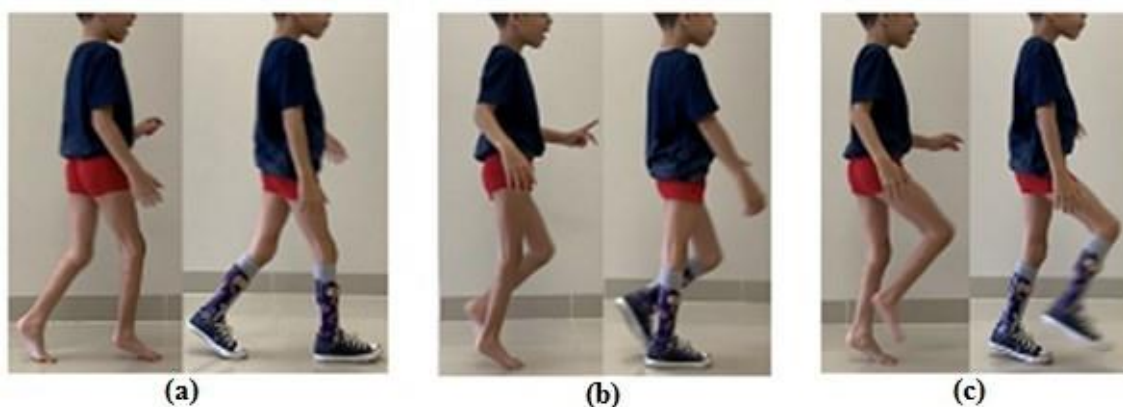


Figura 7. Indivíduo com diagnóstico de PC espástica sem e com OSP. (a) No contato inicial, (b) no médio apoio, e (c) no balanço da marcha (arquivo do autor).

As OSPs rígidas limitam a dorsiflexão do tornozelo no apoio, bloqueando o segundo mecanismo de rolamento⁸⁶, com maior extensão do joelho nesta fase como consequência. As OSPs rígidas ou articuladas são capazes de impedir a flexão plantar inapropriada no apoio, evitando um terceiro mecanismo de rolamento precoce, e ainda controlam o posicionamento do tornozelo e pé durante a fase de balanço da marcha. As OSPs articuladas não deveriam ser prescritas para crianças que apresentem dorsiflexão excessiva do tornozelo no apoio, com o potencial prejuízo de produzir flexão aumentada do joelho nesta fase da marcha⁹⁸. As deformidades flexíveis que resultam em desvio no plano coronal do pé (deformidade em valgo, varo, inversão ou

eversão) podem ser modificadas pelas OSPs, enquanto os desvios rotacionais não são influenciados com uso das OSPs.

Há fortes evidências de que as OSPs induzem pequenas melhoras na velocidade da marcha em crianças com PC espástica e moderada evidência de que as OSPs têm pequeno a moderado efeito na função motora geral¹⁰⁰, com aumento do GDI apenas em 37% dos casos¹⁰¹. Apesar de algumas incertezas, as OSP são dispositivos usados durante o dia por 21,8% das crianças com PC, segundo Sacaze *et al.*¹².

Devido a necessidade de aumentar as evidências científicas do uso de OSPs no processo de reabilitação, o primeiro estudo desta tese, avaliou o impacto global da utilização de órteses na marcha de indivíduos da faixa etária pediátrica com diagnóstico de PC, utilizando as avaliações por meio da A3DM.

3.6 CLASSIFICAÇÕES DOS DESVIOS DA MARCHA NA PC

O termo classificação da marcha refere-se a um sistema que permite a alocação do padrão de marcha do indivíduo em grupos que podem ser diferenciados uns dos outros com base em variáveis definidas previamente²⁰.

A A3DM é considerada o padrão-ouro na avaliação do andar de indivíduos com PC^{14,15}. Entretanto, a grande quantidade de dados biomecânicos multidimensionais produzidos pela A3DM, dificulta a interpretação clínica¹⁰². Resumir esses dados, usando uma classificação da marcha, pode facilitar a tomada de decisões clínicas. Consequentemente, vários Sistemas de Classificações da Marcha (SCM) têm sido desenvolvidos baseados nos dados adquiridos por intermédio da A3DM^{19,20,103–107}
108,109 110.

As principais desvantagens dos atuais SCM são: considerar apenas (ou principalmente) parâmetros cinemáticos; considerar somente um plano de movimento e elaborar as classificações para tipos clínicos específicos, dificultando o uso para a população geral de indivíduos deambuladores com PC¹¹⁰.

Os SCM são construídos de forma qualitativa ou quantitativa, com base na elaboração a partir da experiência clínica ou de dados medidos de forma objetiva, respectivamente¹⁰⁷. Por exemplo, os SCM elaborados a partir de premissas qualitativas apresentaram limitações na sua construção, com avaliação de apenas uma articulação^{111,112}, um único tipo clínico, como hemiparéticos¹¹³ ou diparéticos¹¹⁴,

e apenas um plano de movimento, o sagital^{111,113,114}. A maioria das classificações qualitativas tiveram como origem as classificações de Winters *et al.*, para hemiparéticos e as de Sutherland e Davids¹¹¹ e Rodda *et al.*¹¹⁴ para diparéticos espásticos.

A construção quantitativa utiliza cálculos matemáticos complexos, como rede Bayesiana e regressão logística, e podem usar meios automáticos para extração dos dados da ATM^{19,102}. Entretanto, o aumento no desempenho é limitado e não supera o custo computacional adicional, gerando maior risco de perda da capacidade de interpretação clínica, o que ameaça a sua aceitação e aplicabilidade^{20,102}.

Segundo o estudo de Rethlefsen *et al.*, que avaliaram 1005 crianças com PC, as alterações mais comuns na marcha deste grupo de indivíduos foram: rotação interna, flexão e adução dos quadris, flexão excessiva dos joelhos, joelhos rígidos, pé equino e em rotação interna¹⁰³. Nieuwenhuys *et al.* identificaram 49 padrões articulares, que englobavam alterações nos planos sagital, coronal e transversal, durante as fases de apoio e balanço da marcha das diversas articulações dos membros inferiores¹⁰⁸. Portanto, é possível entender que alterações da marcha na PC não estão limitadas a um único plano de movimento ou nível articular.

Um SCM para indivíduos com PC apresentaria utilidade clínica caso: a classificação fosse aplicada à marcha de hemiparéticos e diparéticos; incorporasse desvios em múltiplos níveis e planos de movimento; incluísse, quando apropriado, dados cinéticos e eletromiográficos; e levasse em consideração o uso de dispositivos auxiliares em pessoas com maior comprometimento funcional e distúrbios mais complexos do movimento.

Em 2019, Papageorgiou *et al.* realizaram uma revisão sistemática da literatura, e determinaram um consenso de padrões da marcha de crianças com PC¹¹⁰. Os seis padrões de consenso foram: genu recurvato, pé caído, equino verdadeiro, marcha em salto, equino aparente e marcha agachada.

Apesar dos padrões estarem relacionados a múltiplos níveis articulares (pelve, quadril, joelho e tornozelo), apenas o plano sagital e a cinemática foram utilizados na classificação.

Sendo assim, o segundo estudo desta tese avaliou o consenso de padrões do andar de crianças com PC, estabelecido por meio da revisão sistemática da literatura conduzida por Papageorgiou *et al.*¹¹⁰. Para tal, uma amostra de indivíduos da faixa

etária pediátrica foi classificada utilizando os padrões relatados e, assim, determinada a capacidade deste instrumento classificar esta amostra e sua reprodutibilidade.

A revisão sistemática da literatura conduzida por Papageorgiou *et al.*, determinou que para avaliar as classificações eram necessárias informações relacionadas à validade, reprodutibilidade e aplicabilidade clínica¹¹⁰. Entre os SCM avaliados por Papageorgiou *et al.*, o sistema proposto por Davids e Bagley apresentou características positivas em sua construção e significativa aplicabilidade clínica. Entretanto, não havia sido testado em uma amostra de sujeitos com PC¹⁰⁷.

O “Sistema de Classificação das Alterações da Marcha de Crianças com PC” de Davids e Bagley, incorpora aspectos úteis clinicamente e baseia-se em processos biomecânicos da PC. A classificação determina alterações do período de apoio e balanço do plano sagital (Figura 8), assim como alterações no plano transversal de movimento (Figura 9).

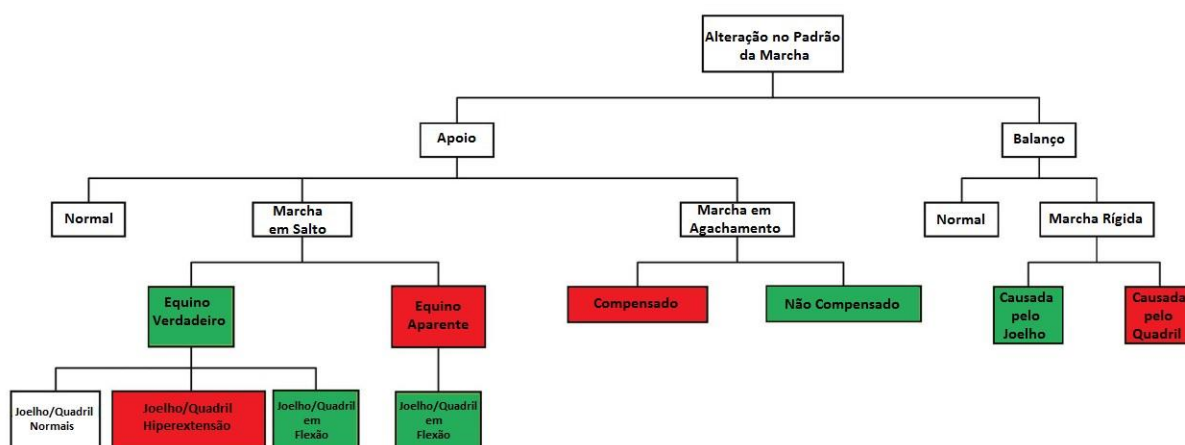


Figura 8. Classificação de Davids e Bagley do plano sagital de movimento durante o ciclo da marcha de crianças com PC¹⁰⁷. Retângulos em verde representam alterações da marcha que deveriam receber tratamento cirúrgico ortopédico e em vermelho alterações que não deveriam receber tratamento cirúrgico (reprodução com permissão do autor).

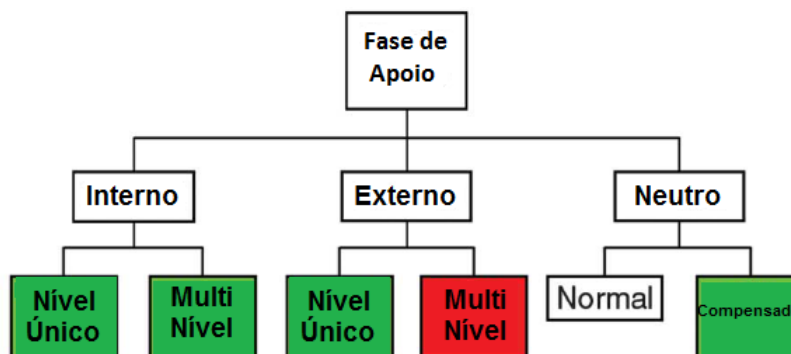


Figura 9. Classificação de Davids e Bagley do plano transverso de movimento durante o ciclo da marcha de crianças com PC¹⁰⁷. Retângulos em verde representam alterações da marcha que deveriam receber tratamento cirúrgico ortopédico e em vermelho alterações que não deveriam receber tratamento cirúrgico (reprodução com permissão do autor).

Esta classificação, apesar de ser categórica, é verticalmente integrada e considera os padrões da marcha em mais de um plano de movimento. Por conta da necessidade de SCM com boa aplicabilidade clínica, o terceiro estudo desta tese avaliou a validade e reprodutibilidade da classificação desenvolvida por Davids e Bagley¹⁰⁷ (autorizado pelo autor), uma vez que ainda não tinha sido testada em uma amostra de crianças com PC.

Por fim, um quarto estudo foi desenvolvido com objetivo de construir uma nova classificação da marcha de crianças com PC para agregar benefícios às classificações anteriormente citadas. Durante o processo de construção, os autores levaram em consideração conceitos de classificações prévias e adicionaram a importante característica de continuidade das alterações da marcha na PC. Para determinar o aspecto progressivo da classificação incluíram o conceito básico descrito por Winter (1980) de que a função primordial dos membros inferiores durante a marcha é resistir ao colapso em flexão e apresentar extensão eficiente para a produção de potência no final do apoio¹¹⁵. Dessa forma, um dos elementos da progressão utilizados nesta nova classificação é o aumento da flexão dos tornozelos e joelhos. A nova classificação incluiu, ainda, a avaliação de mais de um plano de movimento e a utilização de tutores externos durante a marcha (bengalas/muletas/andadores), por estar, esta última, relacionada a menor funcionalidade na deambulação.

4 ARTIGO 1

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Results of orthoses used on ambulatory patients with bilateral cerebral palsy.

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RESULTS OF ORTHOSES USED ON AMBULATORY PATIENTS WITH BILATERAL CEREBRAL PALSY

RESULTADOS DO USO DE ÓRTESES EM PACIENTES DEAMBULADORES COM PARALISIA CEREBRAL

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ABSTRACT

Objective: To investigate the impact of ankle-foot orthoses (AFO) on subjects diagnosed with bilateral cerebral palsy (CP) using the gait index and temporal data parameters. **Methods:** Twenty-four subjects, 14 male and 10 female, with a mean age of 11 (5-17 years old), underwent a comprehensive gait analysis under both barefoot (BF) and braced walking conditions. All children had been wearing the orthoses for at least 2 months before the gait analysis. **Results:** The overall values for the left and right Gait Profile Scores (GPS) did not show statistically significant variations when comparing the same individuals with and without orthoses. Gait velocity increased by 19.5% ($p < 0.001$), while the cadence decreased by 4% with use of orthosis, although it was not statistically significant ($p > 0.05$). The stride and the step lengths on both the right and left sides, however, resulted in statistically significant increases, when wearing AFO. **Conclusion:** AFO, prescribed for assistance by professionals without using gait data, did not significantly affect the gait index (GPS), but improved temporal data. The determination of quantitative clinical parameters for the prescription of orthotics in patients with bilateral CP, as well as orthotics that meet the specific requirements are points to be addressed in the future to obtain more significant effects. **Level of evidence III, Case control study.**

Keywords: Cerebral Palsy. Foot Orthoses. Gait.

RESUMO

Objetivo: Investigar o impacto das órteses suropodálicas (AFOs) utilizando índices de análise computadorizada da marcha (ACM) e dados de tempo e espaço, em indivíduos com diagnóstico de paralisia cerebral (PC) bilateral. **Métodos:** 24 indivíduos, 14 do sexo masculino e 10 do sexo feminino, com média de idade de 11 anos (5-17 anos), foram submetidos a uma análise da marcha, tanto na condição de andar descalço (AD) quanto com uso das órteses. **Todas as crianças usavam as órteses há no mínimo 2 meses antes da ACM.** **Resultados:** Os valores do perfil global da marcha (GPS) dos lados direito e esquerdo não apresentaram variações estatisticamente significativas quando os mesmos indivíduos foram comparados, com e sem órteses. Com o uso de órtese a velocidade da marcha aumentou 19,5% ($p < 0,001$), enquanto a cadência diminuiu 4%, embora não tenha sido estatisticamente significativa ($p > 0,05$). No entanto, com o uso da órtese, a passada e o comprimento do passo dos lados direito e esquerdo tiveram aumentos estatisticamente significativos. **Conclusão:** As AFOs, quando prescritas por profissionais sem o uso de dados da ACM, não alteraram significativamente o índice da marcha (GPS), mas melhoraram os dados de tempo e espaço. A determinação de parâmetros clínicos quantitativos para a prescrição de órteses em pacientes com PC bilateral, bem como órteses que atendam a requisitos específicos, são pontos a serem abordados no futuro, a fim de obter efeitos mais significativos. **Nível de evidência III, Estudo de caso e controle.**

Descritores: Paralisia Cerebral. Órteses do Pé. Marcha.

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INTRODUCTION

Cerebral Palsy (CP) is the most common cause of physical disability affecting children in developed countries, with an incidence rate between 2.0 and 3.5 per every 1,000 live births,¹⁻³ while in developing countries this index may reach 7 for every 1,000.⁴ The explanation for the difference between these two groups of countries is attributed

to poor conditions of antenatal care and primary care for pregnant women. Functionally, approximately 60% of patients with CP can walk independently, approximately 10% use a mobility device, and approximately 30% have limited or no walking ability.⁵ Efficient walking is an important treatment goal for children with CP.⁶ Orthotic management is a significant and useful treatment

All authors declare no potential conflict of interest related to this article.

The study was carried out at Universidade Estadual de Londrina in the Graduate Program in Rehabilitation Sciences at the Universidade Estadual de Londrina-Paraná-Brazil and at the Ana Carolina de Moura Xavier Rehabilitation Center - Curitiba-Paraná-Brazil.

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option for a number of conditions that affect gait and posture, and usually forms part of an overall rehabilitation program established for patients with CP.⁶

Orthoses are commonly prescribed to address both structural and functional deficiencies.⁷ Eighty-five percent of children with CP have had at least one orthotic device.⁸ The most commonly used lower-limb orthoses in CP are AFO that provide direct control of the ankle and foot to improve gait.⁹ Orthoses influence the ankle and foot by providing a control moment opposing ankle motion, and also stabilize the motions of the mid and forefoot joints.¹⁰

In children with CP, the aim of orthotic management in the form of ankle-foot orthoses (AFO) is to produce a more natural gait pattern. AFO may be used to protect the outcome of a surgical procedure during the healing and rehabilitation phases, to prevent the development or worsening of musculoskeletal deformities with growth and to improve gait.¹¹

The prescription of rehabilitation treatments and recommendation of orthoses is generally performed after a clinical evaluation. The use of three-dimensional gait analysis (3DGA) contributes to defining strategies for the treatment of patients with cerebral palsy.¹²⁻¹⁴ However, even with the assistance of gait analysis, the degree to which a patient's gait improves after an intervention remains difficult to assess. Considering not only how each feature of the gait pattern has changed, but also how the relationship between the features changed is important to accurately assess the changes in gait resulting from a specific treatment.¹⁵ For such, the gait profile score (GPS) will be used, in order to produce an overview of the gait.¹⁶ The gait index summarizes the kinematic data, helping the clinician to understand the general changes in gait pathology after a specific treatment.¹⁷ Our study seeks to verify the outcome of the use of orthoses by patients with cerebral palsy that were prescribed through clinical criteria due to the unavailability of gait laboratories in most cities around the world. We must question if we are really improving the gait of patients with cerebral palsy by prescribing orthoses without using 3DGA. It was hypothesized that gait index and spatial-temporal data parameters could improve with the use of orthoses.

METHODS

This retrospective cross-sectional study was conducted using the database of the gait laboratory at the Rehabilitation Center of Paraná in Curitiba, Paraná, Brazil. All participants and parents/guardians signed an informed consent form before the study. The approval of the local research ethics committee (number: 2.447.001) to conduct the study had been previously obtained. A search was conducted for all children with spastic CP who had undergone 3DGA, both barefoot (BF) and for those who were using orthoses during a single visit to the gait analysis laboratory between 2011 and 2017.

Participants

The inclusion criteria were: children with a clinical diagnosis of spastic CP, with bilateral involvement of the lower limbs, using rigid or articulated AFO (the same design worn bilaterally), who had undergone 3DGA with and without orthoses.

Previous treatments such as single event multilevel surgery or botulinum toxin type A injections were allowed, as well as the use of walkers and crutches. All children had been wearing the orthoses for at least 2 months before the gait analysis. The walking motion trials were conducted on those wearing orthoses during the same visit as the barefoot trials.

Measurements

The Gross Motor Classification System (GMFCS) and Functional Mobility Scale (FMS) were assigned by a senior clinical physical therapist and a pediatric orthopedist in appointment with the child and their parents.^{18,19}

The kinematic data was collected using reflective markers strategically placed on specific anatomical points on the participants, as described by Kadaba et al.,²⁰ and recommended by the software user's manual (Cortex Version 1.1.4.368 – User's Manual; Motion Analysis Corporation, Santa Rosa, CA, USA). Three-dimensional kinematic gait data was collected bilaterally using 6 infrared cameras and a motion capture system (infrared digital Hawk; Motion Analysis Corporation, Santa Rosa, CA) sampling at 60 Hz.

Three-dimensional gait kinematics data was used to estimate the GPS and temporal data was used to quantify the overall deviation of an individual's gait from normal gait.

GPS represents the root mean square (RMS) difference between particular gait trials and averaged data from people with no gait pathology. The overall GPS is based upon 15 clinically important kinematic variables including, gait variable score (GVS): Pelvic Tilt (Ant/Post), Pelvic Obliquity (Up/Dn) and the rotation of the left side and hip flexion, abduction, internal rotation, knee flexion, ankle dorsiflexion and foot progression for the left and right sides, as shown in Table 2. In this analysis, a GPS score for each side was used based on all nine GVS for each side. As the GPS uses all the gait features representing the root mean square difference between the patient's data and the average from the reference dataset obtained from all of the relevant kinematic variables for the entire gait cycle, the higher the GPS value the less physiological the gait pattern.²¹

Temporal data, GPS and GVS were used to quantify the changes of the gait with and without orthoses.

Three different analyses were conducted. First, all 24 participants were analyzed while walking barefoot using orthoses. Second, the participants were divided according to the use of rigid or articulate orthoses. Third, they were divided by functional status (GMFCS), classified into levels I, II, III and IV.

Statistical analysis

Data was presented as median and interquartile range, according to the Shapiro-Wilk test for normality. For intragroup analyses (with or without orthoses) the paired t-test or Wilcoxon test was performed, and for the analyses between groups (GMFCS classification and type of orthosis), the t-test for independent samples or Mann-Whitney test was used, according to the normality distribution of the data. Statistical analyses were conducted using SPSS 22 for Windows (SPSS Inc., Chicago, IL), adopting a 5% significance level.

RESULTS

The sample consisted of 24 subjects, 14 male and 10 female, with a median age of 11 [5-17 years old] and with GMFCS as follow: 1 participant at level I, 13 at level II, 9 at level III and 1 at level IV. Regarding orthosis characteristics, 10 patients used rigid AFO and 14 articulated AFO.

No significant differences were found for outcomes considering GPS overall, GPS right and GPS left side when comparing the walking tests with the individuals using or not using the orthoses (Table 1).

Table 1. Median [quartile range] of gait profile scores overall, left and right sides for bilateral cerebral palsy group when walking barefoot and with ankle-foot orthoses.

Variable	Barefoot	AFO	P
GPS overall	14.96 [13.11-18.18]	15.54 [14.05-16.40]	0.25
GPS right	13.06 [11.50-16.13]	14.15 [11.77-15.62]	0.73
GPS left	14.80 [13.00-16.85]	14.62 [12.70-16.30]	0.87

Considering GVS variables such as pelvic tilt, pelvic rotation, pelvic obliquity, hip flexion, hip rotation, hip abduction, knee flexion, ankle dorsiflexion, and foot angle of advancement, no statistically significant differences were observed between BF and with use of orthoses, except for one parameter: GVS Hip Abduction-Adduction left- barefoot = 5.76 [4.42-8.85] and with AFO = 6.44 [5.31-8.97] – $p = 0.01$. All results are shown in Table 2.

Table 2. Median [quartile range] of gait variable scores for the bilateral cerebral palsy group when walking barefoot and with ankle-foot orthoses.

Parameter	Barefoot	AFO	P
GVS Pelvic Tilt (°)	5.76 [4.24-8.77]	6.77 [4.49-9.79]	0.19
GVS Pelvic Rotation (°)	10.16 [8.52-12.84]	9.87 [7.11-13.60]	0.19
GVS Pelvic Obliquity (°)	4.45 [3.07-5.53]	4.66 [3.24-5.67]	0.39
GVS Hip Flex-Extension right (°)	11.96 [8.24-19.91]	12.06 [10.02-17.61]	0.64
GVS Hip Flex-Extension left (°)	13.26 [6.65-20.16]	12.41 [7.41-15.25]	0.08
GVS Hip Ab-Adduction right (°)	6.60 [5.26-7.45]	6.14 [5.13-8.53]	0.84
GVS Hip Ab-Adduction left (°)	5.76 [4.42-8.85]	6.44 [5.31-8.97]	0.01
GVS Hip Rotation right (°)	9.52 [7.92-14.73]	10.52 [7.92-15.16]	0.27
GVS Hip Rotation left (°)	13.84 [8.12-20.51]	11.67 [8.00-15.83]	0.66
GVS Knee Flex-Extension right (°)	21.48 [15.28-27.93]	20.87 [18.51-27.94]	0.62
GVS Knee Flex-Extension left (°)	22.53 [19.17-29.34]	22.12 [19.72-29.72]	0.58
GVS Ankle Dorsi-Plantarflexion right (°)	10.83 [7.80-14.80]	10.98 [8.74-14.34]	0.97
GVS Ankle Dorsi-Plantarflexion left (°)	11.31 [7.88-15.82]	9.42 [7.07-12.89]	0.24
GVS Foot Progression right (°)	11.88 [9.19-20.71]	15.98 [9.59-24.47]	0.06
GVS Foot Progression left (°)	15.05 [8.28-26.05]	12.85 [8.13-26.98]	0.36

When considering the spatio-temporal parameters of gait, there was a 19.5% increase in Gait velocity with the use of orthosis ($p < 0.001$). The Stride length and the step length of the right and left sides showed a statistically significant increase. No difference were observed in cadence. The values are shown in Table 3.

Table 3. Median [quartile range] of velocity and cadence. Mean (standard deviation) of stride length and step length of right and left sides for the bilateral cerebral palsy group when walking barefoot and with ankle-foot orthoses.

Parameters	Barefoot	AFO	P
Velocity (cm/sec)	68.85 [25.95-80.50]	82.31 [36.70-89.25]	0.01
Cadence (steps/min)	112.25 [68.15-123.15]	107.50 [61.42-118.87]	0.46
Stride Length (cm)	68.62 (4.15)	77.65 (4.58)	< 0.01
Right Step Length (cm)	35.15 (2.16)	40.28 (2.28)	< 0.01
Left Step Length (cm)	33.42 (2.20)	37.82 (2.49)	< 0.01

When performing the detailed gait analysis with and without orthoses according to the functional classification – GMFCS 1-2 and GMFCS 3-4, as well as between subjects using rigid and articulated orthoses, we found the same results reported for the general sample. That is, no significant difference was found between the groups related to overall, right, left GPS and GVS. However, the significant increase in velocity and stride length was maintained.

DISCUSSION

The most typical use of an AFO is to optimize the normal dynamics of walking by applying a mechanical constraint (control moment) to the ankle to control motion and, at the same time, to produce a more efficient gait.²²

Different types of orthoses may be prescribed for children with CP, such as AFO, which can help with alignment and in improving gait quality. AFO in fact, reduce, plantarflexion of the ankle, leading to greater stability in the support phase of gait.²²

The values for general, left and right GPS did not present statistically significant differences when comparing the same individuals with and without the use of orthoses. These results are in concordance with a previous study by Danino et al.,²³ that did not find any changes in GPS in subjects with cerebral palsy when walking BF and using AFO. The explanation for the non-improvement in GPS was postulated because the index mainly examined the general kinematics of gait as measured from normal, and despite some changes in distal parameters, the overall gait pattern did not change significantly.

Our study analyzed GVS variables and significant changes were not found when analyzing the subjects walking BF or with orthoses, except for, hip adduction/abduction at the left side, the only parameter that changed. However, this had no clinical significance. In contrast with our results, Galli et al.²² reported improvement in GVS of the ankle and pelvic tilt with a small sample of 10 subjects diagnosed with bilateral cerebral palsy, walking barefoot and with AFO. It is important to remember that the GVS evaluates the area of the kinematic curve as a whole. However, the orthosis positions the ankle in such a way that it avoids extreme positions of plantar flexion and/or dorsiflexion, without necessarily making the ankle movements look close to normal.

On the other hand, the temporal parameters showed changes that included gait velocity increasing by 19.5% with the use of the orthoses, while the cadence decreased by 4%, although the latter is not statistically significant. The lengths of the stride and step of the right and left sides had a statistically significant increase.

With the concept of minimal clinically important difference (MCID), which means a limit to determine when significant changes occur, there is an increasing emphasis in clinical research into establishing whether outcomes are clinically meaningful, as well as statistically significant.^{24,25} Oeffinger et al.,²⁶ reported that changes in gait velocity, cadence and stride length, respectively 9.1%, 8.1% and 5.8% from normal were MCID. The mean subject's velocity, cadence and stride length in our study changed 19.5%, – 4.2% and 13%, respectively. When comparing these changes with normal values, we noted that the velocity and the stride lengths were MCID. The reported changes that reach statistical significance were also clinically meaningful (gait velocity and stride length). As walking velocity is often used as a surrogate measure for overall gait quality, we can say that orthoses in our sample produced functional benefits, agreeing with a systematic review and meta-analysis published by Lintanf et al.,²⁷ despite avoiding the appearance of musculoskeletal deformities. Furthermore, we can observe the results above point to an improvement in function, since the increase in velocity relates to an increase in the stride length, rather than an increase in cadence, as shown in Table 3.

The authors also performed the subdivision of the sample considering greater and lesser motor impairment (GMFCS 1-2 and GMFCS 3-4), and by the type of orthosis used (articulated or rigid). The results reported for the general sample were the same when the sample was divided using the level of motor impairment and type of orthosis. Therefore, the heterogeneity in the sample was not responsible for the changes.

For children with CP, Davids et al.,¹¹ argued that analogous with multilevel surgery decision making, optimal orthotic management

requires the physician to clearly identify the gait deviation and functional deficits to be addressed using the orthosis.

Recommendations for orthoses must meet specific requirements in physical exams and in gait performance. Adequate range of motion for typical alignment while walking is necessary to properly fit the orthosis and to expect good functionality. This requires at least a neutral ankle dorsiflexion with the knee extended and no knee flexion contractures. Femoral anteversion and tibial torsion decrease the effectiveness of a well-made orthosis and should be identified and corrected to maximize effectiveness.⁷ Rodda and Graham,²⁸ proposed the use of articulated AFO in true equinus gait and jump gait as well as the use of rigid AFO for apparent equinus and crouch gait. This recommendation reveals the concern with keeping the ankle in a more neutral position during the stance phase of gait. Careful clinical evaluation of the patient by the professional is essential to avoid prescribing an orthosis under suboptimal conditions for use. Clinical gait analysis may aid in orthosis recommendations. In our study, the fact that prescriptions for orthoses were issued without the aid of quantitative data (gait analysis), may have been a contributing factor for non-significant changes in some parameters such as ankle GVS.

The lack of evidence is also observed due to the scarcity of prescription guidelines.²⁹ In clinical practice, this lack of consensus observed due to differences in treatment paradigms regarding both the recommendations and the mechanical construction of AFO.⁹ A systematic review on the quality of AFO studies in children with CP concluded that substantial variability in the quality or reporting was present in currently published studies.³⁰

The prevention of the occurrence of skeletal muscle dysfunction is one of the reasons to prescribe orthoses in this population. Studies such as these do not evaluate this important effect of the use of orthoses in patients diagnosed with CP.

The limitations of our study relate to the small study cohort sample, collected out of convenience and for the efficacy of orthoses, who were evaluated in a laboratory, and not in an environment where children participated in normal daily activities.

Clinical implications

The attending professional needs to carefully assess the recommendations and effects of orthoses on ambulatory patients with CP. This is because some predicted effects of orthoses recommendations may not be achieved, as occurred in the sample studied in which no changes were observed in the overall gait characteristics.

The determination of quantitative parameters for the prescription of orthotics in patients with bilateral CP, as well as orthotics that meet specific requirements are points to be addressed in the future to obtain more significant effects.

CONCLUSION

In this study, the AFO, prescribed for assistance by professionals without using gait data, did not significantly affect the gait index (GPS), but improved temporal data. Answering the question: are we improving the gait of patients with cerebral palsy by prescribing orthoses without using 3DGA? In the evaluated sample the patients using orthoses became more functional with increased velocity, step and stride length. However, the movements of the lower limbs were no closer to normality.

AUTHORS' CONTRIBUTIONS: Each author contributed individually and significantly to the development of this article: AGM: article design, project design and writing; ACP: data collection and review; DDI: data collection and review; RFMC: data collection and review; SS: statistical analysis, writing and review.

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5 ARTIGO 2

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Title:

The reliability and validity of the multiple joint pattern consensus of gait classifications in children with cerebral palsy.

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Abstract

Purpose: Evaluate the reliability and validity of a gait classification of multiple joint patterns consensus from systematic literature review multiple performed by Papageorgiou et. al. in 2019.

Methods: One hundred and thirty children with CP (61 girls; 69 boys); median age was 12 [10-15] years. Participants were classified using the classification of Papageorgiou et al. through three-dimensional gait analysis. The GMFCS, velocity, cadence, stride length and GPS were determined to characterize the groups of the gait classification. The comparison between the groups was performed using Kruskal-Wallis test, according to the normality of the data. The significance level adopted was 5%. The reliability of the classification was determined using weighted Kappa for inter and intrarater, with 95% confidence interval (CI).

Results: All classification groups were represented in the evaluated sample. 95.4% of the participants in the sample were classified. The six children (4.61%) not classified all had a homogeneous pattern. The classification showed superposition of the kinematic characteristics between close groups. Interrater reliability was 0.803 (0.652-0.953) and intrarater was 0.795 (0.583-1.007) and 0.531 (0.327-0.735).

Conclusions: The present study aims to provide a first insight of the aforementioned consensus-based GCS in children with CP. The proposed classification system is possible to be used in patients with unilateral and bilateral involvement and classified 95.4% of the participants in the sample. The reliability was almost perfect interrater with moderate and substantial intrarater. Consequently, the proposed classification has validity and important clinical utility to classify the sagittal plane of children with CP.

Keywords: Cerebral palsy, Gait, Classifications, Children.

1. Introduction

Accurate gait classification of Cerebral Palsy (CP) can be challenging because of its heterogeneous presentations¹. The motor symptoms associated with CP including spasticity, weakness, impaired balance, and loss of selective motor control affect the child's ability to walk. Because of these different motor symptoms, the variability with which CP affects gait is considerable².

Functionally, approximately 60% of patients with CP are able to walk independently, 10% use a mobility device, and 30% have limited or no walking ability³.

Gait Classification System (GCSs) have been reported to aid in clinical decision making, in improving communication among healthcare providers and in comparing gait between or within specific patients. The GCSs may include the description of deviations occurring in a single or multiple joint pattern simultaneously, the latter category being preferable for the known interrelation of the joints of the lower limbs during ambulation⁴.

The method in which one classification is constructed was coded as either qualitative or quantitative. Qualitative construction methods included those where decisions to group members relied on the judgment and experience of those making the decisions⁵⁻⁷. A potential advantage of qualitative methods is to be more meaningful in terms of clinical diagnosis and treatment planning. When quantitative methods for classification construction were used, the majority of the studies used a variation of cluster analysis⁸. The limitations of cluster analysis include that the process may uncover groups that have no clinical relevance or meaning⁹.

However, both classification processes did not produce a classification capable to cluster the universe of gait possibilities of CP patients as well as being clinically useful. This statement is confirmed by observing the studies of Dobson et al.¹⁰ and McDowell et al.¹¹ They found 12% and 42% of children with hemiplegia as not classifiable according to the Winters⁵ criteria, respectively. In diplegia patients Walsh et al.¹² who applied the GCS of Rodda et al.⁷ where 3 patients in 20 could not be classified and de Morais-Filho, who could not classify 13% of their patients (n=228)¹³ when using the GCS of Sutherland and Davids⁶. More recently, in a reliability study of a GCS where 4.7% of all gait trials could not be classified according to the rules suggested by Nieuwenhuys et al.¹⁴. An additional challenge for gait classification in children with CP is that often the observed joint motions do not match perfectly with a

set of predefined joint motion patterns, and some kind of accommodation ends up being accepted to set a pattern.

Using a literature review, Papageorgiou et al. in 2019, revealed that six multiple joint patterns displayed a relevant consensus⁴. The six multiple joint patterns were derived from classifications built using qualitative methods⁵⁻⁷. Another important factor of the new classification is the fact that it presents existing patterns in patients with unilateral and bilateral neurological involvement. Thus, the clinical applicability of this classification needs to be tested to determine whether the described elements produce a greater ability to classify children with CP.

According to the authors knowledge, the present study is the first to classify a sample of CP patients using the six multiple joint patterns consensus published by Papageorgiou, 2019⁴. Thus, the purpose of this study was to test the consensus⁴ to classify a sample of CP patients. The study focused on exploring whether these six commonly used multiple joint patterns cover all potential patterns in children with spastic CP and the reliability of this classification. The secondary objective was to characterize each pattern based on age, Gross Motor Function Classification System (GMFCS)¹⁵, Gait Profile Score (GPS)¹⁶ and spatiotemporal data parameters (velocity, cadence and stride length).

2. Methods

2.1 Design

A retrospective cross-sectional and reliability study was conducted using the database from Gait Analysis Laboratory of the Ana Carolina de Moura Xavier Rehabilitation Hospital Center in Curitiba, Paraná, Brazil. The project was approved for a local research ethics committee under opinion 2.447.001. The study was developed by an estimated sample of 115 individuals considering the prevalence of 0.3% [3] and maximum standard error of 1%. The search conducted to the database between 2010 and 2017, provided a sample of 130 children who had undergone gait analysis with a diagnosis of spastic cerebral palsy.

The study was performed in two stages. The first was a utility study classifying gait patterns in children with CP using the consensus of the gait classifications for children with CP proposed by Papageorgiou et al.⁴. The second stage was to investigate the intra and inter-observer reliability of the classification.

2.2 Participants

Eligible participants were between 5 years old and 18 years old, classified in GMFCS levels I to IV, predominantly spastic CP. Previous treatments such as single event multilevel surgery or botulinum toxin type A injections were allowed.

All participants underwent a three-dimensional gait analysis under barefoot (BF) walking conditions with self-select speed, during a single visit to the gait analysis laboratory. They have received no benefits.

2.3 Cross-sectional study

The sample group comprised of 130 patients who fulfilled the study criteria, and were classified according to the Papageorgiou et al., by one rater with wide clinical experience in gait analysis. After classifying the sample, the groups formed were compared in terms of age, gait velocity, cadence, stride length and GPS.

2.4 Reliability study

A learning phase was proposed, in which all raters attended and participated in an online presentation, to discuss the classification of, and to present examples that illustrated how to classify cases using Papageorgiou et al. classification. The raters were provided with written definitions and illustrations of the posture of the ankle, knee, hip and pelvis for each gait pattern in relation to the planes of motion ((supplementary material).

To determine interrater reliability, 25 participants (50 lower limbs), from the total sample, were selected to create a sample that included variation in age and levels of neurological involvement (GMFCS). Two raters, with more than 3 years of experience in gait analysis, classified the sample. To determine intrarater reliability one rater evaluated the 25 participants (50 lower limbs) a second time, one month after the initial assessment. The order of the 25 participants was randomly changed between the 2 viewing sessions.

2.5 Measurements

The GMFCS was assigned by a senior clinical physiotherapist and a pediatric orthopedist in consultation with the child and his or her parents.

Each participant's gait was recorded on video, using sagittal and coronal views. Instrumented 3DGA was performed using the conventional gait model (Helen-Hayes

model)¹⁷, with reflective markers (n =26), to obtain spatiotemporal parameters (step and stride lengths, cadence, walking velocity) and lower extremity kinematics at the pelvis, hip, knee, and ankle. The trajectory of the markers within the lab space was captured through an electronic optical system consisting of six digital motion analysis cameras (Motion Analysis Corporation in Santa Rosa, CA) sampling at 60 Hz. Joint kinematics were calculated by the Cortex software (Motion Analysis Corp., Santa Rosa, CA). The data was processed using OrthoTrack software (OrthoTrack 6.5.1 software, Reference Manual 2007. Motion Analysis Corporation, Santa Rosa, CA). The data were smoothed using a Butterworth filter with a cut-off frequency of 6 Hz. The motion analysis system was calibrated before each analysis. All kinematic data were time-normalized to 100 % of one gait cycle.

3DGA kinematics were used to calculate the GPS, which quantifies the overall deviation of an individual's gait from normal gait¹⁸.

The kinematic data were collected from a minimum of 7 gait cycles for each assessed leg and the most representative trial was reported, alongside the corresponding video clips, and classified according to the six multiple joint patterns consensus⁴ (Table 1).

Children who presented an asymmetrical pattern, that is to say, classification on one lower limb side which differed from the other, were classified as asymmetrical group. Children with kinematics of the lower limbs close to normal, were classified as without abnormalities group. Children that presented abnormal kinematic of the lower limbs but did not fit in any classification group, were classified as being in the, not classified group.

2.6 Statistical Analysis

Descriptive data were presented as medians and interquartile ranges, according to the non-normality distribution, analyzed using the Shapiro-Wilk test. Levene test was used to verify the homogeneity of variances. For the comparison between groups was used the Kruskal-Wallis test using Mann-Whitney's post hoc test. The statistical significance was $P < 0.05$.

The reliability of the classification was determined by weighted Kappa (k) statistics for inter and intrarater, with 95% confidence interval (CI). The strength of k was interpreted as: equal to zero, "without agreement"; between zero and 0.19, "poor agreement"; from 0.20 to 0.39, "weak agreement"; from 0.40 to 0.59, "moderate

agreement"; from 0.60 to 0.79, "substantial agreement"; from 0.80 to 1.00, "almost perfect agreement" ¹⁹.

The analyses were performed in IBM SPSS Statistics for Mac, version 27.0 (IBM Corp., Armonk, N.Y., USA).

3. Results

The sample consisted of 130 children with spastic CP, 69 (53.1%) being male and 61 (46.9%) female, of which 114 had been diagnosed with bilateral and 16 with unilateral CP, whose median age was 12 [10-15] years.

The classification of the participants according Papageorgiou et al. resulted in the following distribution among groups: genu recurvatum 10 (7.7%); drop foot 18 (13.9%); true equinus 4 (3.1%); jump gait 18 (13.9%); apparent equinus 9 (6.9%); crouch gait 27 (20.8%); 7 without abnormalities by classification (5.4%); 6 not classified (4.6%); 31 asymmetrical (23.9%). Thus, 95.4% of the sample was classified with 4.6% presenting abnormalities in gait that cannot be classified in one of the classification groups. Considering the distribution of participants according to the GMFCS classification, most participants were included in the GMFCS II (82), followed by the GMFCS III (24), GMFCS I (20) and GMFCS IV (4).

Note that the most common gait pattern seen in participants classified in GMFCS I was drop foot (40,0%). In GMFCS II, the most frequent group was asymmetrical (29.3%). The group most observable in GMFCS III was crouch gait (37.5%). In GMFCS IV, three patients had crouch pattern (75%), and one patient who was classified as asymmetrical, also had one lower limb in crouch, as well.

The summarized sagittal plane kinematic data for the study population is shown in the Figure 1. Across the gait patterns, from genu recurvatum to crouch gait, there were changes between the anatomical levels. At the ankle, there was a change from normal dorsiflexion to equinus and then to excessive dorsiflexion. At the knee, there was hyper extension, which was followed by increasing flexion. The hip and the pelvis, there are no visual changes between the patterns.

The groups showed no statistically significant difference in relation to age and cadence. Differences between groups were observed regarding speed, cadence, stride length and GPS as recorded in Table 2. Taking into account time-distance parameters, the groups without abnormalities, drop foot, true equinus and jump gait

had faster and longer velocity and stride length than the crouch gait pattern participants.

The GPS of the participants in the jump gait, apparent equinus and crouch gait groups presented statistically significant differences in relation to the group without abnormalities ($p < 0.001$). The GPS for the group without abnormalities by the classification had a median of 9.50 [8.39-11.70] (Table 2).

With regard to patients in the not classified group, a total of six children, all of them had the same pattern detected by 2D video and kinematics of the sagittal plane. As shown in Figure 2, the individuals presented trend to knee extension at some point during the stance phase, peak knee flexion delayed in swing phase and dorsiflexion close to normal or increased.

Concerning reliability study, the reliability interrater had almost perfect agreement and the reliability intrarater had moderate and substantial agreement, for rater one and two, respectively (Table 3).

4. Discussion

In recent systematic literature review of gait classifications in CP, Papageorgiou et al.⁴, pointed six multiple joint patterns that reached a consensus in literature. Papageorgiou's classification⁴ added the Rodda classification⁷ into two sub types: "drop foot" and "genu recurvatum". The drop foot pattern was present in Winter's classification⁵ for hemiplegics, while the genu recurvatum pattern was one of the sub types of Sutherland's classification⁶ for diplegics. Thus, the Papageorgiou classification⁴ has as its premise to classify patients with unilateral and bilateral involvement.

Pioneering the classification mentioned above in a patient sample of 130 children diagnosed with spastic CP with unilateral and bilateral involvement, it was found that six participants (4.61%), were not classified and seven (5.38%), showed no detectable abnormalities by classification. These values, although relevant, are lower than when other qualitative classifications were used in children with CP¹⁰⁻¹³. This is because the GCS categories fail to cover all possible gait deviations in children with CP. On the other hand, it has been argued that the gait of children with CP lies along a continuum²⁰. Categorization in fixed patterns leads the evaluator to include within the categories, participants who do not fulfill all the requirements for this. This continuum

of gait abnormalities can be seen in figure 1 by the overlap of the kinematic characteristics of the lower limb joints in some parts within the gait cycle.

Despite the difficulty in establishing a single classification for the varied gait changes in CP, 95.38% of the participants within the sample were classified. Another important contribution of the Papageorgiou's classification⁴ system was the inclusion of this sample of patients with both unilateral and bilateral involvement. This is because the construction of the classification was elaborated using as a basis the gait classifications for both hemiplegic⁵ and diplegic⁷ children.

The gait patterns, from genu recurvatum to crouch gait, presented kinematics changes between the anatomical levels. At the ankle, there was a change from normal dorsiflexion to equinus and then to excessive dorsiflexion. At the knee, there was hyper extension, which was followed by increasing flexion. The results of this paper are similar to Rodda et al⁷. in relation to ankle and knee. Thus, the full biomechanical assessment is essential to evaluate and plan the individual treatment of the patients^{21,22}.

The statistical evaluation of the outcome variables (age, velocity, cadence, stride length and GPS), did not point to differences between the classification groups that could be considered clinically significant (Table 2). Although the comparison between the groups showed some statistically significant differences, it was not possible to determine an evolutionary trend of greater or lesser functional impairment with the classification under study and the groups formed.

It should be reported that patients classified as without abnormalities by the classification had a median GPS of 9.50 [8.39-11.70], and the value for children without disabilities is 5.3^{9,23}. This may be related to the fact that the Papageorgiou's classification⁴ does not consider some data used to calculate the GPS index, as changes in the swing phase of the gait and in other motion planes. As described by Davids and Bagley²⁰, new classifications must take into account the coronal and transverse planes of movement, in addition to the sagittal.

Ounpuu et al.²⁴, mention an overlap of gait problems among patients in the various GMFCS levels, what was also observed in the present study (table 2). On the other hand, the present study in agreement with Rethlefsen et. al.²⁵ found an increase number of equinus posture in lower GMFCS levels and calcaneus posture with crouch gait in higher GMFCS levels. According to Rethlefsen et. al.²⁵ and studies of natural progression of gait in children with CP^{24,26}, there is a deterioration of gait function over

time with great number of individuals with equinus in early in life and calcaneus gait with increasing age. The previous descriptions corroborate the idea of walking in CP children is a continuity, both due to the variability in presentation and the possibility of progression of musculoskeletal deformities. So fixed categorizations, while important, do not include these transition phases. Proof of this is that the present study detected a pattern in participants not classified by the consensus published by Papageorgiou et. al⁴. These individuals had dorsiflexion of the ankle close to normal or increased, knee extension at some point of the stance and peak knee flexion delayed in swing phase. The participants not classified have a different pattern from that observed in jump gait participants due to the lack of equinus during stance phase. They can also be differentiated from apparent equinus gait and crouch gait due to the knee extension that occurs at some point in the stance phase. Researchers should pay attention to this reported movement pattern, as it is possible that this is a transition between pattern or a new one.

The separation of children who walk in equinus during stance phase in two different patterns, true equinus and genu recurvatum, according to Papageorgiou et al. it is still debatable. This is because the prevalence of these groups may not be sufficient to consider different groups. In the present study, only four children were classified as being of the true equinus pattern, which keeps the debate open. The reliability of the gait classification was established using the weighted kappa statistic for both interrater and intrarater, which showed almost perfect and substantial to moderate agreement, respectively. The validity of this classification has been established by the ability to classify a patient sample and confidence on the technique of choice, sagittal kinematics.

In the future, classifications should assess changes in the coronal and transverse planes as contributing to the inability to maintain proper sagittal plane alignment. Initiatives that evaluate the swing phase of the gait and other movement plans remain desirable. The overlap in the kinematic characteristics within the groups revealed that the future classifications could be considered as a continuity rather than categorizing in a static way.

The current study had some limitations. Most participants evaluated were seeking orthopedic intervention to improve their ambulatory function, their gait problems may not reflect those of the general CP population. Some patients used walking aids during gait analysis testing, which could have impacted kinematic data

and, therefore, prevalence of gait deviations such as excessive hip flexion. The influence of previous treatments was not considered in this analysis, since the main objective of the study was to evaluate the instrument's ability to classify the gait of a subject with CP.

5. Conclusion

The present study aims to provide a first insight of the aforementioned consensus-based GCS in children with CP. The proposed classification system is possible to be used in patients with unilateral and bilateral involvement and classified 95.4% of the participants in the sample. The reliability was almost perfect interrater and moderate to substantial intrarater. Consequently, the proposed classification has validity and important clinical utility to classify the sagittal plane of children with CP.

Author contribution statement

Alessandro G. Melanda (Conceptualization) (Methodology) (Validation) (Formal Analysis) (Investigation) (Data Curation) (Writing – Original Draft) (Writing – Review & Editing) (Visualization) (Supervision).

Ana C. Pauleto (Writing – Review & Editing) (Visualization).

Alexandre R M Pelegrinelli (Data Curation) ((Writing – Review & Editing) (Visualization).

Alana EK Ferreira (Writing – Review & Editing) (Visualization).

Dirce Shizuko Fujisawa (Conceptualization) (Visualization) (Supervision).

Suhaila Mahmoud Smaili (Conceptualization) (Formal Analysis) (Writing – Review & Editing) (Visualization) (Supervision).

All authors have read and approved the final manuscript.

Declaration of Competing Interest

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Supplementary material

Appendix A. Written description of the gait consensus classification for children with Cerebral Palsy.

Appendix B. Orientation of how to use the Classification System (PowerPoint presentation for the raters).

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Table 1. Definition of gait parameter of the Gait Classification System from the consensus of Papageorgiou et al.⁴

Sagittal Kinematics				
Gait Pattern	Pelvic tilt	Hip fx/Ext	Knee Fx/Ext	Ankle Df/Pf
Genu Recurvatum	Normal Anterior	Normal Flexed	Towards or in Hyperext.	Reduced dorsiflexion or plantarflexion
Drop Foot	Normal or Minor deviations	Normal or Minor deviations	Normal or Minor deviations	Plantarflexion during the swing phase
True Equinus	Normal Anterior	Normal	Normal	Plantarflexion
Jump Gait	Normal Anterior	Normal Flexed	Flexed	Plantarflexion
Apparent Equinus	Normal Anterior	Flexed	Flexed	Normal
Crouch Gait	Anterior Normal Posterior	Flexed	Flexed	Excessive dorsiflexion

Hip fx/Ext: hip flexion and extension; Knee Fx/Ext: knee flexion and extension; Ankle Df/Pf: ankle dorsiflexion and plantarflexion; Hyperext: hyperextension.

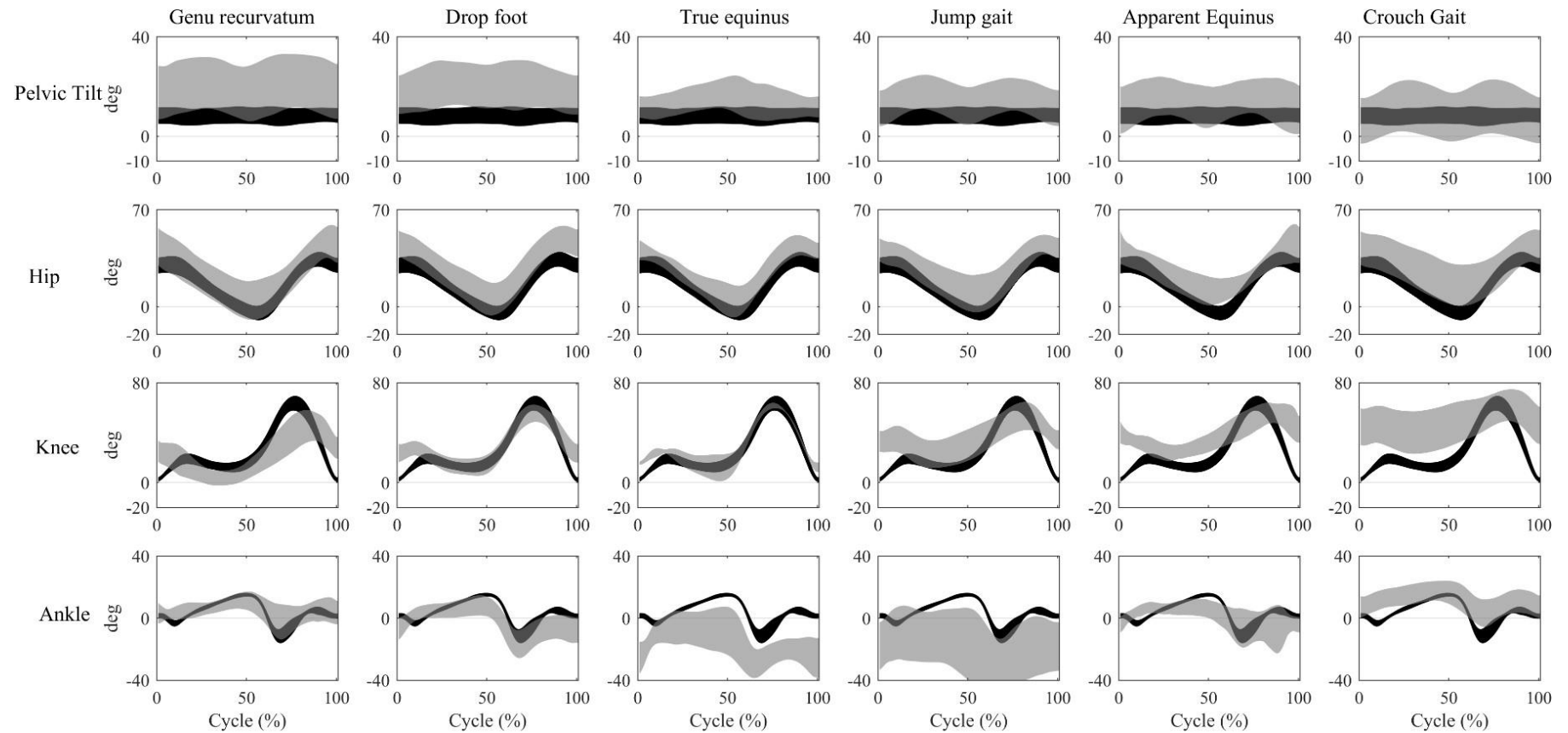


Figure 1. The summarized sagittal plane kinematic data for each gait pattern for the study population. The black band represented the mean \pm 1 SD of kinematic data normal database, and the grey band the mean \pm 1 SD for each gait pattern. The vertical axis represents joint angular displacement and the horizontal axis, 100% of the gait cycle.

Table 2. Median and interquartile range of the variables age, gait velocity, cadence, stride length and GPS in relation to 130 children according to gait pattern of the groups under investigation.

Gait pattern/ variables	Genu recurv n=10	Drop foot n=18	True equinus n=4	Jump gait n=18	Apparent Equinus n=9	Crouch gait n=27	Not class n=6	Without abnorm n=7	Asym. n=31	P
Age (years)	15.5 [11.5-17.0]	11.0 [8.5-13.0]	11.0 [8.0-12.5]	11.0 [9.0-13.0]	11.5 [7.0-16.0]	14.0 [12.0-16.0]	11.0 [8.2-14.0]	14.0 [11.0-15.0]	12.0 [9.0-15.0]	0.052
Velocity (cm/sec)	73.9 [25.1-110.5] ^a	94.9 [80.5-109.1] ^{e,f,g}	104.70 [89.9-108.2] ⁱ	90.0 [72.8-106.1] ^{l,m,o}	71.1 [18.7-81.7]	64.8 [41.1-81.5] ^s	77.4 [61.4-98.2]	90.0 [75.5-98.4] ^u	70.2 [58.5-88.6]	<0.001
Cadence (step/min)	109.3 [64.1-117.4] ^b	114.2 [105.7-126.0] ^f	118.8 [103.9-127.1]	124.7 [106.3-138.6] ^{l,m,o}	106.9 [48.2-121.7]	99.6 [80.0-116.1]	120.9 [87.5-131.2]	109.3 [94.1-126.3]	111.7 [99.4-119.0]	0.440
Stride Length (cm)	81.2 [56.9-107.2] ^a	100.4 [90.4-100.4] ^{e,f,g}	103.7 [99.5-108.0] ⁱ	89.2 [70.4-102.5] ^m	69.2 [45.0-86.7] ^q	74.0 [58.0-86.2] ^s	88.7 [77.3-95.9]	108.3 [91.0-113.7]	80.0 [65.7-98.1]	<0.001
GPS (°)	13.0 [12.2-14.6] ^c	12.7 [11.2-14.2] ^{d,f}	9.3 [8.6-11.1] ^{h,i,j}	18.3 [12.0-19.5] ⁿ	12.4 [11.5-15.6] ^p	16.4 [14.6-21.2] ^{r,s,t}	12.2 [11.2-14.9]	9.5 [8.3-11.7] ^u	14.3 [11.2-17.8]	<0.001

Cm: centimeters; cm/sec: centimeter per second; step/min: steps per minutes; genu recurv: genu recurvatum; without abnorm: without abnormalities; asym.: asymmetrical; (°): degrees; not class: not classified; without abnorm: without abnormalities.

a = statistically significant difference between genu recurvatum and drop foot.

b = statistically significant difference between genu recurvatum and jump gait.

c = statistically significant difference between genu recurvatum and crouch gait.

d= statistically significant difference between drop foot and jump gait.

e= statistically significant difference between drop foot and apparent equinus.

f= statistically significant difference between drop foot and crouch gait.

g= statistically significant difference between drop foot and asymmetrical.

h= statistically significant difference between true equinus and jump gait.

i= statistically significant difference between true equinus and crouch gait.

j= statistically significant difference between true equinus and asymmetrical gait.

l= statistically significant difference between jump gait and apparent equinus.
m= statistically significant difference between jump gait and crouch gait.
n= statistically significant difference between jump gait and without abnorm.
o= statistically significant difference between jump gait and assymetrical gait
p= statistically significant difference between apparent equinus and crouch gait.
q= statistically significant difference between apparent equinus and without abnorm.
r= statistically significant difference between crouch gait and not class.
s= statistically significant difference between crouch gait and without abnorm.
t= statistically significant difference between crouch gait and assymetrical gait
u= statistically significant difference without abnorm. and assymetrical gait

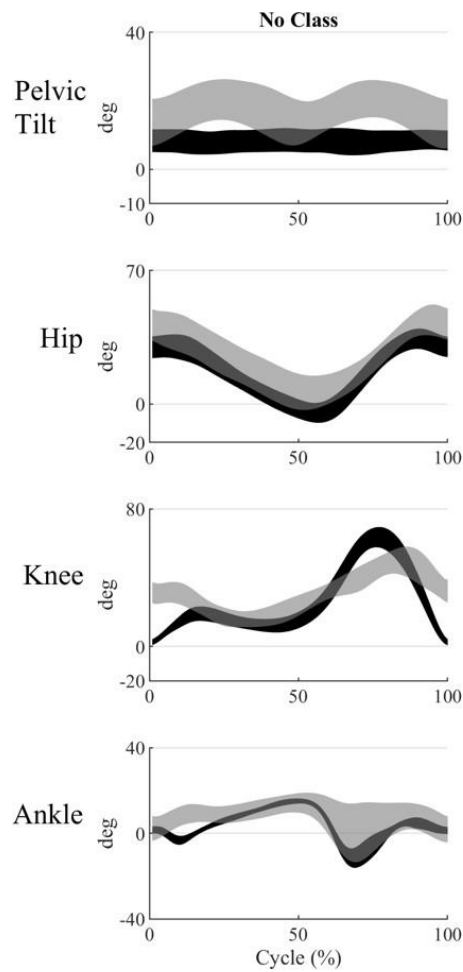


Figure 2. The summarized sagittal plane kinematic data for the limbs of the not classified participants. The black band represented the means ± 1 SD (Standard Deviation) of data normal database, and the grey band the mean \pm SD for each =gait pattern. The vertical axis represents joint angular movement and the horizontal axis, 100% of the gait cycle. No class: not classified.

Table 3. Weighted Kappa (k) statistics with 95% CI for interrater and intrarrater reliability of the classification.

Interrater	k	SE	CI 95%	P
(n=50)				
Total	0.803	0.077	(0.652-0.953)	P<0.001
Intrarrater	k	SE	CI 95%	P
(n=50)				
Rater 1	0.795	0.108	(0.583-1.007)	P<0.001
Rater 2	0.531	0.104	(0.327-0.735)	P<0.001

SE= Standard Error ; CI= Confidence Interval.

5.1. Supplementary material (Training material for raters).

Appendix A. Written description of the gait consensus classification for children with Cerebral Palsy.

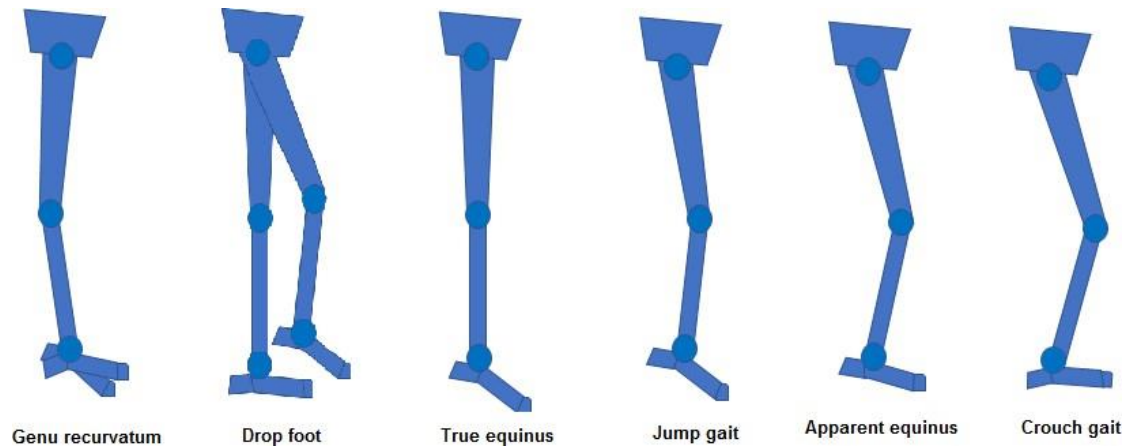


Figure A1. The six multiple joint patterns that displayed a relevant consensus¹.

Multiple joint patterns with consensus

The Gait Classifications Systems (GCS) were initially intended to be applicable to a specific population, either hemiplegic or diplegic CP children.

It was apparent that the multiple joint patterns where agreement was reached have been observed in both populations, further establishing their use in all ambulant children with CP. The literature review revealed that six multiple joint patterns displayed a relevant consensus (Figure A1)¹.

Four out of these six commonly used multiple joint patterns were described in the GCS established by Rodda et al.², who introduced the “true equinus” and “apparent equinus” patterns and extended two patterns originally introduced by Sutherland et al.³.

The patterns “jump gait”, “apparent equinus” and “crouch” can mainly be differentiated from one another based on the position of the ankle joint².

Crouch gait is a pattern not just related of increased knee flexion during stance, knee motion on its own is not sufficient to distinguish crouch from other patterns.

Despite the variability in definitions of these 4 multiple joint patterns, the characteristics presented by Rodda et al. were considered as the most exhaustive

ones, always including information about the co-occurring deviations across all lower limb joints (Table A1).

Apart from these 4 patterns established by Rodda et al.² the literature review also highlighted two additional patterns, namely “drop foot” and “genu recurvatum”.

The “drop foot” appear as a swing phase pattern, there is other gait features in stance (i.e. typical dorsiflexion), as well as minor deviations in other joints (i.e. increased knee flexion at initial contact, during loading response and terminal swing, increased hip flexion during swing and pelvic lordosis throughout the gait cycle).

The patterns “genu recurvatum” describes a knee motion towards or in hyperextension with reduced dorsiflexion and possibly but not necessarily-plantarflexion in the ankle.

Table A1. Definition of gait parameter of the Gait Classification System from the consensus of Papageorgiou et al.¹

Sagittal Kinematics				
Gait Pattern	Pelvic tilt	Hip fx/Ext	Knee Fx/Ext	Ankle Df/Pf
Genu Recurvatum	Normal Anterior	Normal Flexed	Towards or in Hyperext.	Reduced dorsiflexion or plantarflexion
Drop Foot	Normal or Minor deviations	Normal or Minor deviations	Normal or Minor deviations	Plantarflexion during the swing phase
True Equinus	Normal Anterior	Normal	Normal	Plantarflexion
Jump Gait	Normal Anterior	Normal Flexed	Flexed	Plantarflexion
Apparent Equinus	Normal Anterior	Flexed	Flexed	Normal
Crouch Gait	Anterior Normal Posterior	Flexed	Flexed	Excessive dorsiflexion

Hip fx/Ext: hip flexion and extension; Knee Fx/Ext: knee flexion and extension; Ankle Df/Pf: ankle dorsiflexion and plantarflexion; Hyperext: hyperextension.

Genu recurvatum

Full knee Ext or hyperextension (HE) during stance, with almost typical hip motion during stance and impaired ankle motor control, resulting in plantarflexion (PF) or reduced dorsiflexion (DFL) (Figure A2).

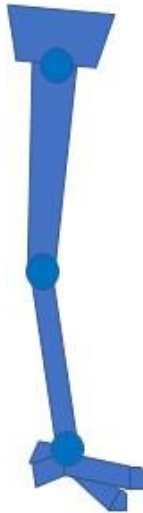


Figure A2. Schematic drawing of the genu recurvatum gait pattern.

Drop foot

Drop foot during swing but adequate DFL range of motion (ROM), increased knee flexion (FL) at terminal swing (TSw), initial contac (IC) and loading response, hip hyperflexion (HFL) during swing and increased lordosis throughout the gait cycle (GC) (Figure A3).



Figure A3. Schematic drawing of the drop foot gait pattern.

True equinus

Ankle in equinus during stance, full knee Ext, full hip Ext, pelvis within typical ROM or anterior tilt (Figure A4).



Figure A4. Schematic drawing of the true equinus gait pattern.

Jump gait

Ankle in equinus, particularly in late stance. Knee and hip in HFL in early stance, followed by Ext to a variable degree in late stance, pelvis within typical ROM or anterior tilt (Figure A5).



Figure A5. Schematic drawing of the jump gait pattern.

Apparent equinus

Ankle typical ROM, knee and hip in HFL throughout stance, pelvis within typical ROM or anterior tilt (Figure A6).



Figure A6. Schematic drawing of the apparent equinus gait pattern.

Crouch gait

Ankle in excessive DFL throughout stance, knee and hip in HFL, pelvis in normal ROM, anterior or posterior tilt (Figure A7).



Figure A7. Schematic drawing of the crouch gait pattern.

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Appendix B. Orientation of how to use the classification system (PowerPoint presentation for the raters).

Orientation of how to use the Classification System

Gait consensus classification for children with Cerebral Palsy

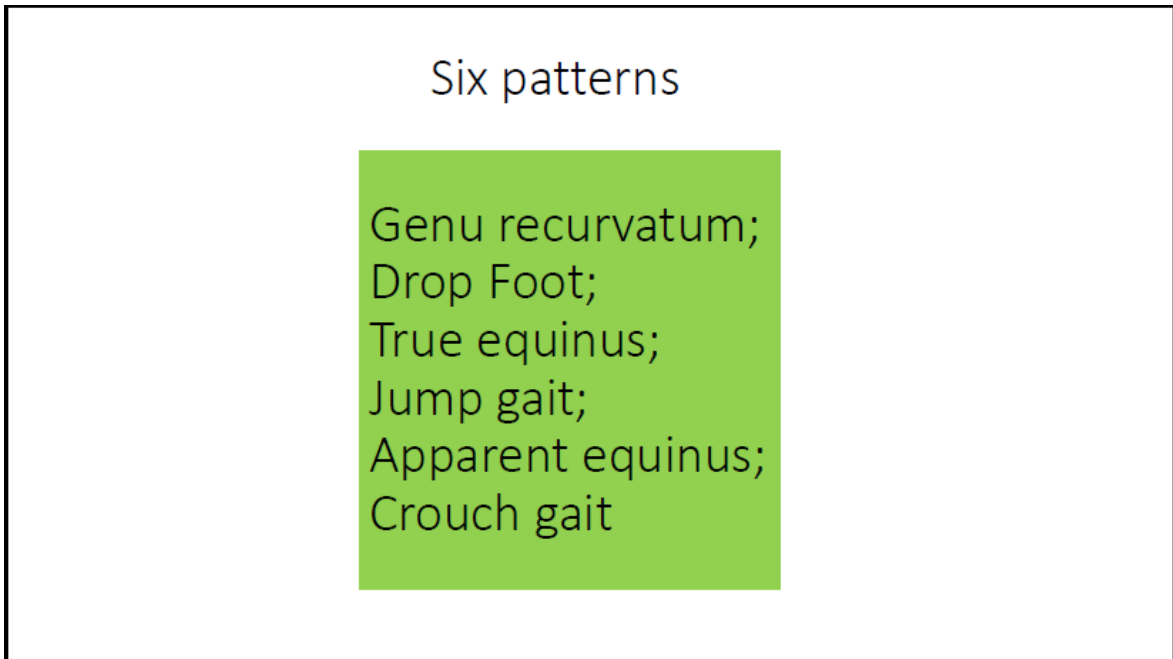
Papageorgiu's classification, 2019

Slide B1. Orientation of how to use the classification system.

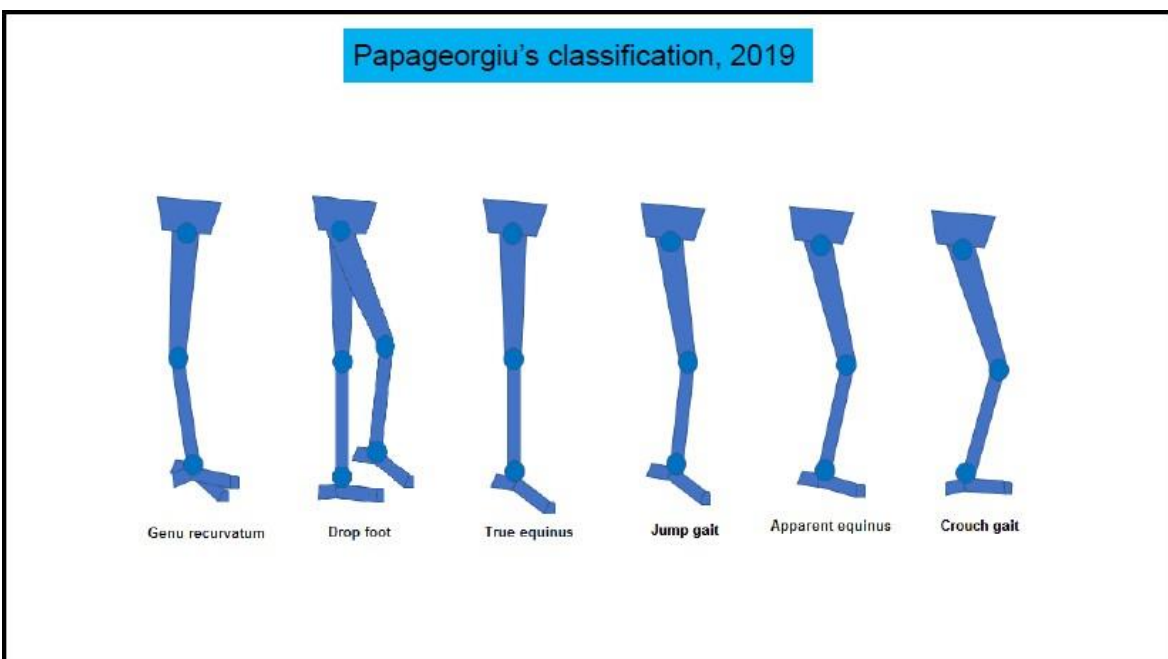
How to proceed

- 1- Printing the classification and guidelines can help during the task of filling out the protocols.
- 2- Complete the classification protocol using videos and graphics (kinematics).

Slide B2. How to proceed to classify the sample of children.



Slide B3. Six gait patterns.



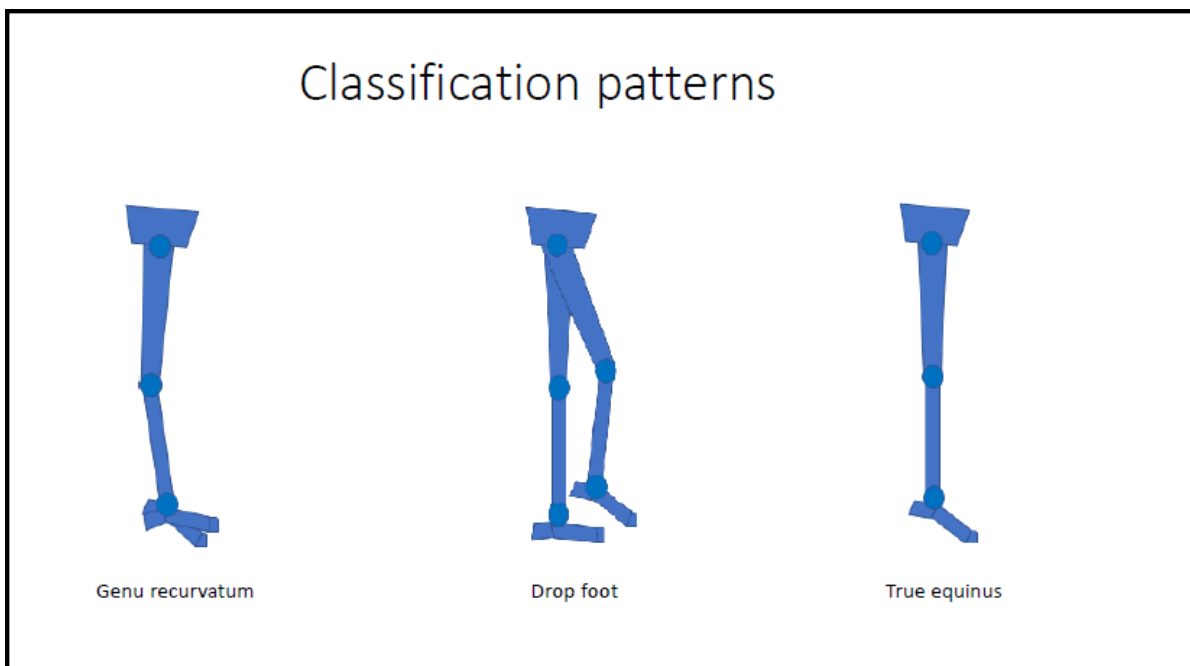
Slide B4. Schematic drawing of the gait patterns of the classification

Papageorgiu's classification, 2019

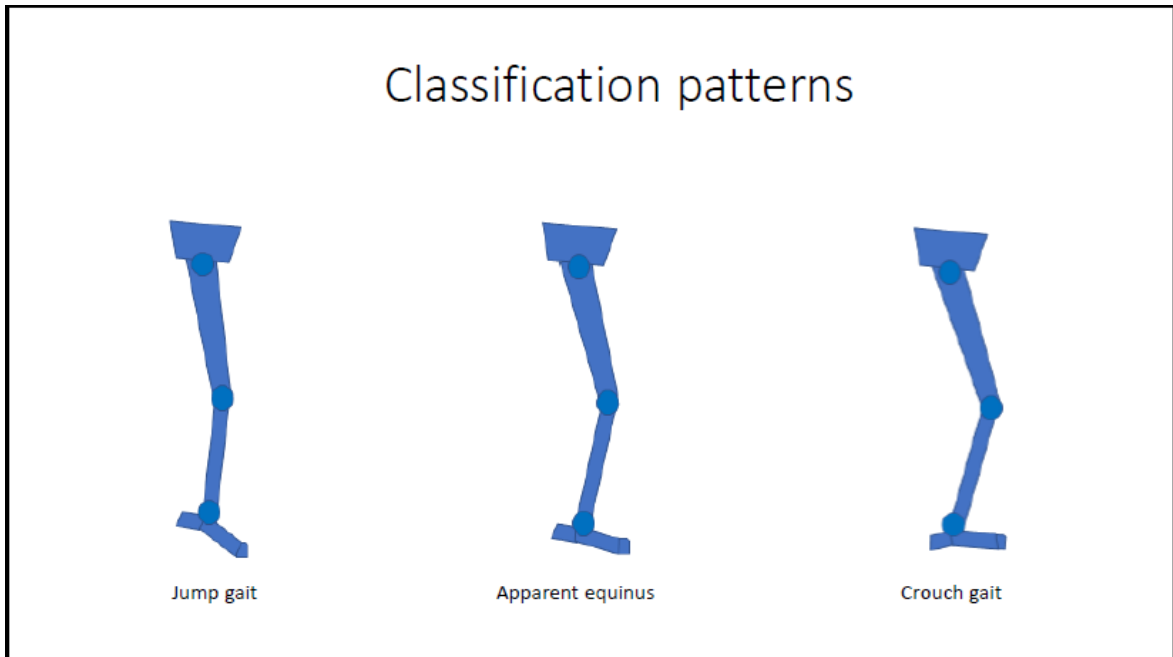
Gait Pattern	Sagittal Kinematics			
	Pelvic tilt	Hip fx/Ext	Knee Fx/Ext	Ankle Df/Pf
Genu Recurvatum	Normal Anterior	Normal Flexed	Towards or in Hyperext.	Reduced dorsiflexion or plantarflexion
Drop Foot	Normal or Minor deviations	Normal or Minor deviations	Normal or Minor deviations	Plantarflexion during the swing phase
True Equinus	Normal Anterior	Normal	Normal	Plantarflexion
Jump Gait	Normal Anterior	Normal Flexed	Flexed	Plantarflexion
Apparent Equinus	Normal Anterior	Flexed	Flexed	Normal
Crouch Gait	Anterior Normal Posterior	Flexed	Flexed	Excessive Dorsiflexion

Slide B5. Definitions of the gait patterns.

Classification patterns



Slide B6. Schematic drawing of the gait patterns: genu recurvatum, drop foot and true equinus.



Slide B7. Schematic drawing of the gait patterns: jump gait, apparent equinus and crouch gait.

Excel spreadsheet protocol

participant	right side	left side
1		
2		
3		
4		
5		
6		
7		
8		
9		
10		
11		
12		
13		
14		
15		
16		
17		
18		
19		
20		
21		
22		
23		
24		
25		

Use one of the options below to fill the protocol, for both the right and left side of each participant of the study.

Genu recurvatum;
Drop Foot;
True equinus;
Jump gait;
Apparent equinus;
Crouch gait.

Not rated;
Without abnormalities.

The authors named the participant as asymmetrical, when the evaluator classified the participant in different pattern the right and left sides.

Slide B8. Example of excel spreadsheet protocol.

Final Orientation

Finalize the filling of the excel spreadsheet and send to the authors.

Slide B9. Final guidance for evaluators.

6 ARTIGO 3

Artigo original formatado de acordo com as normas do periódico Journal of the American Academy of Orthopaedic Surgeons (JAAOS).

Fator de Impacto: 2.286

Title:

Reliability and validity of the Gait Disruption Classification System in Children with Cerebral Palsy (GDSCS-CP).

Authors

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Abstract

Background: Gait classifications systems (GCS) may enable clinicians to differentiate gait patterns into clinically significant categories that assist in clinical decision-making and assessment of outcomes. In 2014, Davids and Bagley described a GCS for children with cerebral palsy (CP); the purpose of our study was to use it for the first time on a sample of patients with CP and to evaluate the reliability and utility of the classification system.

Methods: The gait of 131 children with CP was retrospectively reviewed and classified according to Davids and Bagley's 2014 classification, using 2D video and 3D lower limb kinematics and kinetics. GMFCS levels was determined and the GPS calculated to characterize the sample in relation to gait classification. The comparison between the groups was performed using the Kruskal-Wallis test, in accordance with the non-normal distribution of the data. The intrarater and interrater reliability of the classification was determined using the Kappa index (k) statistics with 95% CI.

Results: All GDCS-CP groups were represented within the evaluated sample. Of the 131 cases evaluated, 127 (96.95%) were able to be classified with respect to sagittal plane stance phase gait deviations. All patients in the sample were able to be classified with respect to sagittal plane swing phase and transverse plane gait deviations. The interrater reliability was 0.596 and 0.485, for the first and second levels of the classification, respectively, according to the Fleiss's Kappa statistics. Intrarater reliability was 0.776 and 0.714 for the raters one and two, respectively, according to the Cohen's Kappa statistics.

Significance: The GDCS-CP exhibited clinical utility, successfully classifying almost all of the subjects with CP, based upon kinematic and kinetic data. The classification is valid and has moderate interrater and moderate to substantial intrarater reliability.

Keywords: cerebral palsy, children, gait, gait analysis, classifications.

Level of Evidence: Level III diagnostic

1. Introduction

Spastic cerebral palsy (CP) is one of the most challenging disorders, because many different clinical variables play a role in the expression of this static brain injury¹. The primary disorder in the brain is associated with abnormal muscle tone, most often hypertonia, accompanied by loss of selective voluntary motor control, muscle weakness, and impaired balance². Hypertonia and the limited use of muscles due to developmental delay result in dynamic muscle–tendon contractures, which become static joint contractures over time as the tight muscles fail to grow in proportion to the long bones, which they traverse. The growing skeleton remodels in response to typical stresses associated with the motor milestones, which when delayed, or absent, result in retention of infantile morphology and development of secondary bone deformities and joint instability, which contribute to lever-arm dysfunction³.

There is pronounced individual variety of movement patterns in ambulatory children with CP¹. The abnormal gait is observed in a wide variety of patterns, depending on the severity of neurologic and motor impairments⁴.

Three-dimensional gait analysis (3DGA) serves as a gold standard to objectively evaluate pathological gait in children with CP⁵.

To support the clinical understanding of gait data, many attempts have been made to identify and classify gait deviation patterns from kinematic and kinetic data, using both qualitative and quantitative approaches⁵.

As reviewed by Dobson et al., qualitative and quantitative strategies for gait classification construction can be distinguished⁶. Qualitative strategies are defined as methods which are experiential and intuitive, distinguish clinically relevant groups, but are frequently limited by their subjective nature and poor reliability^{6,7}. Quantitative strategies, which are systematic and analytical, use varying methods of objective data reduction and classification techniques to preprocess 3DGA data, which unfortunately may have limited clinical utility^{8,9}.

Using computerized three-dimensional (3D) motion analysis has made it possible to identify the similarities and differences within abnormal gait patterns that manifest in patients with CP⁴. Due to the large amount of information produced by movement laboratories using 3DGA, gait classification systems (GCS) have been developed for specific diseases, which simplifies interpretation and facilitates clinical decisions⁹. However, the current classifications of gait for CP have significant

limitations, either in their ability to point out deviations in all planes of movement or in their reproducibility⁶.

Utility of GCSs for individuals with CP is based upon: the classifications can be applied to the gait of patients with unilateral and bilateral involvement; they consider deviations in multiple levels and planes of movement; they include, where appropriate, kinetic and electromyography data; and take into account the use of assistive devices used by people with greater functional impairment and more complex movement disorders^{10,11}. Thus, as with any clinical classification system, GCSs should be useful by facilitating communication among health professionals, assisting in therapeutic decisions and comparing results, treatments or natural history.

In 2019, Papageorgiou et al. carried out a systematic review of the literature on the subject of GCSs for children with CP, and determined that to assess the classifications, information related to validity, reproducibility and clinical applicability was necessary¹².

Among the GCSs evaluated by Papageorgiou et al., the one proposed by Davids and Bagley presented positive characteristics in its construction and significant clinical applicability^{10,12}. However, it had not been tested on a sample of subjects with CP. Therefore, the purpose of this study was to validate the existing “Gait Disruption Classification System in Children with Cerebral Palsy (GDCCS-CP)” as described by Davids and Bagley by evaluating its usefulness in a defined population of children with CP¹⁰. The study focused on exploring whether this classification covered all potential patterns in children with spastic CP, regardless of unilateral and bilateral involvement. The secondary objective was to evaluate the intra and inter-observer reliability of the classification.

2. Methods

2.1. Study design

This study was conducted as a retrospective study after the project was approved by a local research ethics committee under opinion 2.447.001. The study was developed by an estimated sample of 115 individuals considering the prevalence of 0.3% [3] and maximum standard error of 1%. The search conducted from the database of the Gait Analysis Laboratory at the Ana Carolina de Moura Xavier Rehabilitation Hospital Center in Curitiba, Paraná, Brazil, provided a sample of 131

children who had undergone gait analysis with a diagnosis of spastic cerebral palsy. Written informed consent was obtained from all participants.

The study was performed in two stages. The first was a cross-sectional study classifying gait patterns in children with CP using the GDCS-CP. The second stage was to investigate the intra and inter-observer reliability of the classification¹⁰.

2.2. Participants

Eligible participants were between five and nineteen years old, classified as GMFCS levels I to IV, and predominantly had spastic CP. Previous treatments such as single event multilevel surgery or botulinum toxin type A injections were acceptable within the sample.

All participants underwent a 3DGA under barefoot (BF) walking conditions at a self-selected speed, during a single visit to the gait analysis laboratory. They received no remuneration for participation.

2.3. Cross-sectional study

The sample group comprised of 131 patients who fulfilled the study criteria and were classified according to the GDCS-CP¹⁰, by one rater with wide clinical experience in gait analysis. After classifying the sample, the groups formed were compared in terms of age, GPS and gait velocity.

2.4. Reliability study

A training program was developed, in which all raters attended and participated in an online presentation, to discuss the classification's structure, and to present examples that illustrated how to classify cases using the GDCS-CP. The raters were provided with written definitions and illustrations of the posture of the ankle, knee, hip and pelvis for each gait pattern in relation to the planes of motion (supplementary material). Each rater was supplied with a package that included a pen drive, standardized information which included definitions of the classification categories, as well as videos and 3DGA data from the participants included in the study.

To determine interrater reliability, 60 participants diagnosed with ambulatory CP who had had 3DGA were evaluated by four raters, two pediatric orthopedic surgeons and two physiotherapists who all had experience in gait analysis. To determine intrarater reliability two of the evaluators (randomly selected) evaluated 30 participants

from the group that would later be assessed a second time, a month after the initial assessment. The cases with their 3DGA and corresponding videos were selected to create a sample that included variation in age and levels of motor impairment (as reflected by the GMFCS).

Intra and interrater reliability were calculated for the first and second levels of the GDCS-CP.

2.5. Measurements

Each participant's gait was recorded on video, using sagittal and coronal views. Instrumented 3DGA was performed using the conventional gait model (Helen-Hayes model)¹³, with reflective markers (n =26), to obtain spatiotemporal parameters (step and stride lengths, cadence, walking velocity) and lower extremity kinematics and kinetics at the pelvis, hip, knee, and ankle. 3D kinematic and kinetic gait data were collected bilaterally using 6 digital motion analysis cameras (Motion Analysis Corporation in Santa Rosa, CA) sampling at 60 Hz, alongside two force plates (AMTI Biomechanics Force Plate OR6-7 2000 - Watertown, MA, USA) sampling at 1000 Hz. Joint kinematics and external movements were calculated by the Cortex software (Motion Analysis Corp., Santa Rosa, CA). The data was processed using OrthoTrack software (OrthoTrack 6.5.1 software, Reference Manual 2007. Motion Analysis Corporation, Santa Rosa, CA). The data were smoothed using a Butterworth filter with a cut-off frequency of 6 Hz. The motion analysis system was calibrated before each analysis. All kinematic and kinetic data were time-normalized to 100 % of one gait cycle.

3DGA kinematics were used to calculate the GPS, which quantifies the overall deviation of an individual's gait from normal gait¹⁴

The kinematic and kinetic data were collected from a minimum of 7 gait cycles for each assessed leg and the most representative trial was reported, alongside the corresponding video clips, and classified according to the GDCS-CP¹⁰. Kinetic data was not collected for participants who used walking aids, typically GMFCS III and IV. Children who presented an asymmetrical gait pattern, which resulted in classification on one lower limb side which differed from the other, were excluded from the analysis of GPS.

The GMFCS was assigned by a senior clinical physiotherapist and a pediatric orthopedist in consultation with the child and his or her parents.

2.5.1 Description of the gait classification categories.

The gait parameters of the GDSC-CP, for the sagittal plane in stance and swing phases, and the transverse plane, are summarized in Table 1. For the sagittal plane stance phase, the first level of distinction is between normal, jump, and crouch gait (based upon kinematic data). Jump gait is then subdivided into the second level as either true equinus or apparent equinus (based upon kinematic data). Crouch gait is subdivided into compensated and uncompensated patterns; in the former, the internal knee extensor moment is normal, while in the latter there is increased internal knee extensor moment throughout the stance phase (based upon the kinetic data). For the sagittal plane swing phase, the first level of distinction is between normal gait and stiff gait (based upon kinematic data). The stiff gait is subdivided into knee source and hip source. Stiff gait-knee source had a fast flexion of the hip during the transition from stance to swing phase, unlike hip source that had a slow slope of the hip flexion during the transition phases. The transverse plane is classified in a hierarchical manner, with the first level of distinction including internal, external, and neutral foot progression patterns (based upon the kinematic data). Both internal and external progression patterns are subdivided into single-level and multilevel patterns. The neutral progression pattern is characterized by a neutral foot-progression angle (i.e., orientation of the long axis of the foot that is comparable to the line of progression of gait) and subdivided into normal and offset patterns, with the latter due to internal rotation of the hip compensated for by increased external tibial torsion¹⁰.

2.6. Statistical Analysis

Descriptive data was presented as means and standard deviations or as medians and interquartile ranges, according to normal distribution, and analyzed using the Shapiro-Wilk test. The Levene test was used to verify the homogeneity of variances. The comparison between the groups was performed using the Kruskal-Wallis test and Mann-Whitney's post hoc test, in accordance with the non-normal distribution of the data. The level of significance was set at $p < 0.05$.

The reliability of the classification was determined using Kappa index statistics with 95% CI, used to describe intra and inter-observer agreement with the following reference values: equal to zero, "without agreement"; between zero and 0.19, "poor agreement"; from 0.20 to 0.39, "weak agreement"; from 0.40 to 0.59, "moderate

agreement"; from 0.60 to 0.79, "substantial agreement"; from 0.80 to 1.00, "almost perfect agreement"¹⁵. Fleiss's Kappa was used for interrater reliability and Cohen's Kappa for intrarater.

The analyses were performed using IBM SPSS Statistics for Windows, version 22.0 (IBM Corp., Armonk, N.Y., USA).

3. Results

3.1 Cross-sectional study study

The sample consisted of 131 subjects with spastic CP, 70 being male (53.43%) and 61 being female (45.56%); 116 with bilateral and 15 with unilateral CP. The median age was 12 [10-15] years. Considering the distribution of participants according to the GMFCS classification, most participants were included in the GMFCS II - 83, followed by the GMFCS III - 24, GMFCS I - 20 and GMFCS IV - 4. Participants at GMFCS III, 12 used walkers, 9 used crutches and 2 used canes.

There were no statistically significant age differences between the classification groups (Table 2). The GPS showed differences between the normal group and the other groups in the sagittal stance phase. The GPS in the transverse plane was different between neutral normal and neutral off-settings, as well as between neutral normal and external multilevel. The normal group exhibited the lowest GPS values in both situations, 10.8° [9.09 - 12.15], and 11.8° [10.04-13.88].

All the groups within the classification were represented in the evaluated sample. Of the 131 cases evaluated, 127 (96.95%) were able to be classified according to the GDCS-CP proposed for the stance phase of the sagittal plane. All patients in the sample were able to be classified according to the GDCS-CP proposed for both the swing phase of the sagittal plane and the transverse plane.

Across the gait patterns, from the true equinus to crouch gait, there were changes between the anatomical levels from equinus to excessive dorsiflexion of the ankle and increase of knee flexion from apparent equinus to crouch gait (Figure 1). In the non-compensated crouch pattern, there was an increase in the knee extensor moment in the stance phase.

The stiff gait presented a delayed and diminished peak knee flexion in the swing phase (Figure 1). The stiff gait hip source group manifested slower overall gait velocity than the normal and stiff gait/knee source ($p=0.015$) (Table 2).

The internal, external and neutral positions are clearly illustrated by the angle of progression of the foot as observed in Figure 2. On the other hand, there was an overlap between the subdivisions single and multi-level of the internal and external, as well as neutral normal and offset positions (Figure 2).

3.2 Reliability

The overall interrater reliability of the four raters for the first level of the GDSCS-CP was 0.596 (0.562-0.631) and 0.485 (0.461-0.509) for the second level of the classification according to the Fleiss's Kappa statistics. The interrater reliability for each plane of the first and second levels of the classification are presented in Table 3.

Intrarater reliability of the first level of the classification was 0.888 (0.827-0.949) and 0.791 (0.709-0.873) for raters 1 and 2, respectively, according to the Cohen's Kappa statistics. Intrarater reliability of the second level of the classification was 0.776 (0.706-0.846) and 0.714 (0.634-0.794) for raters 1 and 2, respectively, according to the Cohen's Kappa statistics. The Intrarater reliability for both raters, for each plane of the first and second levels of the classification, are presented in Table 4.

4. Discussion

The gait classifications for CP have shown limited ability to point out gait deviations in the various planes of movement. As a result, they have limited utility for clinical decision making, outcome assessment, and research⁶.

This is the first study to evaluate the performance of the CDCG-CP. The GDSCS-CP showed utility in successfully classifying a large sample of individuals with CP, based upon sagittal and transverse kinematics at the ankle, knee, hip and pelvis; and sagittal plane kinetics of the knee. Measurement validity, and clinical utility, consider the extent to which an instrument measures what it is intended to measure¹⁶; and the GDSCS-CP showed an ability to classify the gait of children with CP more completely than previous qualitative classifications¹⁷⁻¹⁹.

The present classification uses a progressive hierarchy of the motor dysfunction gait patterns seen in children with CP to classify observed problems, allocating the alterations in the stance and swing phase of the sagittal and transverse planes. As the GDSCS-CP is more inclusive and specific, as it offers the rater a greater number of options to allocate the deviations observed in an individual with CP, content validity

was examined to provide objective evidence for the existence of joint motion patterns in CP classified as problem and as normal. To assess the ability of the classification to differentiate gait problems from normality, GPS was used. The GPS showed a statistically significant difference, in the stance phase of the sagittal plane, between the subjects classified as normal in relation to all groups in the GCDS-CP. The GPS showed no difference in the swing phase GCDS-CP groups, probably because these groups consisted of individuals with categorization of problems at a single anatomic level (the knee) during a relatively small portion of the gait cycle. However, the overall gait velocity of patients in the stiff gait/hip source group was slower and statistically different from the stiff gait/knee source, and the normal group, in the swing phase.

The classification did not consider the coronal plane because the authors of the classification¹⁰ believe that true coronal plane gait disruption patterns in children with CP are less common and are generally of minimal magnitude and functional significance. According to Nieuwenhuys et al., there were no significant associations identified with any of the investigated variables in the coronal plane, leading these investigators to question their clinical relevance and the need to include them in gait classification schemes for children with CP²⁰.

Of the four unclassifiable participants, all had a jump gait pattern²¹ at the knee, but increased ankle dorsiflexion in the stance phase. The pattern was named "crump" by one of the authors (JRD), due to the mix of crouch and jump gait parameters, who has characterized it as a transitional pattern between jump and crouch gait, which occurs as the foot equino plano valgus segmental malalignment and instability progress, resulting in lever arm deficiency for the ankle plantar flexors.

The GCDS-CP exhibited moderate to substantial intrarater reliability. The interrater reliability was moderate, even when only the first level of the classification was assessed. The explanation for the moderate interrater reliability of the GCDS-CP can be related to lack of sharp demarcations between the various patterns. This can be seen in Figures 1 and 2, which show overlap between the movements of several joints with similar features. However, in many biomedical studies, reliability of greater than 40% ($k > 0.40$), is considered to be a clinically useful method of measurement²². The transverse plane had the lowest reliability, and again the explanation seems to be clear when looking at Figure 2, which shows significant overlap between the curves of the neutral normal and offset, internal single and multilevel, as well as external single

and multilevel, subgroups. In the future, improved gait pattern definitions and classification training materials may result in improved reliability metrics.

Some limitations should be considered. Most of the participants in the study were referred for gait analysis for preoperative evaluation to improve ambulatory function. The walking velocity was not controlled during gait testing. Therefore, some deviations, such as stiff knee gait, may have been related to slow walking speed. Some patients used assistive devices during gait analysis testing, which could have impacted kinematic and kinetic data collection.

5. Conclusion

The GDACS-CP provides a powerful methodology to categorize gait patterns in children with CP, using kinematic data for multiple joints from more than one plane of movement, and kinetic data from a single joint in a single plane. It appears to be applicable for subjects with unilateral and bilateral CP. The validity and utility of the classification, in this study, has been established by its ability to classify the sample of individuals with CP, through data from 3DGA. The classification shows that, even with limited learning, evaluators will be able to use it. However, a more quantitative delineation of the categories, and improved training materials, may be required to improve reliability among raters.

Author contribution statement

Alessandro G. Melanda (Conceptualization) (Methodology) (Validation) (Formal Analysis) (Investigation) (Data Curation) (Writing – Original Draft) (Writing – Review & Editing) (Visualization) (Supervision).

Jon R. Davids (Conceptualization) (Writing – Review & Editing) (Visualization)

Ana C. Pauleto (Writing – Review & Editing) (Visualization).

Alana EK Ferreira (Writing – Review & Editing) (Visualization).

Alexandre R M Pelegrinelli (Data Curation) (Writing – Review & Editing) (Visualization).

Luiz Alberto Knaut (Methodology) (Validation) (Formal Analysis) (Visualization)

Suhaila Mahmoud Smaili (Conceptualization) (Formal Analysis) (Writing – Review & Editing) (Visualization) (Supervision).

All authors have read and approved the final manuscript.

Declaration of Competing Interest

All authors declare that they have no conflicting interests. This research did not receive any specific grant from funding agencies in the public, commercial, or not-for-profit sectors.

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Not applicable.

Supplementary material

Appendix A. Written orientation for raters (definitions).

Appendix B. Orientation for the raters (how to use the files).

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Table 1. Definition of the gait parameter of the GDCS-CP, sagittal plane in the stance and swing phases, and the transverse plane.

Kinematics				
Sagittal Plane	Pelvic tilt	Hip Fx/Ext	Knee Fx/Ext	Ankle Df/Pf
True Equinus	Normal Anterior	Normal Excessive extension Flexion	Normal Excessive extension Flexion	Plantarflexion
Apparent Equinus	Normal Anterior	Flexed	Flexed	Normal
Crouch Gait Compensated [^]	Anterior	Flexed	Flexed (more than 30° in the stance)	Excessive dorsiflexion
Crouch Gait Uncompensated*	Normal Posterior	Flexed	Flexed (more than 30° in the stance)	Excessive dorsiflexion
Stiff Gait knee source		hip profile in the stance-to-swing interval is normal	delayed and diminished peak knee flexion in swing phase (<45° flexion)	
Stiff gait hip source		hip profile in the stance-to-swing interval is abnormal (slow)	Delayed and diminished peak knee flexion in swing phase (<45° flexion)	
Transverse plane	Pelvic rotation	Hip rotation	Knee rotation	Foot progression
Neutral normal	neutral	Neut/ext	Neut/ext	Neutral
Neutral off-settings	Neut/ext/int	Internal	External	Neutral
Internal single/multilevel	Neut/ext/int	Neut/int	Neut/int	Internal
External single/multilevel	Neut/ext/int	Neut/ext	Neut/ext	External

Hip fx/Ext: hip flexion and extension. Knee Fx/Ext: knee flexion and extension. Ankle Df/Pf; ankle dorsiflexion and plantarflexion. Hyperext.: hyperextension. Neut/ext/int= neutral, external, internal.

[^] = normal internal extensor moment during stance phase

* = increase internal extensor knee moment during stance phase.

Table 2. Median and interquartile range of age, GPS and velocity, according to the sagittal stance phase, the sagittal swing phase and the transverse plane of the gait patterns.

Stance phase Sagittal Plane							
Gait pattern/ variables	Normal n = 21	Jump gait [true equinus] n = 15	Jump gait [apparent equinus] n = 42	Crouch gait Compensated n = 5	Crouch gait Uncompensated n = 8	Others n = 4	P
Age (years)	12.50 [9.75 – 14.00]	10.00 [8.00 – 10.00]	11.00 [9.50 – 14.00]	14.00 [12.50 – 15.50]	16.00 [12.50 – 17.00]	14.50 [8.75 – 15.75]	0.070
GPS st (°)	10.80 [9.09 – 12.15] ^{a,b,c,d}	13.60 [10.80 – 19.50]	12.90 [11.40 – 15.01]	15.10 [14.17 – 18.27]	16.45 [14.77 – 19.40]	14.08 [12.65 – 17.55]	<0.001
Velocity (cm/sec)	85.55 [71.10 – 107.55]	103.70 [70.30 – 112.40]	88.60 [66.60 – 102.85]	50.30 [36.37 – 82.97]	76.05 [56.17 – 83.65]	75.05 [37.90 – 114.67]	0.406
Swing phase Sagittal Plane							
Gait pattern/ variables	Normal n = 110	Stiff gait Knee source n = 18	Stiff gait hip source n = 3				P
Age (years)	13.00 [10.00 – 15.00]	12.00 [10.00 – 13.50]	14.00 [12.00 – 14.00]				0.926
GPS st (°)	13.70 [11.70 – 17.52]	12.10 [10.75 – 17.31]	18.40 [16.20 – 20.30]				0.125
Velocity (cm/sec)	75.45 [62.05 – 91.30] ^e	89.1 [59.20 – 102.45] ^f	26.10 [20.10 – 26.70]				0.015
Stance phase Transverse plane							
Gait pattern/ variables	Neutral – normal n = 46	Neutral – off setting n = 20	Internal single level n = 41	Internal multilevel n=3	External single level n = 6	External multilevel n=7	P
Age (years)	14.00 [12.00–15.00]	12.00 [10.00 – 14.00]	11.00 [9.00 – 15.00]	10.00 [7.50-10.00]	15.00 [7.50 – 16.50]	14.00 [10.00-16.25]	0.172
GPS st (°)	11.80 [10.04 – 13.88] ^{g,h,i}	14.00 [12.99 – 19.00]	13.70 [11.47 – 18.06]	15.40 [11.20-19.18]	13.90 [13.25 – 15.69]	19.50 [14.50-23.75]	<0,001
Velocity (cm/sec)	89.95 [67.35 – 103.07] ⁱ	74.08 [57.80 – 87.90]	83.10 [61.35 – 99.50] ^j	69.00 [65.20-76.10]	70.20 [44.10 – 82.85]	66.10 [35.00-79.75]	0.004

GPS st: Global Profile Score standard; (°) degrees; GMFCS: Gross Motor Function Classification System; cm/sec: centimeter per second.

a = statistically significant difference between normal and jump knee/true equinus.

b = statistically significant difference between normal and jump knee/ apparent equinus.

c = statistically significant difference between normal and crouch gait compensated.

d = statistically significant difference between normal and crouch gait uncompensated.

e = statistically significant difference between normal and stiff gait hip source.

f = statistically significant difference between stiff gait knee source and stiff gait hip source.

g = statistically significant difference between neutral normal and neutral off-settings.

h = statistically significant difference between neutral normal and external multilevel.

i = statistically significant difference between neutral normal and others.

j = statistically significant difference between internal single level and others.

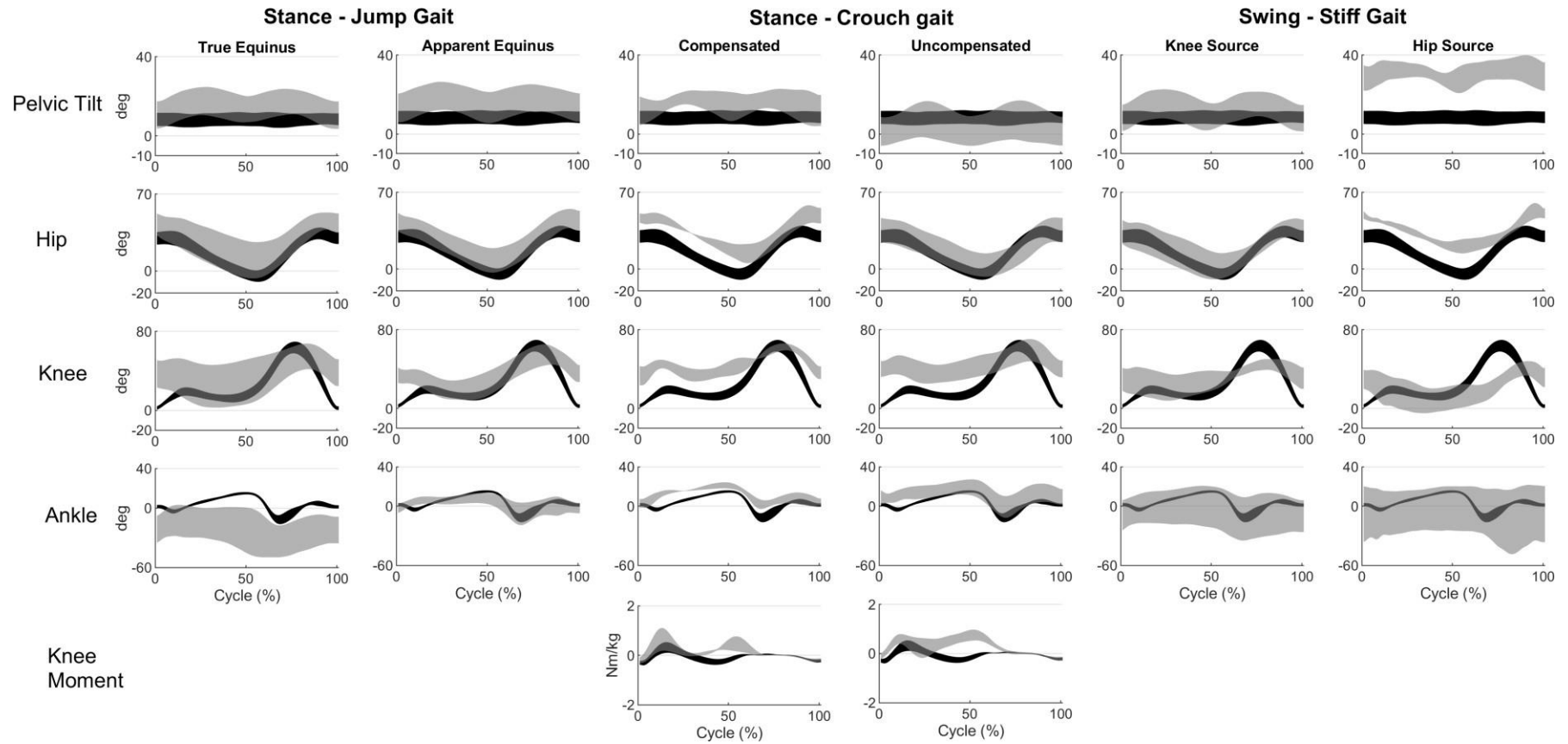


Figure 1. The summarized stance and swing phases of the sagittal plane kinematic data for each gait pattern from the study population. The black band represents the mean \pm 1 SD of kinematic data normal database, and the grey band the mean \pm 1 SD for each gait pattern. The vertical axis represents joint angular displacement and the horizontal axis, 100% of the gait cycle.

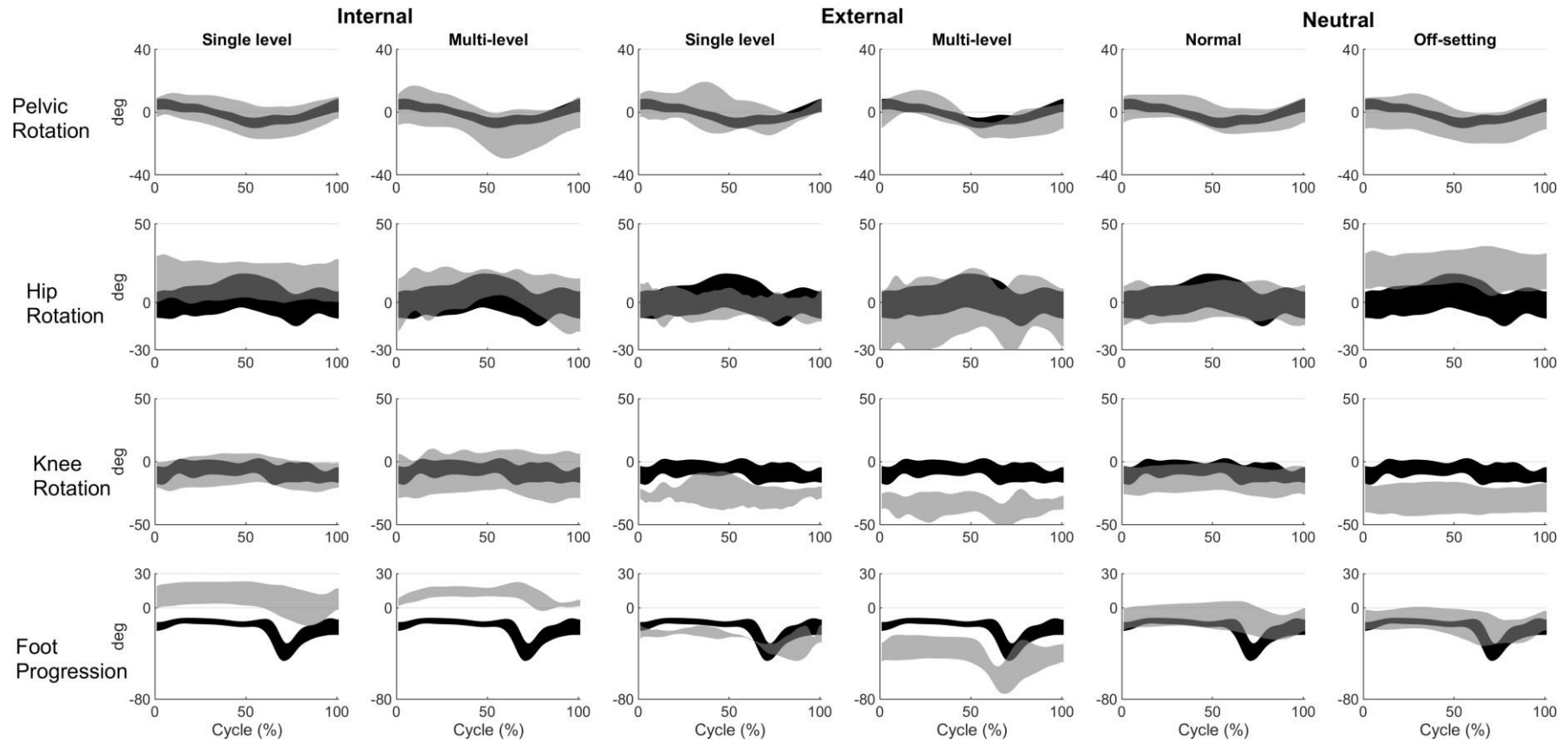


Figure 2. The summarized stance phase of the transverse plane kinematic data for each gait pattern from the study population. The black band represents the mean \pm 1 SD of kinematic data normal database, and the grey band the mean \pm 1 SD for each gait pattern. The vertical axis represents joint angular displacement and the horizontal axis, 100% of the gait cycle.

Table 3. Fleiss's Kappa (κ) statistics with 95% CI for interrater reliability in the first and second level of the classification.

First Level n=60	k	SE	CI 95%	P
Stance sagittal	0.409	0.028	0.355-0.464	<0.001
Swing sagittal	0.570	0.037	0.498-0.642	<0.001
Stance transverse	0.516	0.030	0.456-0.575	<0.001
Total	0.596	0.018	0.562-0.631	<0.001
Second Level n=60	k	SE	CI 95%	P
Stance sagittal	0.434	0.021	0.394-0.475	<0.001
Swing sagittal	0.491	0.032	0.429-0.553	<0.001
Stance transverse	0.275	0.019	0.237-0.312	<0.001
Total	0.485	0.012	0.461-0.509	<0.001

SE= Standard Error; CI= Confidence Interval.

Table 4. Cohen's Kappa (k) statistics with 95% CI for intrarater reliability in the first and second level of the classification.

First Level n=60	Rater	k	SE	CI 95%	P
Stance Sagittal	1	0.913	0.060	0.795-1.000	<0.001
	2	0.797	0.066	0.667-0.926	<0.001
Swing Sagittal	1	0.550	0.226	0.107-0.993	<0.001
	2	0.643	0.188	0.274-1.000	<0.001
Stance transverse	1	0.807	0.067	0.747-0.867	<0.001
	2	0.692	0.089	0.518-0.866	<0.001
Total	1	0.888	0.031	0.827-0.949	<0.001
	2	0.791	0.042	0.709-0.873	<0.001

Second Level n=60		k	SE	CI 95%	P
Stance Sagittal	1	0.760	0.069	0.625-0.895	<0.001
	2	0.743	0.065	0.616-0.870	<0.001
Swing Sagittal	1	0.550	0.226	0.107-0.993	<0.001
	2	0.565	0.193	0.187-0.943	<0.001
Stance transverse	1	0.623	0.073	0.48-0.766	<0.001
	2	0.567	0.076	0.419-0.715	<0.001
Total	1	0.776	0.036	0.706-0.846	<0.001
	2	0.714	0.041	0.634-0.794	<0.001

SE= Standard Error; CI= Confidence Interval.

6.1. Supplementary material (Training material for raters).

Appendix A. Written orientation Classification of Gait Deviations for raters (definitions)

Classification of Gait Deviations – Davids and Bagley – 2014.

- Definition of the classification.
- Figures.
- Graphics – kinematics and kinetics.
- Overview of the classification.
- Protocols.

Gait disruption patterns in the sagittal plane are best classified in a hierarchical manner, with the first level of distinction being between stance phase and swing phase¹.

In stance phase, the first level of distinction is between normal, jump, and crouch gait (Figure A1). The latter two gait patterns are differentiated by the foot contact pattern with the floor. Jump gait is characterized by the loss of heel strike at initial contact, with a toe contact pattern for the duration of the stance phase (Figure A2).

Crouch gait is characterized by a flatfoot or calcaneal contact pattern for the duration of stance phase (Figure A2)². All children with CP and crouch gait will have increased knee flexion throughout stance phase (more than 30° of flexion)³.

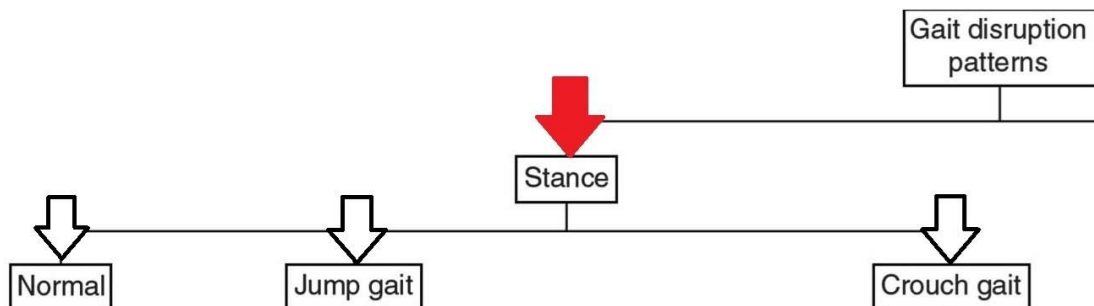


Figure A1. Flowchart of the first level of the classification in the stance phase of the sagittal plane

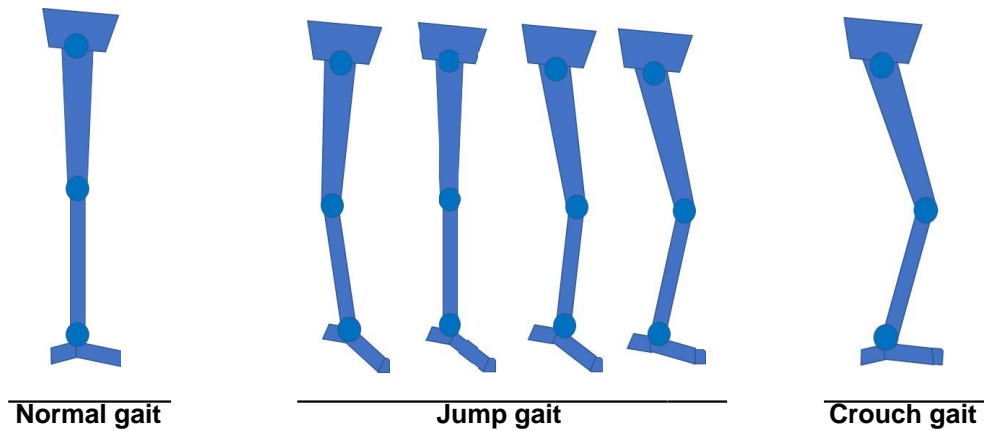


Figure A2. First level of the classification - stance phase of sagittal plane (with permission from the author).

Jump gait may be further subdivided into true equinus and apparent equinus patterns (Figure A3). True equinus is characterized by plantar flexion of the foot relative to the tibia. In apparent equinus, the foot appears to be in plantar flexion (ie, relative to the floor) but is actually normally aligned relative to the tibia (Figure A4).

Crouch gait may be subdivided into compensated and uncompensated patterns, based on sagittal plane knee kinetics (Figure A3). In the compensated pattern, the knee is effectively offloaded in midstance (i.e., reflected by a decreased internal knee extensor moment), despite the increased knee flexion throughout the stance phase (Figure A5).

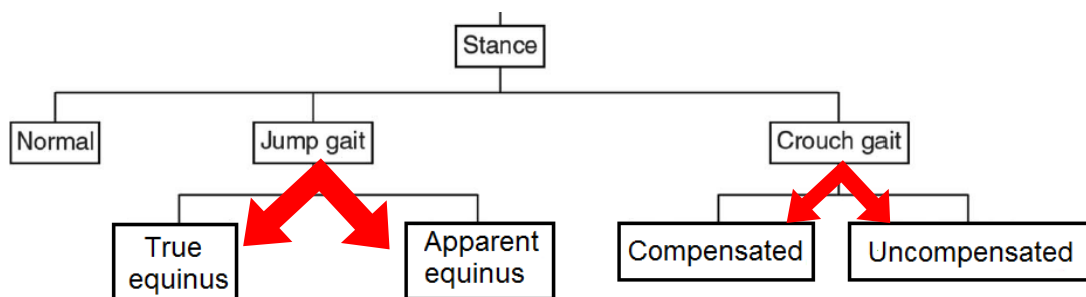


Figure A3. Flowchart of the second level of the classification in the stance phase of the sagittal plane

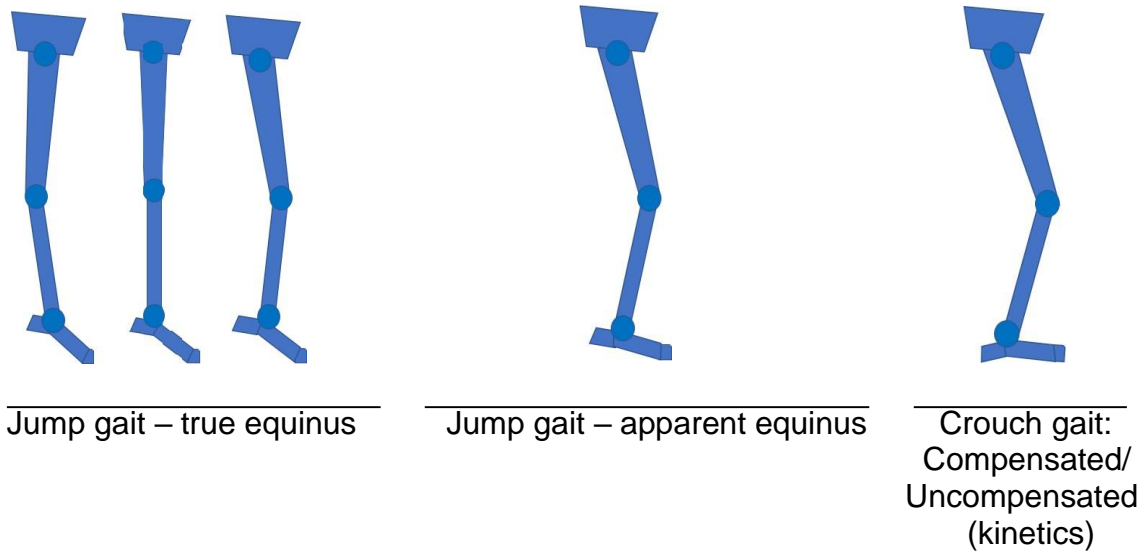


Figure A4. First and second level of the classification - stance phase of sagittal plane (with ask permission from the author).

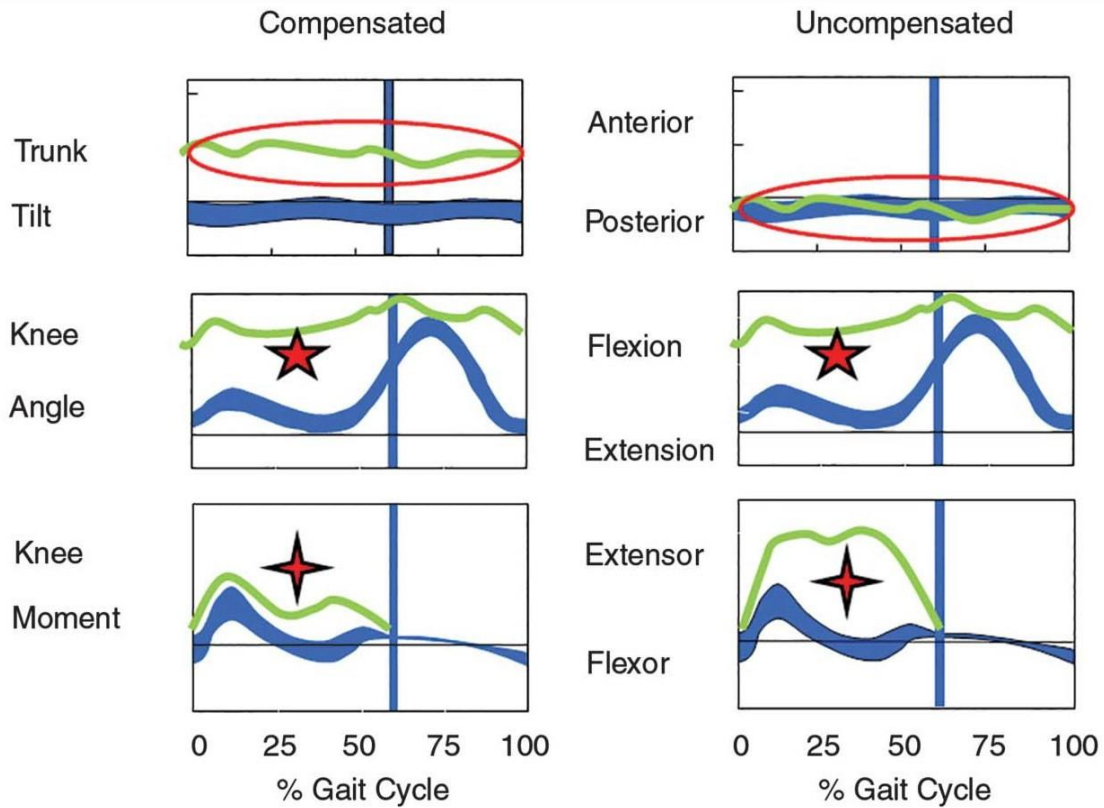


Figure A5. Example of compensated and uncompensated crouch gait (kinematic and kinetic) (with permission from the author).

In swing phase, the first level of distinction is between normal gait and stiff gait (Figure A6). Stiff gait is characterized by delayed and diminished peak knee flexion in swing phase (less than 45° of flexion)³.

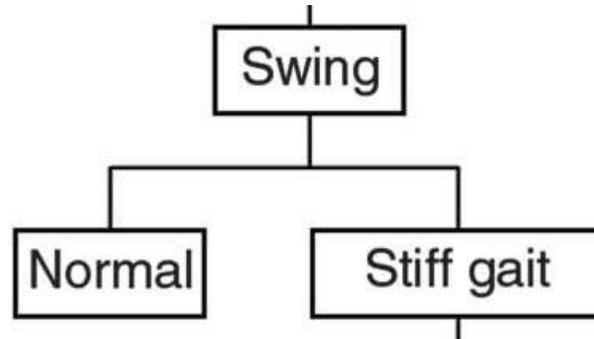


Figure A6. First level of the classification - swing phase of the sagittal plane (with permission from the author).

The stiff gait may be further subdivided into knee source and hip source (Figure A7).

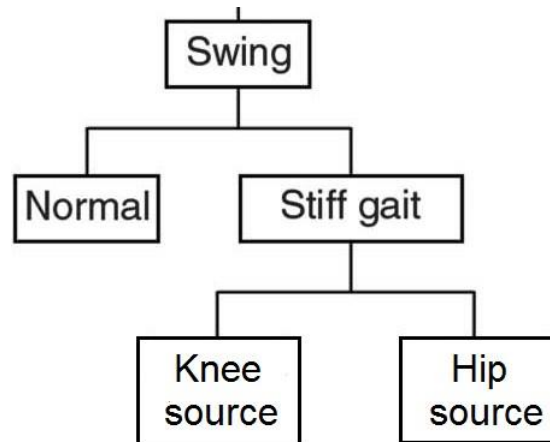


Figure A7. First and Second level of the classification – swing phase of sagittal plane (with permission from the author).

In the stiff gait knee source, the hip profile in the stance-to-swing interval is normal. In the stiff gait hip source, the swing-phase knee deviations are preceded by kinematic (i.e., diminished flexion slope) and kinetic (i.e., diminished internal flexor moment and

decreased power generation) deviations at the hip in terminal stance and pre-swing of the gait cycle (Figure A8).

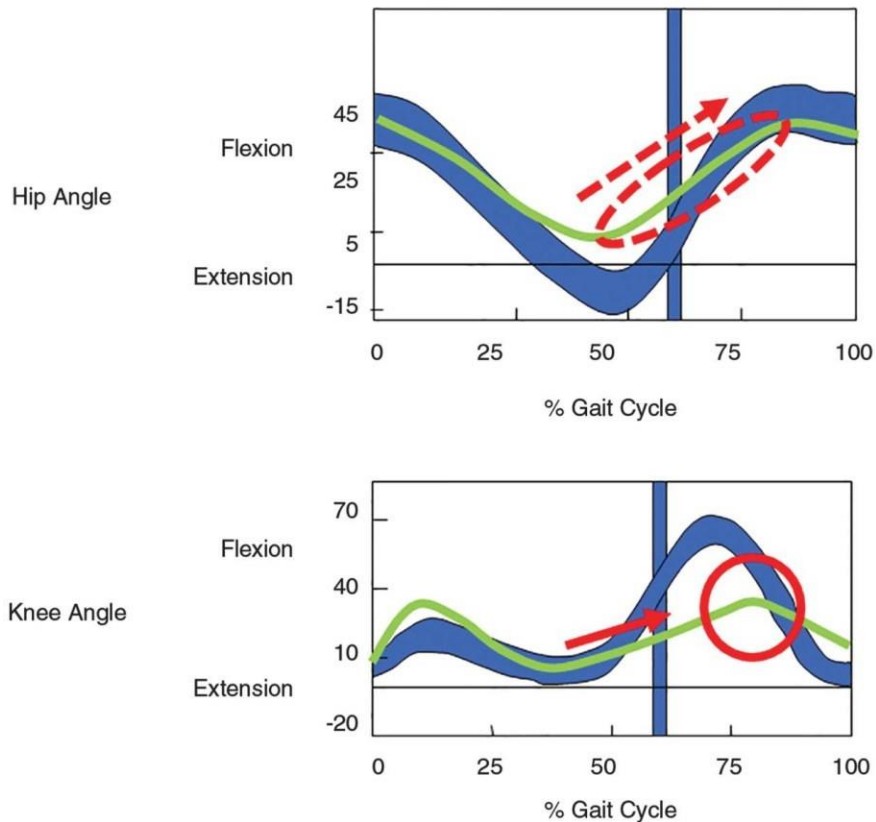


Figure A8. Kinematic of the stiff gait hip source (with permission from the author).

Gait disruption patterns in the transverse plane are best classified in a hierarchical manner, with the first level of distinction including internal, external, and neutral progression patterns (Figure A9). The internal progression pattern is characterized by an internal foot-progression angle (i.e., medial orientation of the long axis of the foot relative to the line of progression of gait). The external progression pattern is characterized by an external foot-progression angle (i.e., lateral orientation of the long axis of the foot relative to the line of progression of gait). The neutral progression pattern is characterized by a neutral foot-progression angle (i.e., orientation of the long axis of the foot that is comparable to the line of progression of gait)

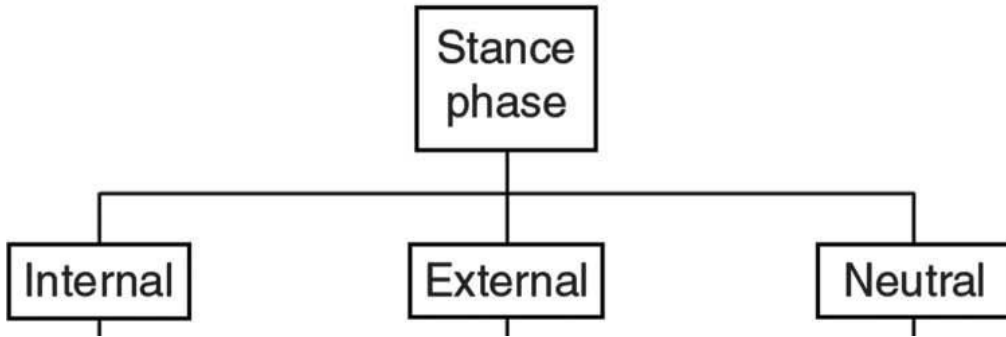


Figure A9. First level of the classification – transverse plane (with permission from the author).

Both internal and external progression patterns may be subdivided into single-level and multilevel patterns (Figure A10).

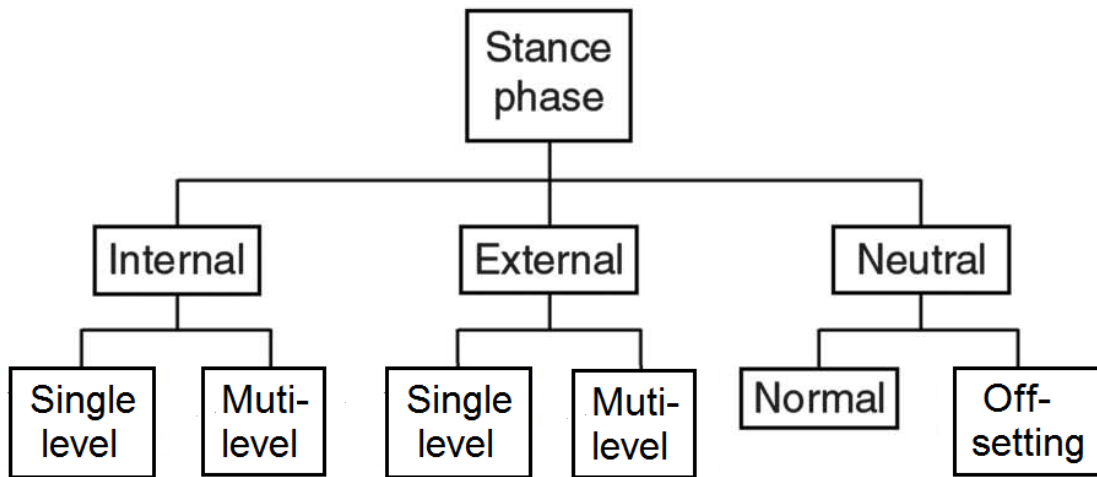


Figure A10. First and second level of the classification – transverse plane (with permission from the author).

The neutral progression pattern can be divided into normal and off-setting patterns (the latter is also known as miserable malalignment) (Figure A11).

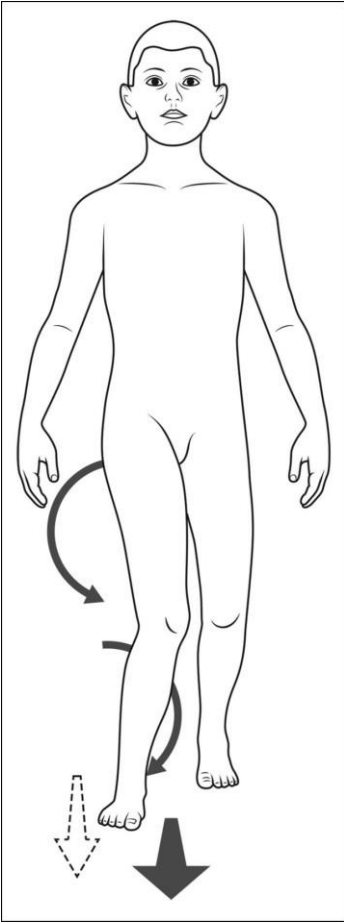


Figure A11. Illustration of the stance phase, neutral progression, gait disruption pattern. The foot-progression angle (dashed arrow) of the reference limb is comparable to the line of gait progression (solid arrow). Internal rotation of the hip, related to increased femoral anteversion (i.e., transverse plane), is offset by external rotation at the knee, related to increased external tibial torsion (i.e., transverse plane), resulting in a neutral foot progression angle. This gait disruption pattern may compromise patellar tracking and knee loading (with permission from the author).

Table A1. Overview of classification definitions.

Kinematics				
Sagittal Plane	Pelvic tilt	Hip Fx/Ext	Knee Fx/Ext	Ankle Df/Pf
True Equinus	Normal Anterior	Normal Excessive extension Flexion	Normal Excessive extension Flexion	Plantarflexion
Apparent Equinus	Normal Anterior	Flexed	Flexed	Normal
Crouch Gait Compensated [^]	Anterior	Flexed	Flexed (more than 30° in the stance)	Excessive dorsiflexion
Crouch Gait Uncompensated *	Normal Posterior	Flexed	Flexed (more than 30° in the stance)	Excessive dorsiflexion
Stiff Gait knee source		hip profile in the stance-to- swing interval is normal	delayed and diminished peak knee flexion in swing phase (<45° flexion)	
Stiff gait hip source		hip profile in the stance-to- swing interval is abnormal (slow)	Delayed and diminished peak knee flexion in swing phase (<45° flexion)	
Transverse plane	Pelvic rotation	Hip rotation	Knee rotation	Foot progression
Neutral normal	neutral	Neut/ext	Neut/ext	Neutral
Neutral off-settings	Neut/ext/int	Internal	External	Neutral
Internal single/multilevel	Neut/ext/int	Neut/int	Neut/int	Internal
External single/multilevel	Neut/ext/int	Neut/ext	Neut/ext	External

Hip fx/Ext: hip flexion and extension. Knee Fx/Ext: knee flexion and extension. Ankle Df/Pf; ankle dorsiflexion and plantarflexion. Hyperext.: hyperextension. Neut/ext/int= neutral, external, internal.

[^] = normal internal extensor moment during stance phase

* = increase internal extensor knee moment during stance phase.

Table A2. Research protocols right and left sides.

Gait Classification (right side)	Gait Classification (left side)
Participant n°	Participant n°
Sagittal Plane	Sagittal Plane
Stance	Stance
Normal ()	Normal ()
Jump gait () $\left\{ \begin{array}{l} \text{True equinus ()} \\ \text{Apparent equinus ()} \end{array} \right.$	Jump gait () $\left\{ \begin{array}{l} \text{True equinus ()} \\ \text{Apparent equinus ()} \end{array} \right.$
Crouch gait () $\left\{ \begin{array}{l} \text{Compensated ()} \\ \text{Uncompensated ()} \end{array} \right.$	Crouch gait () $\left\{ \begin{array}{l} \text{Compensated ()} \\ \text{Uncompensated ()} \end{array} \right.$
Swing	Swing
Normal ()	Normal ()
Stiff gait () $\left\{ \begin{array}{l} \text{Knee source ()} \\ \text{Hip source ()} \end{array} \right.$	Stiff gait () $\left\{ \begin{array}{l} \text{Knee source ()} \\ \text{Hip source ()} \end{array} \right.$
Transverse Plane	Transverse Plane
Stance	Stance
Internal () $\left\{ \begin{array}{l} \text{Single level ()} \\ \text{Multi-level ()} \end{array} \right.$	Internal () $\left\{ \begin{array}{l} \text{Single level ()} \\ \text{Multi-level ()} \end{array} \right.$
External () $\left\{ \begin{array}{l} \text{Single level ()} \\ \text{Multi-level ()} \end{array} \right.$	External () $\left\{ \begin{array}{l} \text{Single level ()} \\ \text{Multi-level ()} \end{array} \right.$
Neutral () $\left\{ \begin{array}{l} \text{Normal ()} \\ \text{Off-setting ()} \end{array} \right.$	Neutral () $\left\{ \begin{array}{l} \text{Normal ()} \\ \text{Off-setting ()} \end{array} \right.$

References

1. Davids JR, Bagley AM. Identification of Common Gait Disruption Patterns in Children With Cerebral Palsy. *J Am Acad Orthop Surg*. 2014;22(12):782-790. doi:10.5435/JAAOS-22-12-782
2. Rodda JM, Graham HK, Carson L, Galea MP, Wolfe R. Sagittal gait patterns in spastic diplegia. *J Bone Jt Surg*. 2004;86(2):251-258. doi:10.1302/0301-620X.86B2.13878
3. Sutherland, DH; Davids J. Common Gait Abnormalities of the Knee in Cerebral Palsy. *Clin Orthop Relat Res*. 1993;march(288):139-147.

Appendix B. Orientation for the raters (PowerPoint presentation).

Orientation of how to use the Classification System

Orientation for Raters

Slide B1. Orientation of how to use the classification.

Media

Cases - protocols, videos and graphics

The pen drive comes with this animated PowerPoint presentation of the classification with an example and separate written instructions.

The cases to be evaluated are in numbered files. For each case there are:

videos with anterior, posterior, right and left lateral views;

kinematics graphs on the right and left side;

in addition to kinetics graphs for GMFCS 1 and 2 patients.

Slide B2. Media description.

How to proceed

- 1- Printing the classification and guidelines can help during the task of filling out the protocols.
- 2-Complete the classification protocol using videos and graphics (kinematics and kinetics).

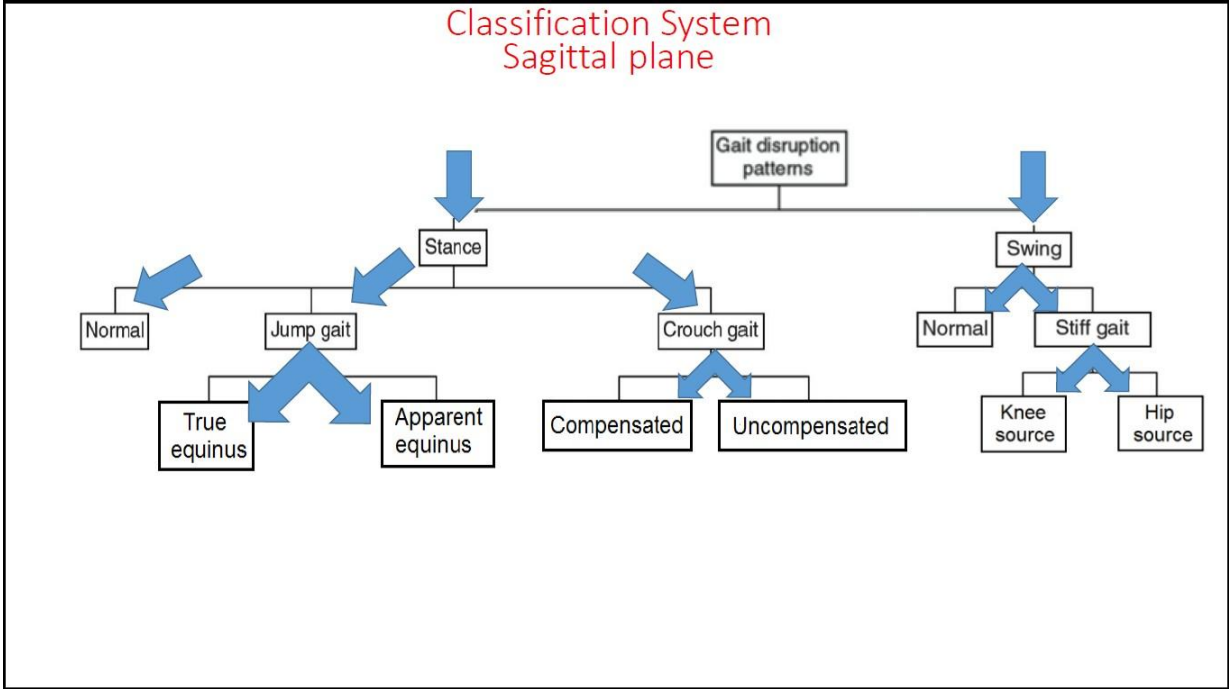
Slide B3. How to proceed to classify the sample of children.

How to use classification

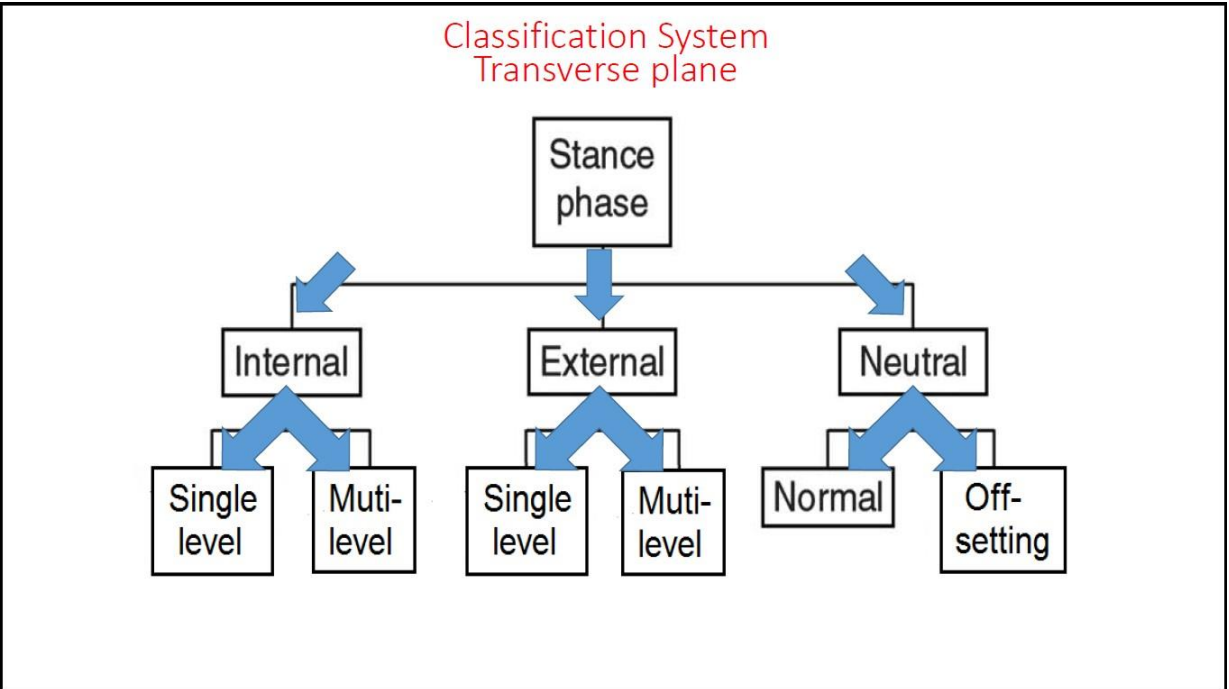
Hierarchical :

- Sagittal plane: stance and swing
- Transverse plane: stance

Slide B4. How to use de classification.



Slide B5. Flowchart of the sagittal plane of classification.



Slide B6. Flowchart of the transverse plane of classification.

Gait Classification (right side)

Participant n°

Sagittal Plane

Stance

Normal ()

Jump gait () { True equinus ()
Apparent equinus () }

Crouse gait () { Compensated ()
Uncompensated () }

Swing

Normal ()

Stiff gait () { Knee source ()
Hip source () }

Transverse Plane

Stance

Internal () { Single level ()
Multi-level () }

External () { Single level ()
Multi-level () }

Neutral () { Normal ()
Off-setting () }

Protocols

Gait Classification (left side)

Participant n°

Sagittal Plane

Apoio

Normal ()

Jump gait () { True equinus ()
Apparent equinus () }

Crouse gait () { Compensated ()
Uncompensated () }

Balanço

Normal ()

Stiff gait () { Knee source ()
Hip source () }

Transverse Plane

Stance

Internal () { Single level ()
Multi-level () }

External () { Single level ()
Multi-level () }

Neutral () { Normal ()
Off-setting () }

Slide B7. Right and left sides protocols for use during the classification of the children.

Excel spreadsheet protocols

	participant	sagittal stance phase right	swing phase right	transverse plane right	sagittal stance phase left	swing phase left	transverse plane left
1							
2							
3							
4							
5							
6							
7							
8							
9							
10							
11							
12							
13							
14							
15							
16							
17							
18							
19							
20							
21							
22							
23							
24							
25							

Slide B8. Example of excel spreadsheet protocol.

Example of how to fill out the excel spreadsheet

1	participant	sagittal stance phase right	swing phase right	transverse plane right	sagittal stance phase left	swing phase left	transverse plane left
2	1	jump gait/true equinus	normal	neutral/normal	jump gait/apparent equinus	normal	neutral/normal
3	2	crouch gait/compensated	normal	external/single level	crouch gait/compensated	normal	neutral/off-setting
4							

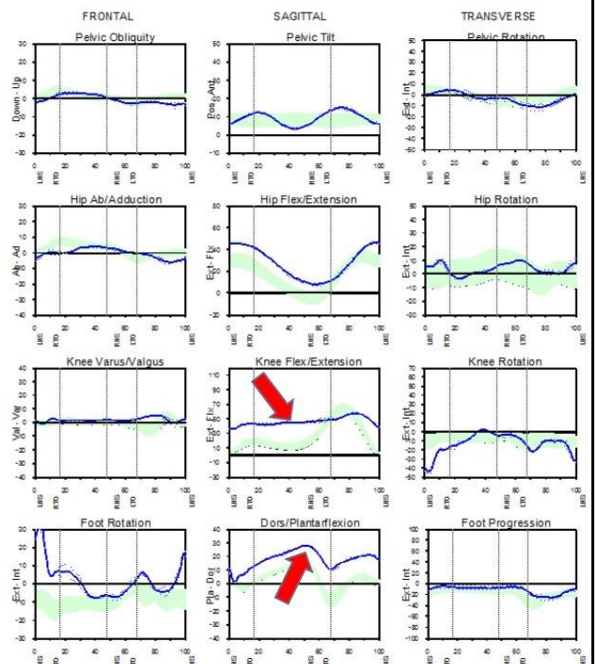
Slide B9. Example of how to fill out the excel spreadsheet protocol.

Example of how to classify

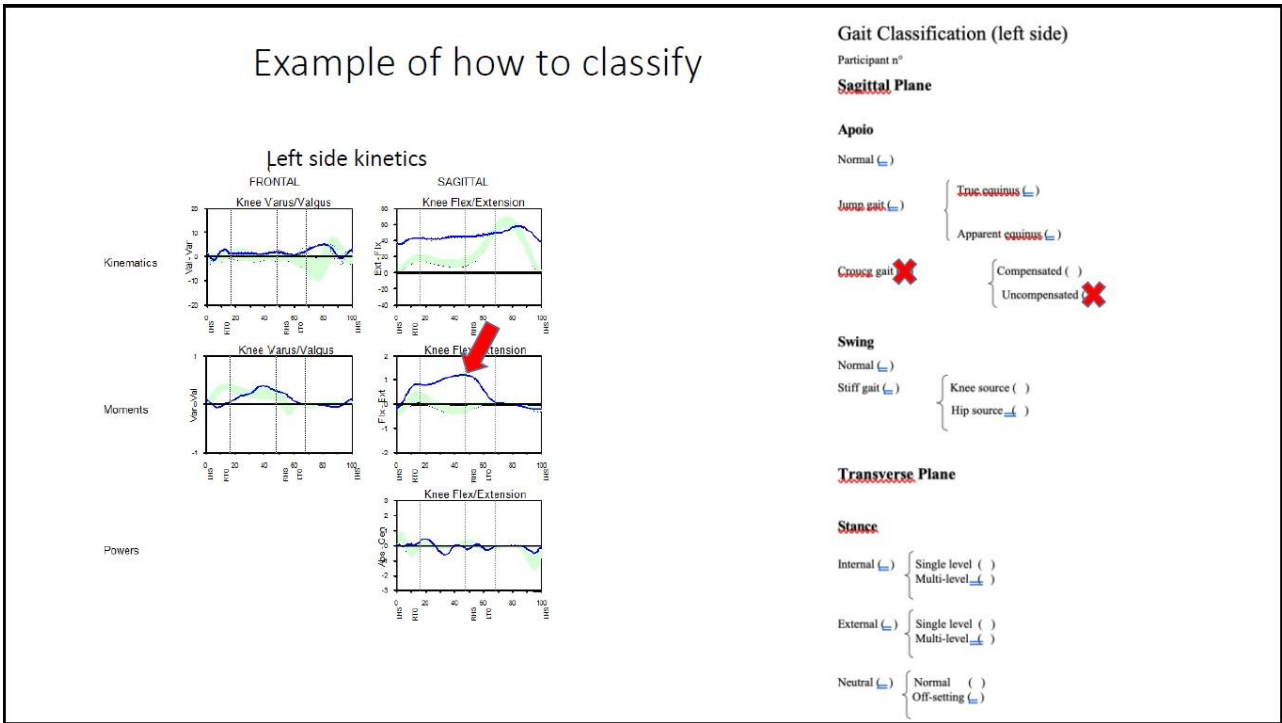


(Video sagittal view)

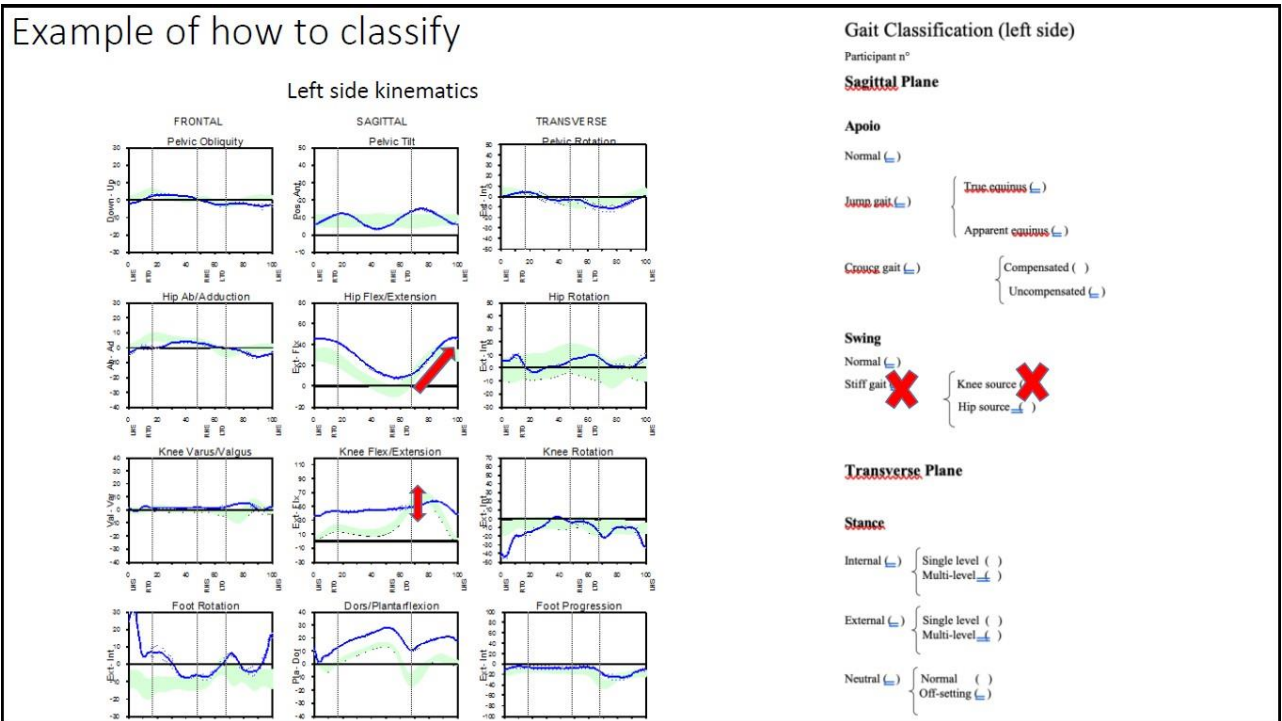
Left side kinematics



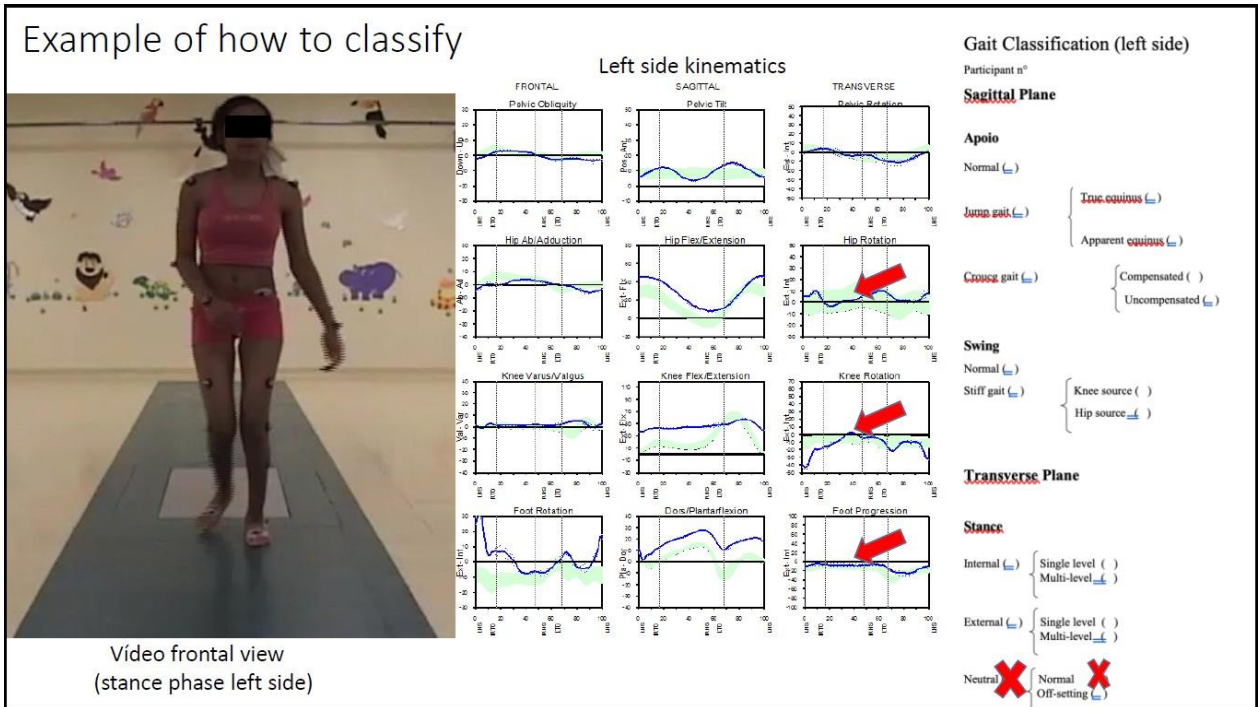
Slide B10. Example how to classify a child using the video and kinematics of the sagittal plane.



Slide B11. Example of how to use the kinetic data to classify the crouch gait pattern.



Slide B12. Example of how to use the kinematic data to classify the stiff gait pattern.



Slide B13. Example how to classify a child using the video and kinematics of the transverse plane.

Example of how to fill out the excel spreadsheet (left side).

	A	B	C	D	E	F	G
1	participant	sagittal plane stance phase right	sagittal plane swing phase right	transverse plane right	sagittal plane stance phase left	sagittal plane swing phase left	transverse plane left
2					crouch gait - uncompensated	stiff gait - knee source	neutral - normal
3							
4							
5							

Slide B14. Example of how to fill out the excel spreadsheet protocol.

Final Orientation

Finalize the filling of the protocols and excel spreadsheet on the 2 planes (sagittal and transverse) and send to the authors.

Slide B15. Final guidelines for evaluators.

7 ARTIGO 4

Artigo original formatado de acordo com as normas do periódico Gait and Posture.

Fator de Impacto: 2,414 Qualis: A1.

Title:

Constructing a classification for gait levels on a continuum for children with cerebral palsy.

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Abstract

Background: Gait deviations in cerebral palsy (CP) tend to be a continuum of deviations rather than well delineated groups. The purpose of this study was to classify gait in CP children using the concept of levels rather than categorize into patterns.

Research question: Is the classification of gait levels of children with CP valid and reliable?

Methods: CP children (N=101; 51 F, 50 M; 12.2+-3.4 years), were assessed using observational gait analysis (OGA) and three-dimensional gait analysis (3DGA). Age, gait velocity, Gross Motor Function Classification System (GMFCS) and Global Profile Score (GPS) were used to characterize the sample. Build a classification using the increase of problems from ankle to more proximal joints in sagittal and transverse planes and the necessity of walking aids. The comparison between the levels was performed by the ANOVA test, according to the normality of the data. The reliability of the classification was determined by Kappa index.

Results: We determined 3 gait levels for children with CP. All levels were represented in the evaluated sample and all participants were classified. The GPS was on average three degrees different between the levels, increasing from level 1 to 3 ($p<0.001$). The interrater reliability was substantial for the classification using 3D data and observational gait analysis (OGA) according Fleiss's Kappa statistics. The intrarater reliability, between the raters and the authors consensus, and between the two professional categories, was substantial to almost perfect using OGA and 3DGA ($p<0.001$), according to weighted Kappa statistics.

Significance: The level classification presented validity in the sample of CP evaluated. The interrater reliability was substantial and substantial to almost perfect for intrarater and between raters and authors consensus. Longitudinal studies in the future can determine the utility of the classification to follow patients during the natural evolution or after treatments.

Keywords: cerebral palsy, gait, children, classification.

Highlights

- Classification with face, criterium and concurrent validity;
- Substantial reliability interrater and substantial to almost perfect reliability intra rater and between raters and authors consensus.
- Positive relationship between previous calf surgery, external and neutral off-setting rotated position with level 3.
- The classification can be used for evaluators with less experience in gait analysis with only observational analysis, which increases its applicability in the daily clinic.

1. Introduction

The cerebral palsy (CP) results from a primary injury in the central nervous system, and clinical symptoms are observed in the peripheral neuromuscular system [1]. Walking capacity is significantly impaired in children with CP, walking at 5 years of age was reported for 70% of the patients [2] [3]. The motor impairments are multifactorial and included: abnormal muscle tone, spasticity, loss of selectivity and muscle weakness [3]. To explain what happens in this group of patients it is necessary to remember that, during the ontogenetic phase of independent human locomotion, two separate forms of growth occur [4]: the infants physical size, their mass and their height increase [5]; and specific neural circuits develop during ontogeny and transform the infants locomotor pattern [6]. The developmental of neural circuits are impairment and the complexity of controls is reduced in children with CP [7]. With growth, musculoskeletal deformities usually appear as a result of abnormal forces acting on the developing body. Therefore, the gait of children with CP is the result of neurological changes and musculoskeletal disorders.

There is pronounced individual variety of movement patterns in ambulatory children with CP, depending on the severity of such disorders [8] [9]. Using computerized three-dimensional gait analysis (3DGA), it has been possible to identify the similarities and differences of abnormal gait patterns in patients with CP [9]. Gait Classification System (GCSs) have been reported to aid in clinical decision making, in improving communication among healthcare providers and in comparing gait between or within specific patients [10].

Several gait classifications of qualitative and quantitative data were described for the past few decades [11]–[19]. Accurate gait classification of CP has been shown challenging because of its heterogeneous presentations [20], and the difficulty in which gait parameters provide a faithful measure of neuromuscular function [21].

In 2016, Nieuwenhuys et al. identified 49 clinically important gait patterns across the pelvis, hip, knee and ankle [22]. Thus, seemingly infinite variation in and combinations of patterns are possible [10], [19].

According, Rodda et al., sagittal gait pattern changed in 50% of patients, some towards true equinus and others to crouch gait [14]. Bell et al., confirmed that deterioration in normalized walking speed, increased flexion and increased stiffness may be the natural

history for children with spastic diplegia [23]. Rosenbaum et al. describes a plateau in motor development around the age of seven years [24] and in some there is deterioration in walking ability through adolescence and adulthood [23].

In children with CP, sagittal gait patterns and their associated classifications are not always static [14]. Gait deviations in CP tend to be a continuum of deviations rather than well delineated groups [25], and categorization approaches are often based on partial information, and data close to the boundary between classes could be erroneously classified [22].

The development of a classification of levels of gait, that allows the assisting professional to easily identify the current gait status of the children with CP and create a panorama with probable evolutions, seems desirable.

To build the classification, it was taking into account that the basic function of the lower limb during stance is to resist collapse and to extend sufficiently to achieve the required push-off. Collapse of the lower limb requires a flexion at all three joints: knee, ankle and hip [26]. A cycle of muscle damage, tendinous lengthening, bone deformity and increasing tension may explain the progressive nature of flexed-knee gait [27]. The excessive flexion of the hip, knee, and ankle during the stance phase of gait produce an inefficient walking pattern and if left untreated can lead to joint pain, bone deformities and, in some cases, loss of independent gait [28]. For that, we conceptualized that the joints of the ankles and knees would determine the progression of the classification. The increase in knee flexion with ankle dorsiflexion would be determinants of less gait functionality.

The aim of this study is to develop a classification with a concept of continuity using elements of previous classifications. The secondary objective was to evaluate the reliability of the new classification. Intra and interrater reliability was assessed using only observational gait analysis (OGA) and then including 3DGA data. Reliability was also assessed among different professionals, in relation to more and less experienced evaluators and between each evaluator and the authors' consensus rating.

2. Methods

After the project was approved by local research ethics committee, number: 2.447.001, the study was developed by an estimated sample of 51 individuals considering the prevalence of 0.3% [3] and maximum standard error of 1.5%. The search conducted from the database of the Gait Analysis Laboratory at the Ana Carolina de Moura Xavier Rehabilitation Hospital Center in Curitiba, Paraná, Brazil, provided a sample of 101 children who had undergone gait analysis with a diagnosis of spastic cerebral palsy and symmetrical lower limbs. Written informed consent was obtained from all subjects.

Eligible patients were between 5 years old and 18 years old, classified in Gross Motor Function Classification System (GMFCS) levels I to IV, had predominantly spastic CP, and had undergone OGA and 3DGA. Previous treatments such as single-event multilevel surgery or botulinum toxin type A injections were allowed.

The study was made in three parts. The first was a cross-sectional study to develop a classification of the gait levels for children with CP. The second part was to classify the sample using the new classification and to make comparisons between the groups formed. The third part was to investigate the reliability of the classification.

2.1. Measurements

Each participant's gait was recorded on video, using sagittal and coronal views. The OGA, was performed by visual observation of two-dimensional videos. The patients walked barefoot on a ten meters walkway at their normal self-selected speed. Instrumented 3DGA was performed using the conventional gait model (Helen-Hayes model)¹³, with reflective markers (n =26), to obtain spatiotemporal parameters (step and stride lengths, cadence, walking velocity) and lower extremity kinematics at the pelvis, hip, knee, and ankle. 3D kinematic and kinetic gait data were collected bilaterally using 6 digital motion analysis cameras (Motion Analysis Corporation in Santa Rosa, CA) sampling at 60 Hz. Joint kinematics were calculated by the Cortex software (Motion Analysis Corp., Santa Rosa, CA). The data was processed using OrthoTrack software (OrthoTrack 6.5.1 software, Reference Manual 2007. Motion Analysis Corporation, Santa Rosa, CA). The data were smoothed using a Butterworth filter with a cut-off frequency of 6 Hz. The motion

analysis system was calibrated before each analysis. All kinematic data were time-normalized to 100 % of one gait cycle. 3DGA kinematics were used to calculate the GPS, which quantifies the overall deviation of an individual's gait from normal gait¹⁴The kinematic data were collected from a minimum of 7 gait cycles for each assessed leg and the most representative trial was reported, alongside the corresponding video clips, and classified according to the gait classification of level in CP children.

The GMFCS was assigned by a senior clinical physiotherapist and a pediatric orthopedist in consultation with the child and his or her parents.

2.2. Cross-sectional study

The sample of 101 participants, with symmetrical lower limbs, were assessed using OGA and 3DGA data to elaborate the classification of gait levels. The progressive knee flexion (sagittal plane), transverse plane deviations and need to use walking aids, were the determinants for the elaboration of the new classification.

After the elaboration of the new classification the sample of patients was classified into the levels, and the groups formed were compared in respect to age, gait velocity, GMFCS and GPS.

The face and criterium validity were assessed through the classification capacity to allocate the sample in the levels, and for the use of quantitative kinematic data, respectively. The concurrent validity was assessed by the clinical significance difference between the average GPS in the levels of the classification.

2.3. Reliability study

A brief learning phase was proposed, when all raters participated in an online presentation, with discussion of the classification and presentation of examples to illustrate how to grade the cases using the new classification. The raters were provided with written definitions and illustrations of the posture of the ankle, knee, hip and pelvis for each gait pattern in relation to the planes of motion (supplementary material).

To determine intra and interrater reliability, 20 participants were evaluated (40 lower limbs) with predominantly asymmetrical movement pattern of the lower limb, different from the 101 participants evaluated in the cross-sectional study. These participants were

selected in order to create a sample that included variation in age and levels of neurological involvement (GMFCS). Four raters classified the sample (two PT and the two PO), three of them had more than 3 years of experience in gait analysis, and one had limited experience in 3DGA. The evaluators, during online presentation of the cases, were asked to initially classify using only video (OGA) and then using video and 3DGA data. To determine intrarater reliability, the raters evaluated the 20 participants (40 lower limbs) a second time, at the same way, one month after the initial assessment. The right and left sides of the lower limbs were classified. The authors produced a consensus classification of the sample under study of reliability. Then, the reliability between the raters and the consensus was calculated. The reliability between the two PT and the two PO was also assessed.

2.4. Statistical Analysis

Descriptive data were presented as means and standard deviations or as medians and interquartile ranges, according to the normality distribution, analyzed using the Shapiro-Wilk test. For the comparison between groups with normal distribution, one-way ANOVA analysis was performed using Tukey's post hoc test. For data with non-normal distribution, the Kruskal-Wallis test was used and Mann-Whitney's post hoc test. The level of significance was set at $p < 0.05$.

The reliability of the classification was determined by Fleiss's Kappa for interrater evaluation. Weighted Kappa statistics were used to summarize intrarater reliability, between raters and golden standard, and between the two professional categories, with quadratic weight for the three ordered levels. The analyses were performed in SPSS statistical software, Version 27.

The strength of k was interpreted as: equal to zero, "without agreement"; between zero and 0.19, "poor agreement"; from 0.20 to 0.39, "weak agreement"; from 0.40 to 0.59, "moderate agreement"; from 0.60 to 0.79, "substantial agreement"; from 0.80 to 1.00, "almost perfect agreement" [31].

3. Results

3.1 Cross-sectional study

The sample consisted of 101 participants with spastic CP, being 50 boys (49.50%) and 51 girls (50.49%), 15 unilateral and 86 bilateral CP. Of these, 20 were GMFCS I, 62 were GMFCS II, 16 were GMFCS III and 3 were GMFCS IV. The mean age was 11.89 ± 3.4 years and 35.64% of the patients had prior orthopedics surgery. Walking assistive devices were used for 16 individuals (15.84%) in the sample, with 10 walkers, 4 crutches and 2 walking sticks. All groups of the classification were represented in the evaluated sample and all patients in the sample were classified according the levels.

3.1.1 Description of the gait classification categories.

The three levels of gait abnormalities were defined after reviewing the entire sample and are described in Table 1 and represented schematically in Figure 1. Figure 2 summarizes the kinematic data from the sagittal plane (pelvis, hip, knee, ankle) for each gait level within one standard deviation from normal.

Level 1 participants had kinematics in the sagittal plane as typical or minor deviations from normality in the hips and knees and normal or with a trend to plantar flexion in the ankles (Table 1). In the transverse plane they had normal rotational profile or deformity in just one level (pelvic/hip/knee/foot). The distribution of transverse plane alterations in level 1 participants was: normal in 40 lower limbs (86.95%), single level internal rotation in 5 (10.98%), and single level external rotation in 1 (2.17%). The Figure 3 presents a trend to internal foot progression angle. The level 1 participants did not use any walking aids.

The participants of levels 2 had the kinematics in sagittal plane of motion similar to level 1, when using walking aids. The participants level 2 presented, independently of walking aids or deformities in transverse plane, with knees in flexion or hyperextension and ankle in normal dorsiflexion or plantarflexion (Table 1). Level 2, normal transverse plane was present in 49 lower limbs (44.54%), normal off- setting alignment (compensated internal and external rotation) in 11 (10%), single level internal rotation in 42 (38.18%),

multi-level internal rotation in 6 (5.45%), and multi external rotation in 2 (1.81%). The Figure 3 presents a trend to internal foot progression angle.

The participants of the level 3 had the kinematics in sagittal plane in triple flexion of the hip, knee and ankle (trend to excessive dorsiflexion). The participants level 3 could use walking aids and have transverse plane deformities in single or multilevel (Table 1). The level 3, presented with normal transverse plane in 19 lower limbs (41.30%), normal off-setting alignment (compensated internal and external rotation) in 12 (26.08%), single level internal rotation 3 (6.52%), single level external rotation in 3 (6.52%), and multi-level external rotation in 9 (19.56%). Figure 3 shows a more variable position of foot progression angle.

The characteristics of the three levels of the classification in relation to age, gait velocity, GMFCS and GPS, are shown in Table 2. The velocity decrease from the levels 1 and 2 to level 3, with statistically difference between level 1 and 3 and level 2 and 3. The GMFCS increases from level 1 to 2 and 3, with statistically difference between level 1 and 2 and level 1 and 3 (Table 2). The GPS overall showed decrease of functionality from level one to 3 with statistically difference between all groups of the classification (Table 2). The difference was progressively higher than 3 degrees between the levels ($p < 0.001$).

Level 2, 8 participants (14.54%) used walking assistive devices, 4 crutches and 4 walkers. Level 3, 9 participants (39.13%) used walking aids, 6 walkers, 1 pair of crutches and 2 walking sticks.

Among GMFCS I participants, 12 were level 1 and 8 were level 2. Participants from GMFCS II, 11 were level 1, 36 were level 2 and 15 were level 3. The GMFCS III group, 11 were level 2 and 5 were level 3. All three GMFCS IV participants were level 3.

The relation between previous calf surgery and levels of gait was: 4 participants (17.39%) level 1, 17 participants level 2 (30.90%), and 15 participants level 3 (65.22%) had previous calf surgery.

3.2 Reliability study

The overall interrater reliability across the levels of the classification was 0.684 (0.595-0.774) using 3DGA, and 0.671 (0.581-0.761) using OGA, according Kappa Fleiss (k) statistics with 95% CI.

Intrarater reliability of the classification using OGA and 3D data is presented in Table 3. The reliability between the raters and authors consensus, using OGA and 3DGA were presented in Table 4.

An additional analysis was performed considering the comparison between different professionals and between more and less experienced raters. The reliability between the two PT and between the two PO was 0.870 (0.768-0.972) and 0.826 (0.715-0.938) for 3DGA, respectively. The reliability between the two PT and between the two PO was 0.936 (0.864-1.008) and 0.740 (0.599-0.881) using OGA, respectively, according Kappa weighted, with 95% confidence interval (CI). The reliability of the more and less experienced raters showed similar results.

4. Discussion

The current study uses the concept of gait in children with CP as a continuum of changes and not something that can be categorized in a static way. When assessing the gait of 101 children with CP, it was possible to develop a classification of gait levels. To construct the classification, data from 2D videos and kinematics of more than one plane of movement (sagittal and transverse planes) was used. The level classification uses concepts from previous classifications, such as the sagittal plane of the classification of Rodda et. al. [14] and Papageorgiou et al [32], and the transverse plane of the Davids and Bagley classification [15].

The classification developed also incorporated the use of walking aids because of the possibility of, when used, masking kinematic changes in the lower limbs [33]. The use of walking aids is a way to compensate for deficits in balance and/or muscle weakness [34].

In the sagittal plane, the levels of the gait were divided according to the position of the knee and ankle in the stance, this because over 80% of the variance of the support moment of CP patients is explained by a linear relationship with knee flexion [35]. In this sense, the levels classification use factors that lead children with CP to develop increased knee flexion. These are a combination of factors, including mechanical insufficiency of the plantar flexors and knee extensors muscles (sagittal plane), lever-arm dysfunction (transverse plane), and weakness (walking aids) [35].

The classification showed face and criterium validity, due capacity to allocate the sample in the levels and for the use of quantitative kinematic data, respectively. The concurrent validity was assessed by the difference between the average GPS of the levels of 3°, that is the minimal clinically important difference between levels of the GMFCS (2.98°) [36]. The GMFCS levels increased with the increase of the classification's levels, and it also presents a progressive frequency of knee flexion in the stance phase of the gait [37]. However, the GMFCS has an overlap of motor patterns [37], and does not present mobility, it is almost stable. The level classification of the gait has the capacity to differentiate motor levels and present mobility between the levels, something uncommon to GMFCS.

Participants with complete knee extension were classified as level 1 and the ones with knee flexion in levels 2 and 3. The positioning of the ankle on the stance differentiates level 2 and 3, with the first presenting the ankle in a normal position or in plantar flexion, while the latter with tendency to excessive dorsiflexion. Therefore, level 1 resembles the mild gait and true equinus pattern; level 2, true equinus, jump gait and apparent equinus; and level 3, apparent equinus and crouch gait of the Rodda et al. classification [14]. The transverse plane used the concept of position of the foot progression angle and the elements that produce the alignment, single or multilevel [15]. The alignment of the transverse plane showed a progressive increase in the frequency and complexity of abnormalities. Level 1 had 86.95% of normal participants, while the percentage of normal was 44.54% and 41.30%, at levels 2 and 3, respectively. The abnormalities at level 3 showed a higher frequency of more complex disorders (multilevel), being 45.62% compared to 17.26% at level 2. This situation corroborates the classification's ability to identify progressive abnormalities in this plane of movement.

In ambulant children with cerebral palsy, the self-selected velocity of walking is reduced in proportion to the severity of disability [38]. This premise was confirmed by the progressive decrease in velocity according to the increase in classification levels (Table 2). The impairment of selective control is another significant factor for less motor function and the GPS has a negative correlation [39]. In the classification proposed in this study, there is a progressive increase of three degrees in the GPS between the classification

levels. What seems to demonstrate that the progression of the levels was related to a decrease in the selective control and motor function of the participants.

The gait classification in levels for CP can be used for children with unilateral or bilateral impairment. However, only children with bilateral impairment will reach the most advanced level of the classification.

The authors recommend using the classification to guide treatments and future comparisons. The traffic light classification provides a simple and common language based upon three-level colors coding, according Novak et al [40]. Level 1 (green) would indicate that the patient is progressing without significant skeletal muscle problems. Level 2 (yellow), a warning signal should be recognized, as skeletal muscle problems are apparent and must be interfering with the walking ability. At level 3 (red), skeletal muscle changes are significantly altering gait capacity and should have their correction strongly considered.

Although there is an attempt to delimit the characteristics of each level, the data produces continuity between the classification ranges and allows a simple and practically automatic classification of the participants. The authors encourage the use of transition levels such as 1-2 and 2-3 in future work.

The classification showed substantial interrater reproducibility using OGA and using 3DGA and video. The intra rater reliability of the classification using 3D data and OGA was substantial to almost perfect.

The reliability between the raters and authors consensus, was substantial to almost perfect for all raters. In the evaluated sample, similar results were obtained by evaluators with and without experience with 3DGA. The reliability within the two professional categories was substantial to almost perfect. The daily clinical applicability of the classification was determined by the significant results obtained only with the analysis of the video, for the ability of less experienced evaluator and different professionals to use the classification properly.

Previous calf surgery may play a predisposing cause to evolution to level 3, in the sample evaluated. It's important to remember that crouch gait, one pattern of level 3, are also part of the natural history of spastic diplegia for some children [14]. However, as the age range of individuals from the other groups was not statistically different, triceps sural

lengthening surgery should be considered a predisposing factor for the evolution to the level 3, since the soleus muscle provide significant stance phase support [41].

Limitations of this study are related to the fact that most of our participants were referred for gait analysis for preoperative evaluation to improve their ambulatory function, their gait problems may not reflect those of the general CP population. During the cross-sectional study the classification was not used in asymmetric patients. However, during the reliability study, symmetrical and asymmetric individuals were analyzed and the rater classified differently each lower limb.

5. Conclusion

The new classification proved to be valid, reliable and has advantages because uses the idea of continuity rather than rigid categorization. The classification can be used for evaluators with less experience in gait analysis using only OGA. Longitudinal studies in the future to determine the responsiveness of the classification during the natural evolution or after treatments is strongly encouraged.

Author contribution statement

Alessandro G. Melanda (Conceptualization) (Methodology) (Validation) (Formal Analysis) (Investigation) (Data Curation) (Writing – Original Draft) (Writing – Review & Editing) (Visualization) (Supervision).

Alexandre R M Pelegrinelli (Data Curation) (Writing – Review & Editing) (Visualization).

Dirce Shizuko. Fujisawa (Conceptualization) (Visualization) (Supervision).

Suhaila Mahmoud Smaili (Conceptualization) (Formal Analysis) (Writing – Review & Editing) (Visualization) (Supervision).

All authors have read and approved the final manuscript.

Declaration of Competing Interest

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Supplementary data

Complementary material related to this article can be found after the illustrations.

Appendix A. Written description of the gait classification categories.

Appendix B. Orientation of how to use the Classification System (PowerPoint presentation).

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Table 1. Characteristics definition of kinematics and walking aids for levels of gait in CP children.

Gait Level	Sagittal plane			Ankle Df/Pf	Transverse plane	Walking aids
	Pelvic tilt	Hip Fx/Ext	Knee Fx/Ext			
Level 1 (n=23)	Normal Anterior	Normal or Minor deviations	Normal or Minor deviations	Normal or trend to plantarflex.	Normal or single level	No
* Level 2 (n=55)	Normal Anterior	Normal or Minor deviations	Minor deviations or hypertext.	Normal or Plantarflex .	Multi-level	and/or Yes
	Normal Anterior Posterior	Flexed	Flexed	Normal or Plantarflex	Normal Single/multi-level	No or Yes
Level 3 (n=23)	Anterior Normal Posterior	Flexed	Flexed	Excessive dorsiflex.	Normal Single/multi-level	No or Yes

Hip Fx/Ext: hip flexion and extension. Knee Fx/Ext: knee flexion and extension. Ankle Df/Pf; ankle dorsiflexion and plantarflexion. Hyperext.: hyperextension. Plantarflex.: plantarflexion. Dorsiflex.: dorsiflexion.

* Note that a child with sagittal plane characteristics of level 1 becomes level 2 when presenting multi-level deformity in the transversal plane of movement or use walking aids to walk.

Walking aids: walking sticks, crutches or walkers.

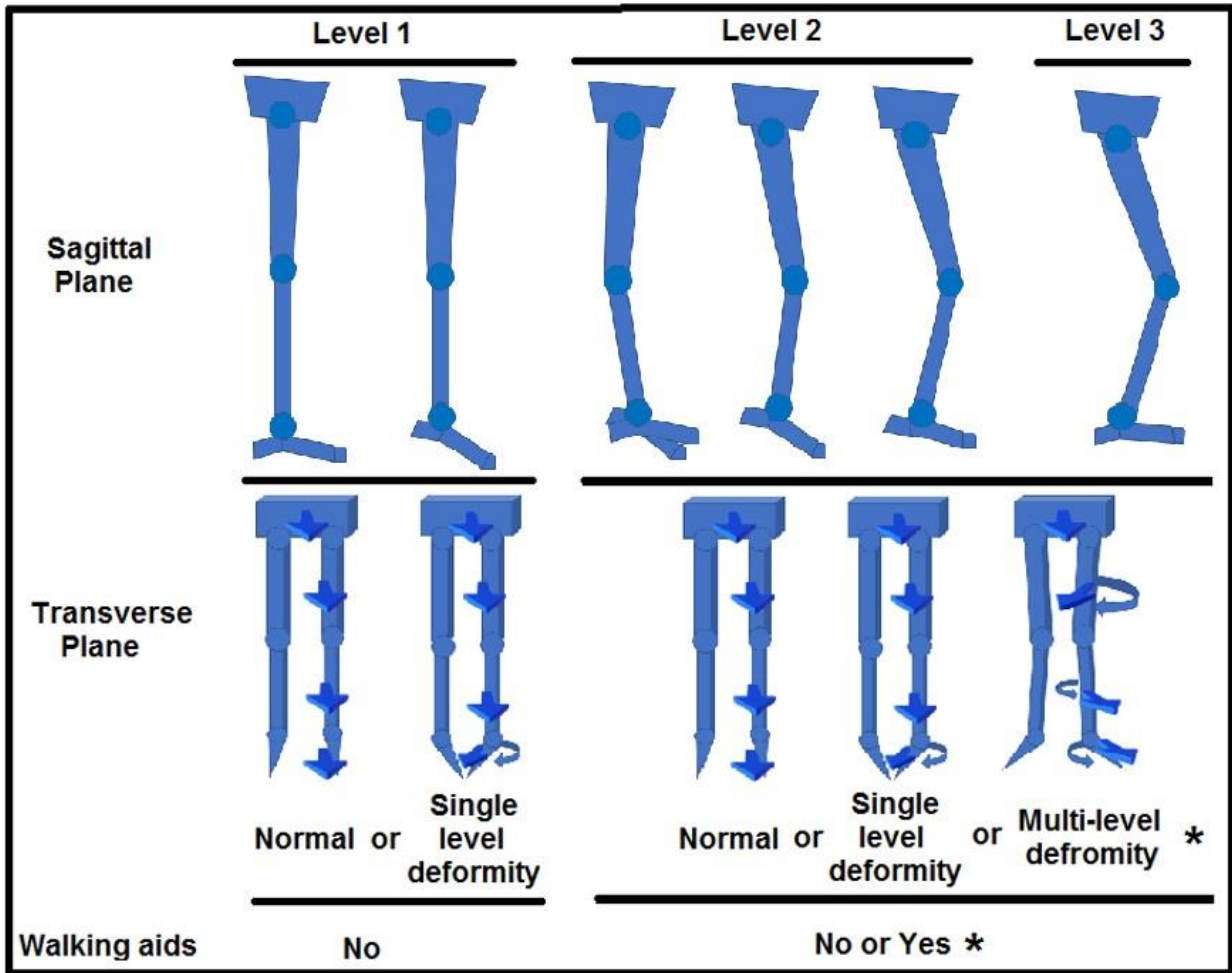


Figure 1. Diagrams showing schematic drawing of the sagittal and transverse plane gait characteristics of the lower limbs, as well as the use of walking aids for each gait level in children with CP.

* Note that a child with sagittal plane characteristics of level 1 becomes level 2 when presenting multi-level deformity in the transverse plane of movement or use walking aids to walk.

Walking aids: canes, crutches or walkers.

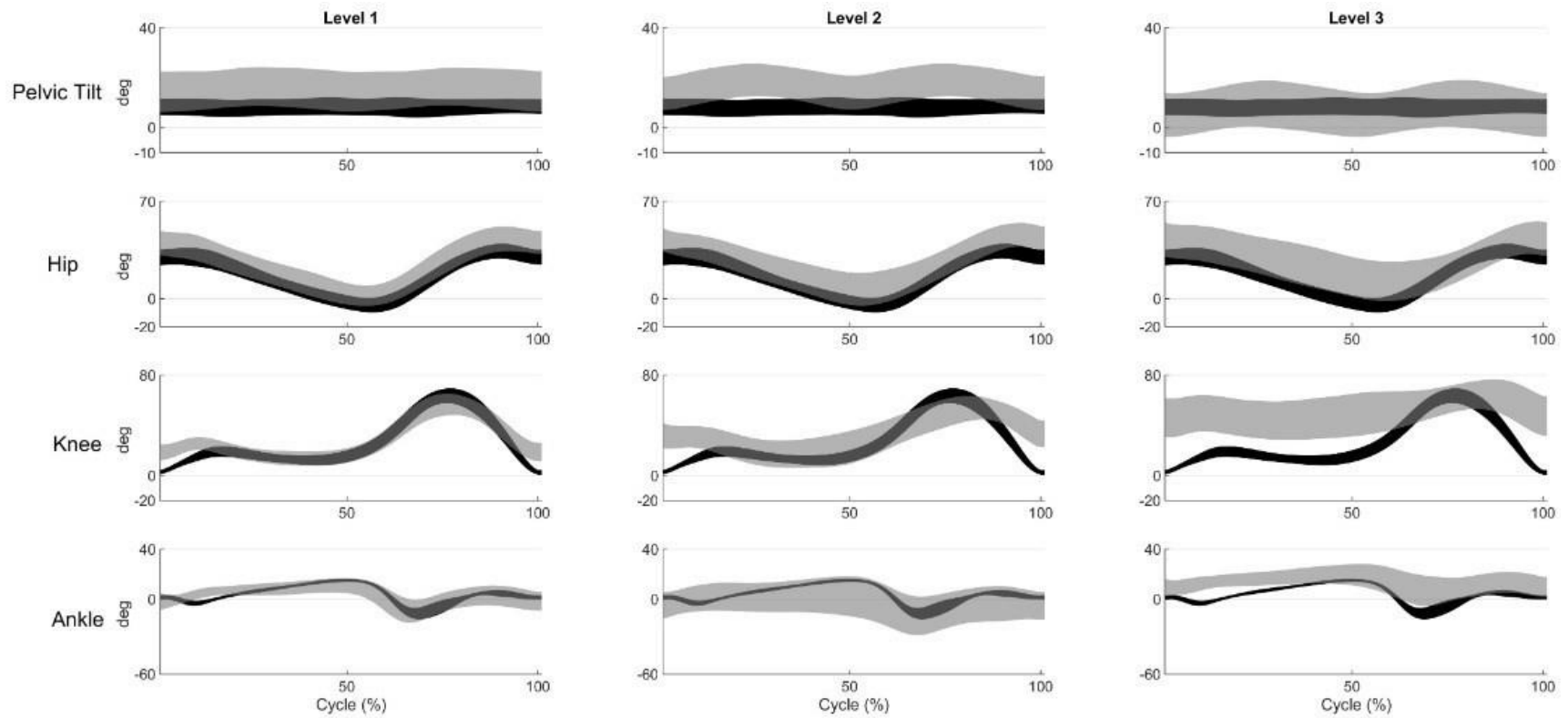


Figure 2. The summarized sagittal plane kinematic data for each gait level for the study population. The black band represented the mean \pm 1 SD of kinematic data normal database, and the grey band the mean \pm 1 SD for each gait pattern. The vertical axis represents joint angular displacement and the horizontal axis, 100% of the gait cycle

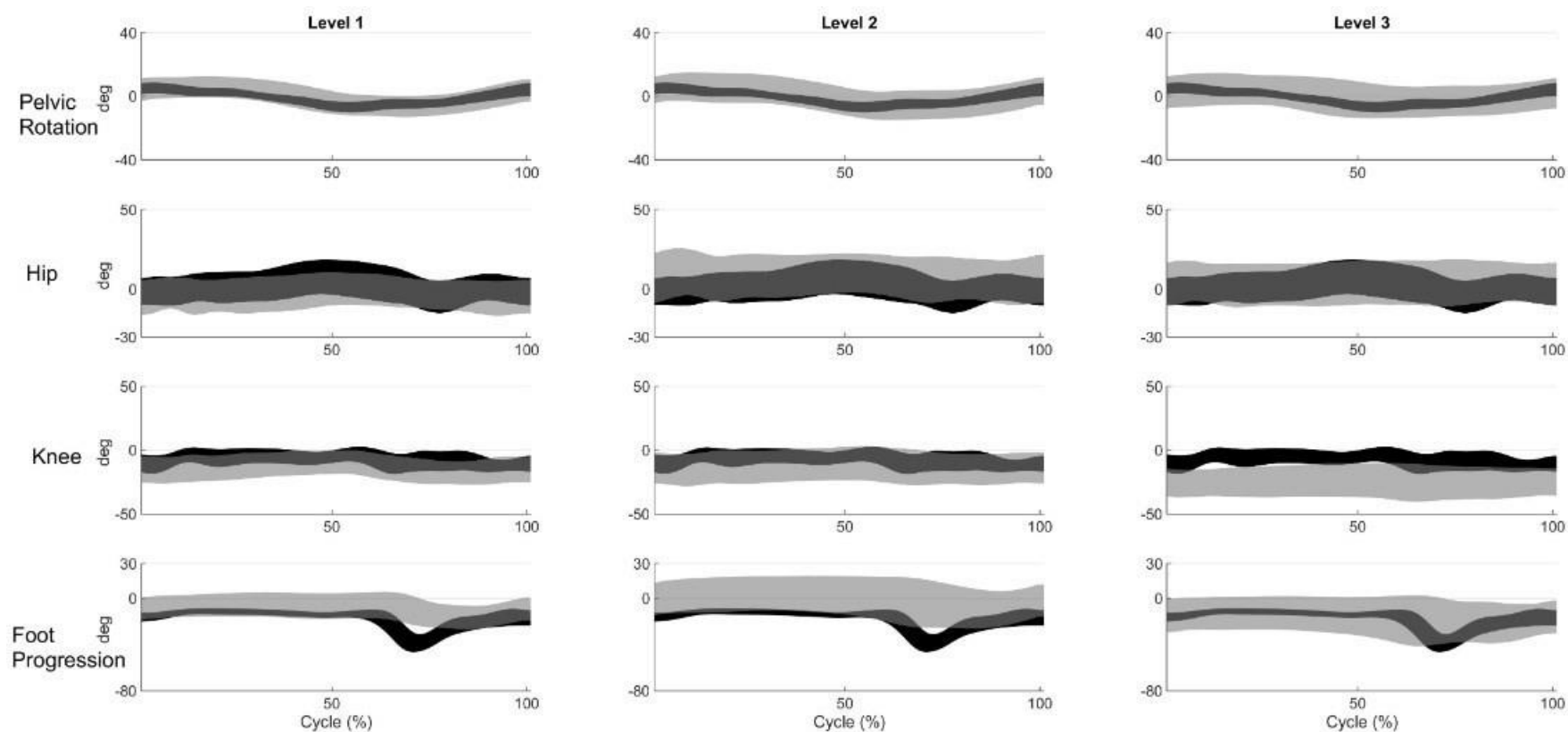


Figure 3. The summarized transverse plane kinematic data for each gait level for the study population. The black band represented the mean \pm 1 SD of kinematic data normal database, and the grey band the mean \pm 1 SD for each gait pattern. The vertical axis represents joint angular displacement and the horizontal axis, 100% of the gait cycle.

Table 2. Mean and standard deviation or median and interquartile range of the variables age, gait velocity, GMFCS and GPS according to gait level under investigation.

Gait levels/ variables	Level 1 (n=23)	Level 2 (n=55)	Level 3 (n=23)	P
Age (years)	12.16 ±2.81	11.31±3.37 ^a	13.95±2.76 ^b	0.008
Velocity (cm/s)	90.00 [73.00-106.80]	84.00 [64.90-98.10]	56.85 [39.90-83.60] ^{b,c}	0.001
GMFCS	1 [1-2]	2 [2-2] ^a	2 [2-3] ^b	<0.001
GPS (°)	10.40 [8.60-11.70]	13.40 [11.40-16.10] ^a	16.40 [15.00-19.80] ^{b,c}	<0.001

cm/s= centimeters per second, GMFCS= Gross Motor Function Classification System, (°) = degrees.

a = statistically significant difference between level 1 and level 2.

b = statistically significant difference between level 1 and level 3.

c = statistically significant difference between level 2 and level 3.

Table 3. Weighted Kappa (k) statistics with 95% CI for intrarater reliability using OGA and 3DGA to classify the sample.

Raters/ OGA n=40	k	SE	CI 95%	P
*rater 1	0.887	0.046	0.796-0.978	<0.001
*rater 2	0.774	0.067	0.642-0.906	<0.001
*rater 3	0.814	0.057	0.702-0.926	<0.001
rater 4	0.767	0.066	0.639-0.896	<0.001
Raters/ 3DGA n=40	k	SE	CI 95%	P
*rater 1	0.857	0.054	0.752-0.963	<0.001
*rater 2	0.892	0.049	0.796-0.987	<0.001
*rater 3	0.867	0.046	0.776-0.958	<0.001
rater 4	0.717	0.091	0.539-0.895	<0.001

SE= Standard Error; CI= Confidence Interval; OGA: observational gait analysis.

*Experienced clinicians (>3y experience assessing 3DGA).

Table 4. Weighted Kappa (k) statistics with 95% CI for reliability between the raters and the authors consensus using OGA and 3DGA to classify the sample.

Raters/ OGA n=40	k	SE	CI 95%	P
*rater 1	0.941	0.034	0.873-1.008	<0.001
*rater 2	0.879	0.049	0.784-0.975	<0.001
*rater 3	0.781	0.065	0.653-0.908	<0.001
rater 4	0.896	0.046	0.805-0.987	<0.001
Raters/ 3DGA n=40	k	SE	CI 95%	P
*rater 1	0.876	0.050	0.777-0.974	<0.001
*rater 2	0.842	0.057	0.731-0.954	<0.001
*rater 3	0.845	0.054	0.739-0.950	<0.001
rater 4	0.942	0.034	0.876-1.008	<0.001

SE= Standard Error; CI= Confidence Interval. OGA: observational gait analysis;
*Experienced clinicians (>3y experience assessing 3DGA).

7.1. Supplementary data (Training material for raters)

Appendix A. Written description of the gait classification categories.

The three levels of gait abnormalities have been defined after the review of the entire sample. Figure A1 and Table A1 summarizes the kinematic data from the sagittal plane (pelvis, hip, knee, ankle) for each gait level within one standard deviation from normal.

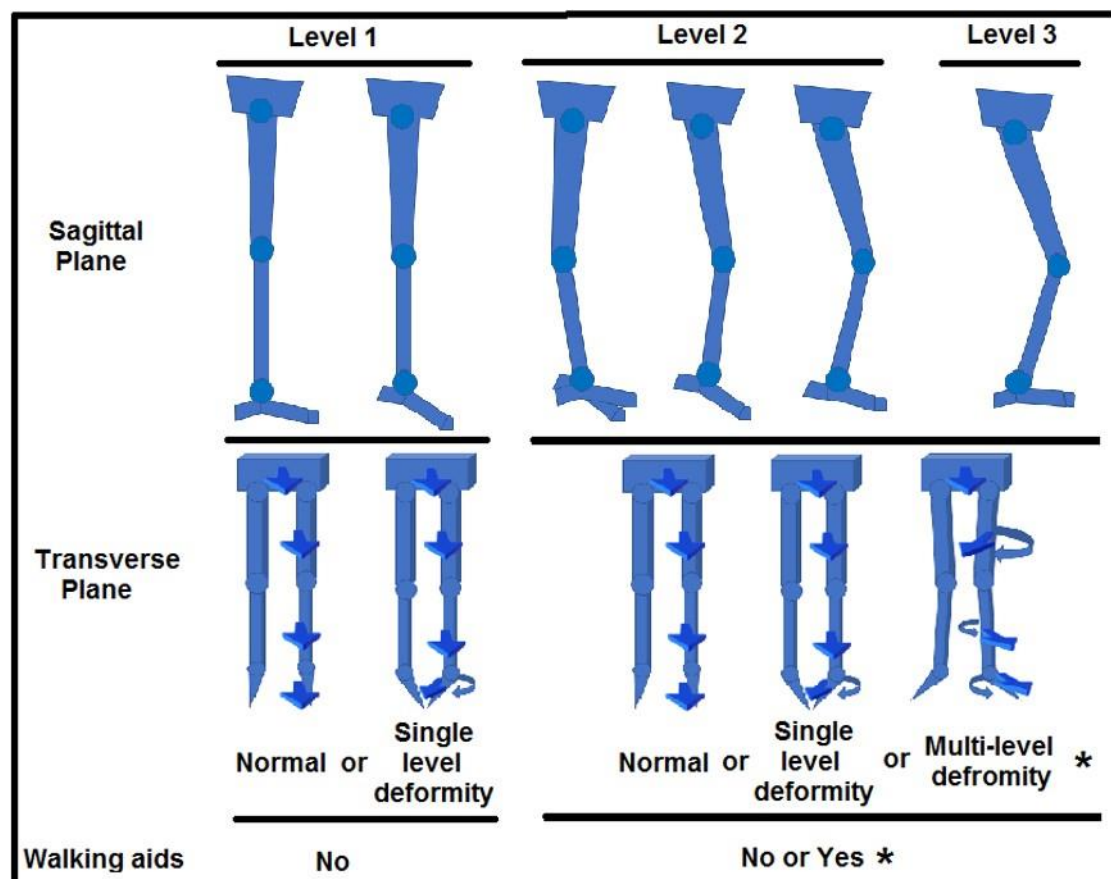


Figure A1. Diagrams showing schematic drawing of the sagittal and transverse plane gait characteristics of the lower limbs, as well as the use of walking aids for each gait level in children with CP.

* Note that a child with sagittal plane characteristics of level 1 becomes level 2 when presenting multi-level deformity in the transverse plane of movement or use walking aids to walk.

Walking aids: canes, crutches or walkers.

Level 1 participants had kinematics in the sagittal plane as typical or minor deviations from normality in the hips and knees and normal or with a trend to plantar flexion in the ankles (Figure A2). In the transverse plane they had normal rotational profile or deformity in just one level (pelvic/hip/knee/foot). The level 1 participants did not use any walking aids.

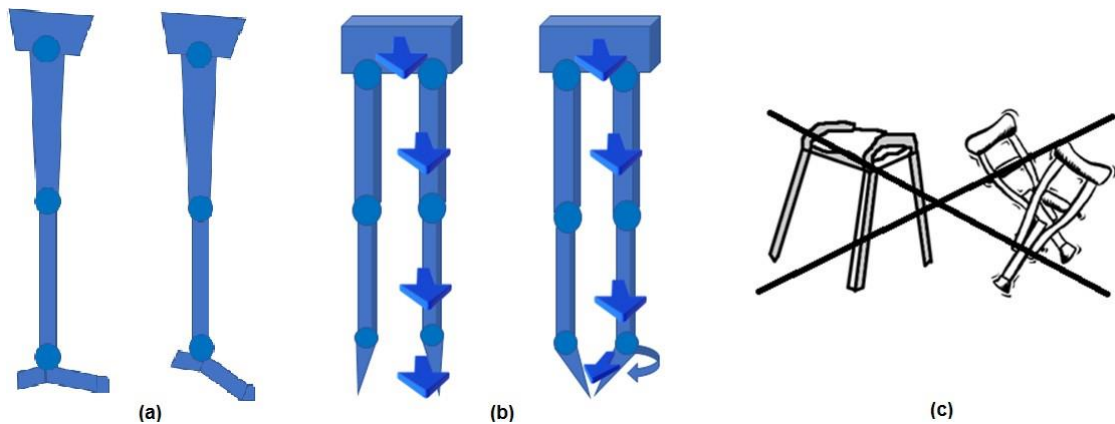


Figure A2. Schematic drawing of the first level of the classification. Sagittal plane (a), transverse plane (b), walking aids (c).

The participants of levels 2 had the kinematics in sagittal plane of motion similar to level 1, when using walking aids. The participants level 2 presented, independently of walking aids or deformities in transverse plane, with knees in flexion or hyperextension and ankle in normal dorsiflexion or plantarflexion (Figure A3).

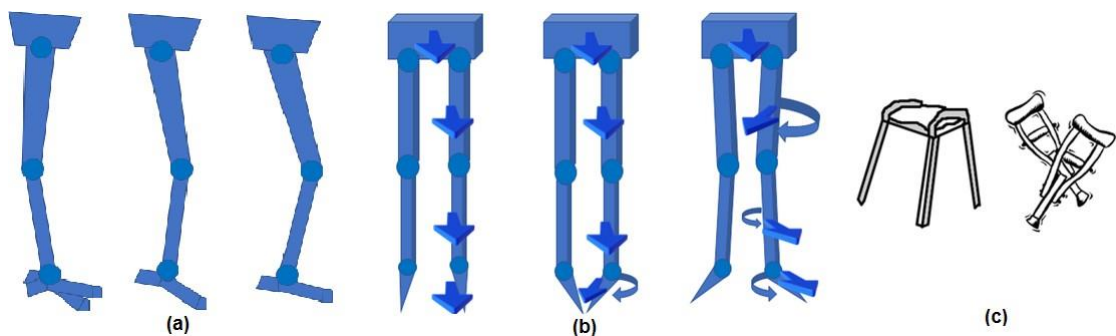


Figure A3. Schematic drawing of the first level of the classification. Sagittal plane (a), transverse plane (b), walking aids (c).

The participants of the level 3 had the kinematics in sagittal plane in triple flexion of the hip, knee and ankle (trend to excessive dorsiflexion). The participants level 3 could use walking aids and have transverse plane deformities in single or multilevel (Figure A4).

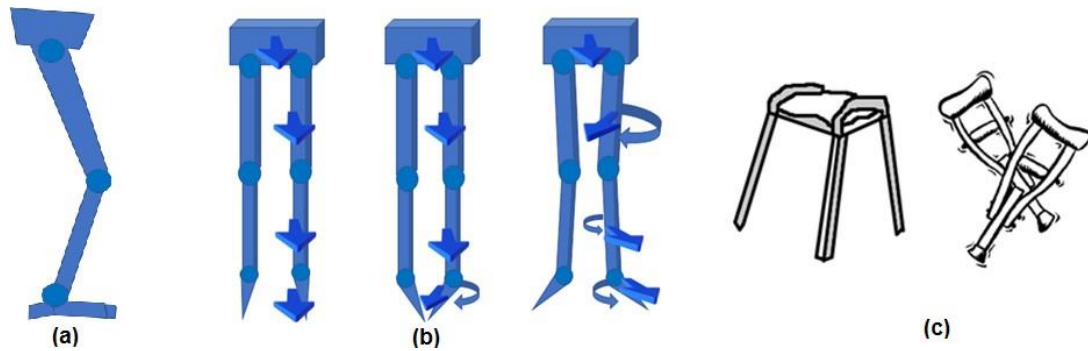


Figure A4. Schematic drawing of the first level of the classification. Sagittal plane (a), transverse plane (b), walking aids (c).

Table A1. Characteristics definition of kinematics and walking aids for levels of gait in CP children.

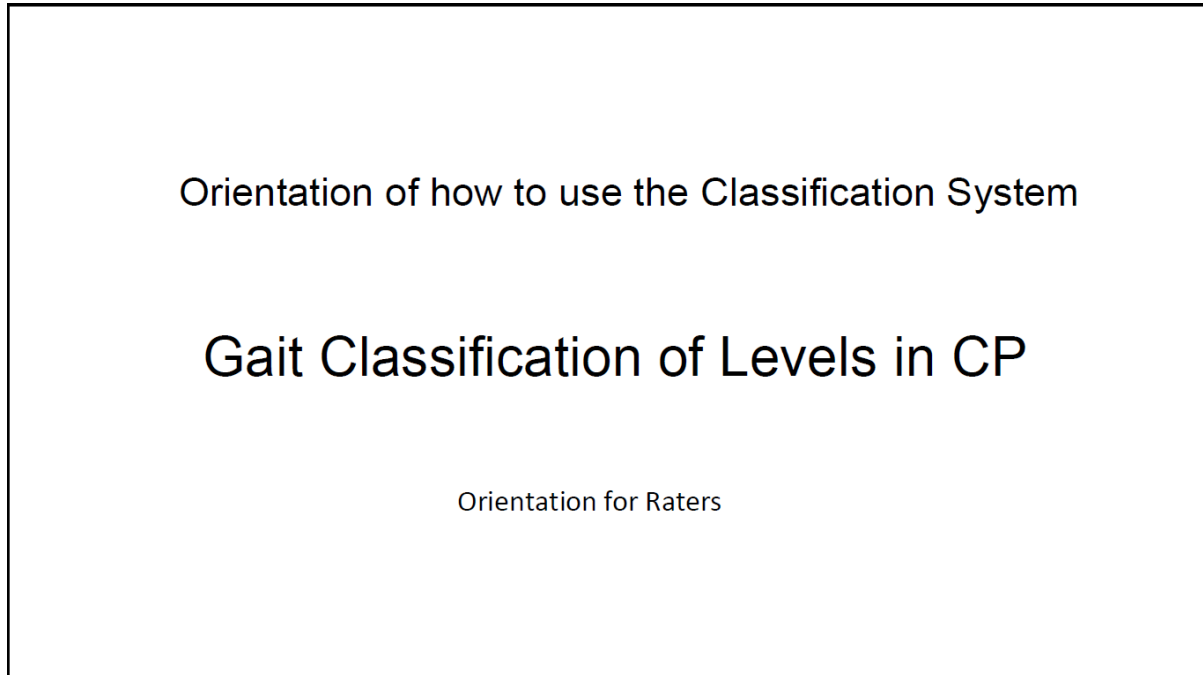
Gait Level	Sagittal plane			Ankle Df/Pf	Transverse plane	Walking aids
	Pelvic tilt	Hip Fx/Ext	Knee Fx/Ext		Rotation profile	canes/ Crutches / walkers
Level 1 n=23	Normal Anterior	Normal or Minor deviations	Normal or Minor deviations	Normal or trend to plantarflex.	Normal or single level	No
* Level 2 n=55	Normal Anterior	Normal or Minor deviations	Minor deviations or hypertext.	Normal or Plantarflex.	Multi- level	and/or Yes
	Normal Anterior Posterior	Flexed	Flexed	Normal or Plantarflex	Normal Single/ multi- level	No or Yes
Level 3 n=23	Anterior Normal Posterior	Flexed	Flexed	Excessive dorsiflex.	Normal Single/ multi- level	No or Yes

Hip Fx/Ext: hip flexion and extension. Knee Fx/Ext: knee flexion and extension. Ankle Df/Pf; ankle dorsiflexion and plantarflexion. Hyperext.: hyperextension. Plantarflex.: plantarflexion. Dorsiflex.: dorsiflexion.

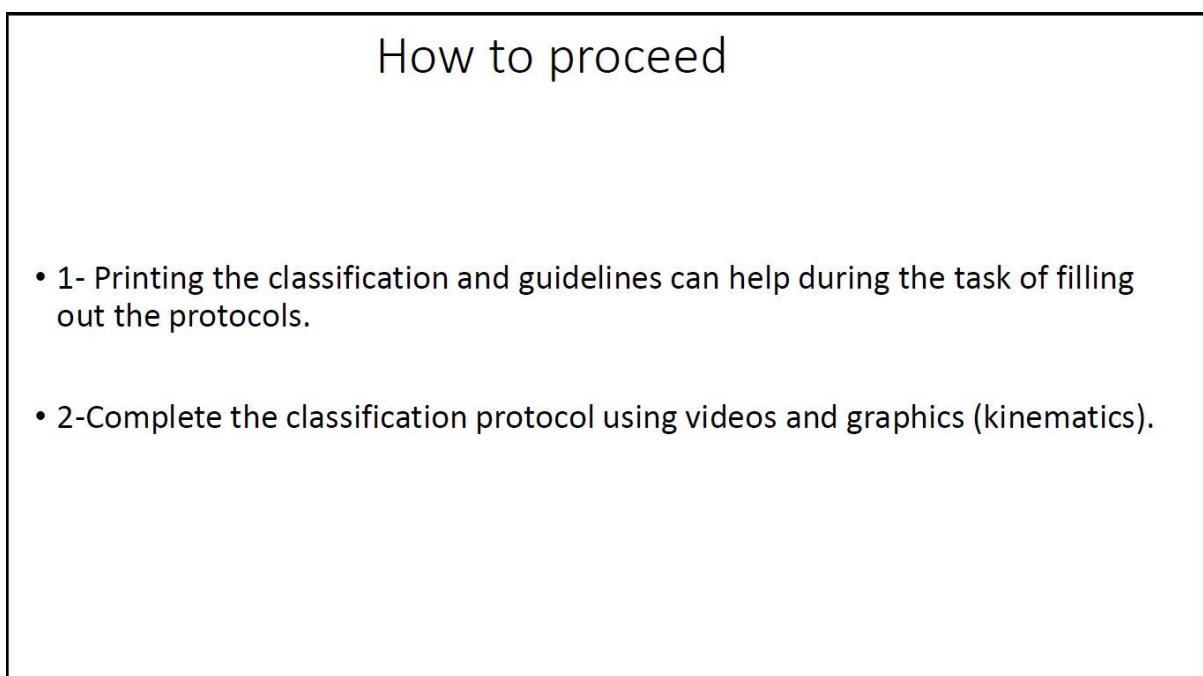
* Note that a child with sagittal plane characteristics of level 1 becomes level 2 when presenting multi-level deformity in the transversal plane of movement or use walking aids to walk.

Walking aids: walking sticks, crutches or walkers.

Appendix B. Orientation of how to use the classification system (PowerPoint presentation).



Slide B1. Orientation of how to use the classification system

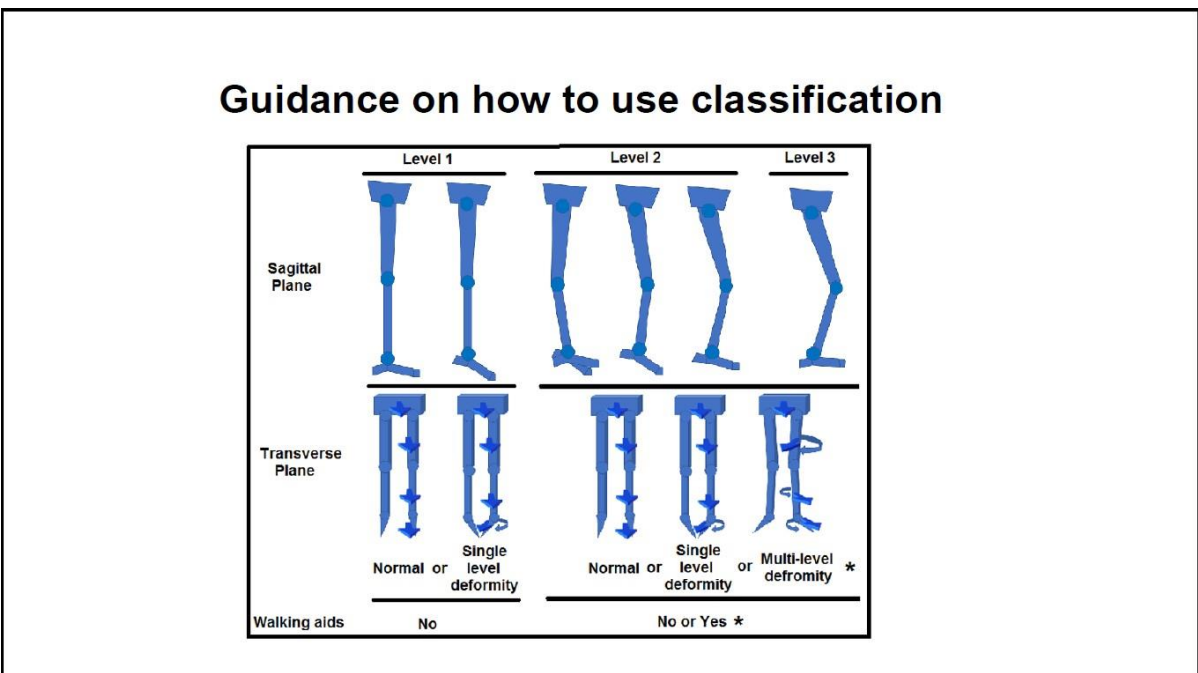


Slide B2 How to proceed to classify the sample of children.

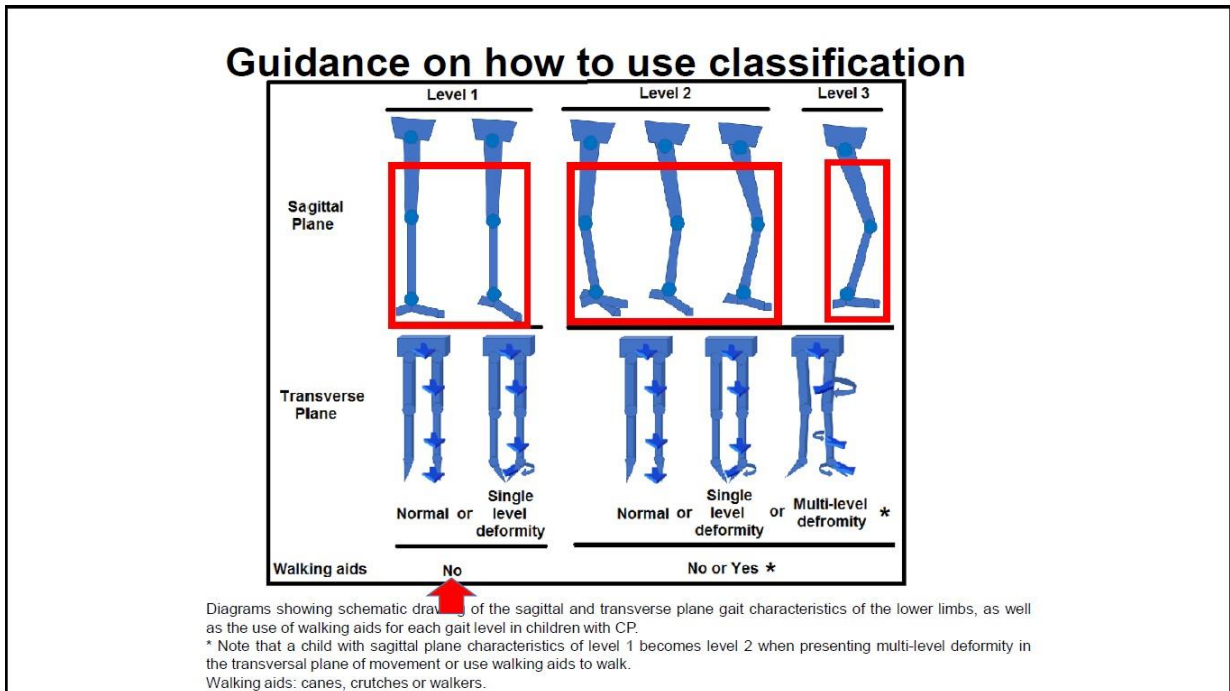
Description of the classification of gait levels in children with CP

Gait Level	Sagittal plane				Transverse plane	Mobility aids
	Pelvic tilt	Hip fx/Ext	Knee Fx/Ext	Ankle Df/Pf	Rotation profile	Crutches/walkers
Level 1 N=23	Normal Anterior	Normal or Minor deviations	Normal or Minor deviations	Normal dorsiflexion or trend to plantarflex.	Normal or single level	NO
Level 2 N=55	Normal Anterior	Normal or Minor deviations	Minor deviations or hypertext.	Normal dorsiflex. or Plantarflex.	Normal Single/multi level	NO or Yes
		Flexed	Flexed			
Level 3 N=23	Anterior Normal Posterior	Flexed	Flexed	Excessive dorsiflexion	Normal Single/multi level	No or Yes

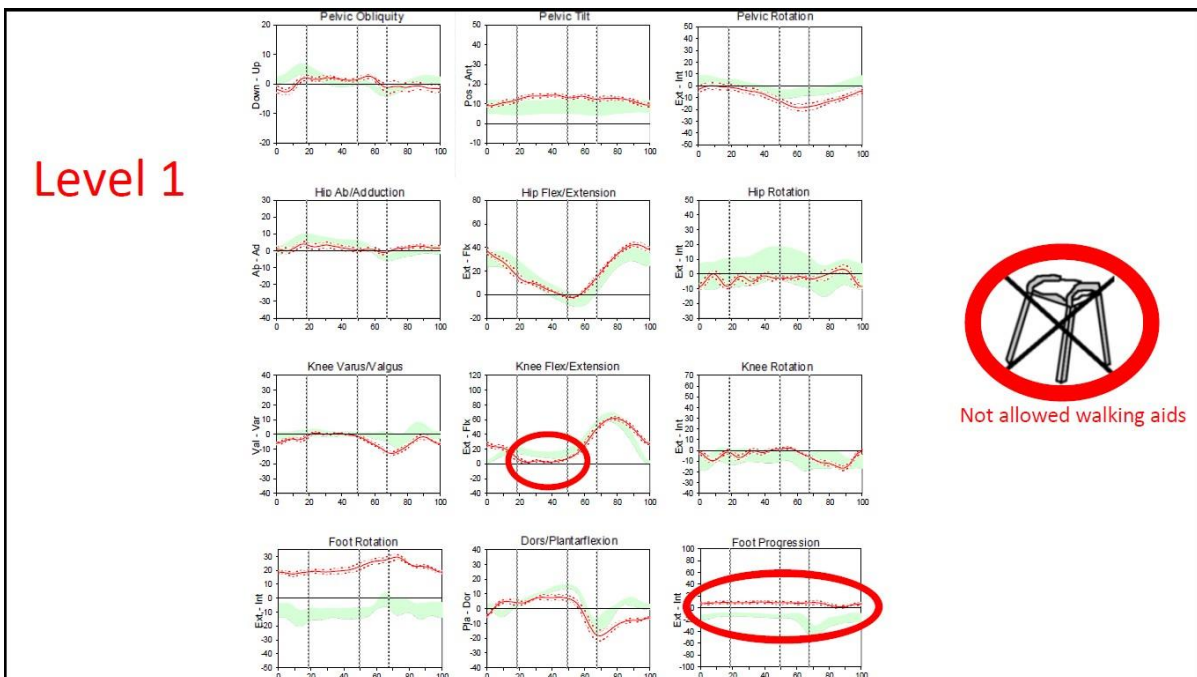
Slide B3. Definitions of the gait patterns.



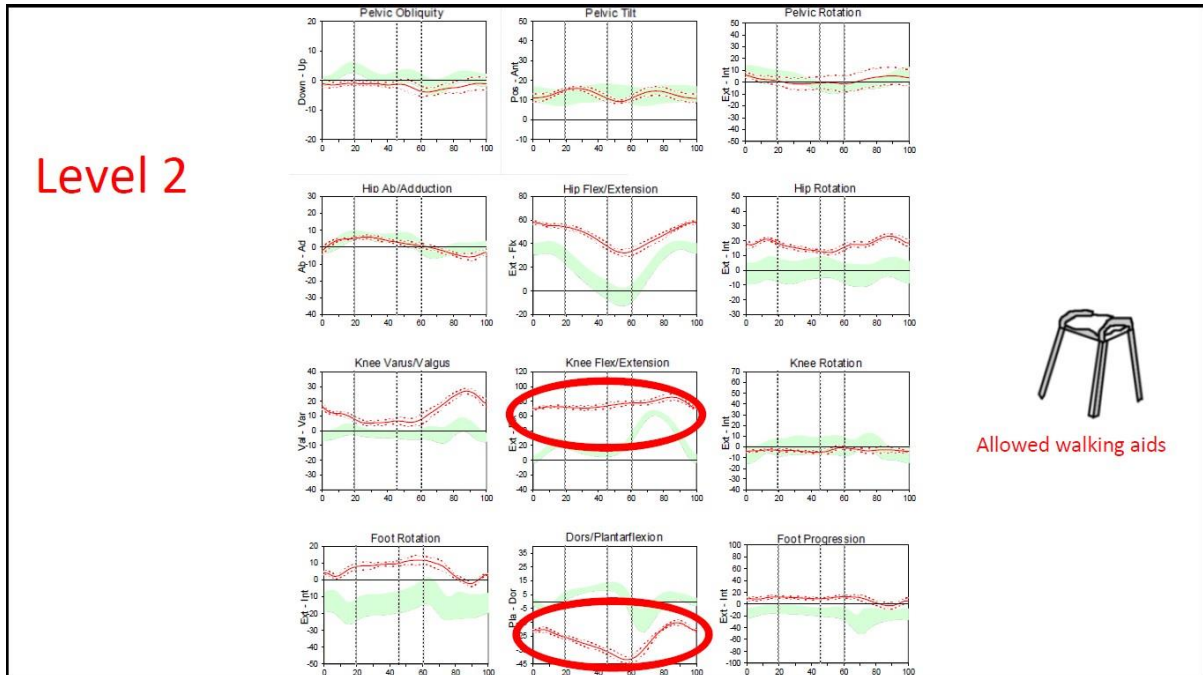
Slide B4. Schematic drawing and explanations of the gait patterns of the classification



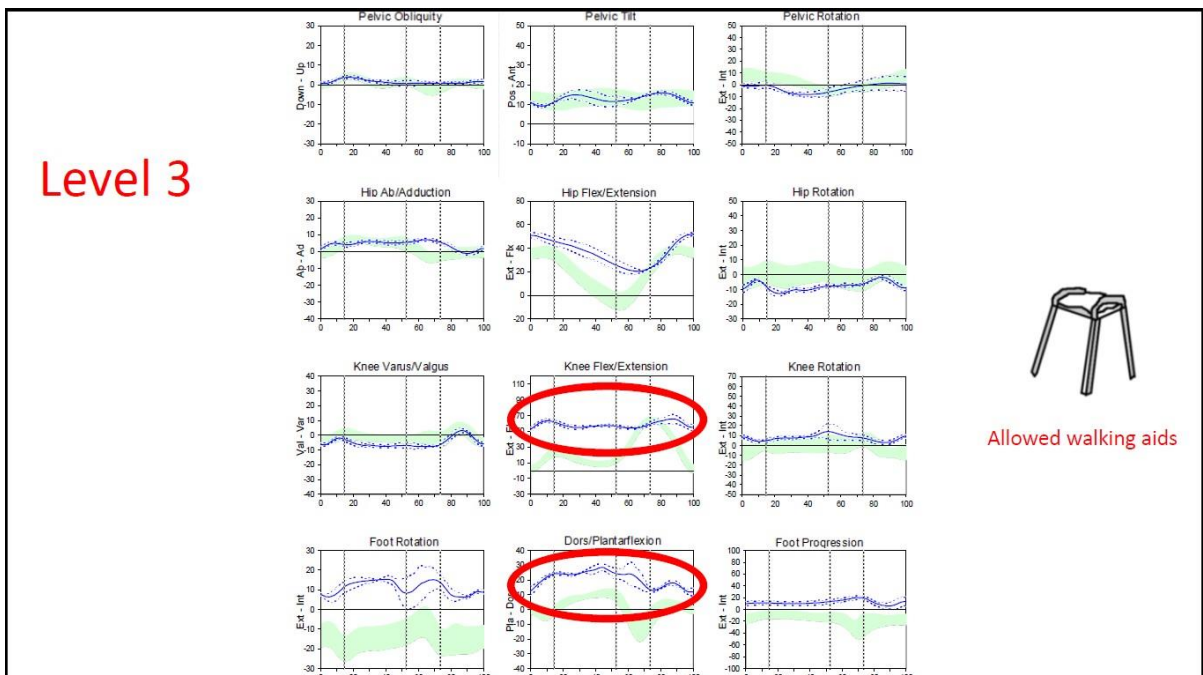
Slide B5. Guidance on how to use classification.



Slide B6. Example of kinematics of the lower limb and use of walking aids in level 1 of the classification



Slide B7. Example of kinematics of the lower limb and use of walking aids in level 2 of the classification



Slide B8. Example of kinematics of the lower limb and use of walking aids in level 3 of the classification

Excel spreadsheet protocol

participant	right side	left side
1		
2		
3		
4		
5		
6		
7		
8		
9		
10		
11		
12		
13		
14		
15		
16		
17		
18		
19		
20		
21		
22		
23		
24		
25		

Use one of the options below to fill the protocol, for both the right and left side of each participant of the study.

Level 1;
Level 2;
Level 3.

	Level 1	Level 2	Level 3
Sagittal Plane			
Transverse Plane			
Walking aids	No	No or Yes *	No or Yes *

Slide B9. Example of excel spreadsheet protocol.

Final Orientation

Finalize the filling of the excel spreadsheet and send to the authors.

Slide B10. Final guidance for evaluators.

8 CONCLUSÃO GERAL DA TESE

A presente tese acrescenta para a literatura atual achados científicos relacionados a marcha de crianças com PC. Foram realizados quatro estudos originais, sendo o primeiro relacionado ao impacto do uso de OSP durante a marcha e os demais relacionados à classificação da marcha nessa população.

O primeiro estudo mostrou que as OSP quando prescritas por profissionais sem o uso de dados da A3DM, não alteraram significativamente o índice da marcha (GPS), mas melhoraram os dados de tempo e espaço, na amostra avaliada. A determinação de parâmetros clínicos quantitativos para a prescrição de órteses em pacientes com PC bilateral, bem como, órteses que atendam aos requisitos específicos são pontos a serem abordados no futuro, a fim de obter efeitos mais significativos.

A tese avaliou duas classificações da marcha na PC, de forma pioneira, em amostras de indivíduos da faixa etária pediátrica. A utilização de ambas as classificações em uma série de casos, com grande número de participantes, possibilitou determinar a capacidade das classificações em avaliar o universo de situações encontradas na marcha de crianças com diagnóstico de PC, e determinar a reprodutibilidade inter e intraobservador dos instrumentos.

Deste modo, o segundo estudo validou a classificação derivada da revisão sistemática da literatura realizada por Papageorgiou *et al.*¹¹⁰. Essa classificação avalia vários níveis articulares e classifica indivíduos com envolvimento unilateral e bilateral.

Apesar dos grupos do sistema de classificação apresentarem sobreposição de características cinemáticas, a reprodutibilidade inter e intraobservador foi substancial e quase perfeita, respectivamente. Uma porcentagem significativa da amostra (>95%), foi classificada utilizando-se esse instrumento. Embora a comparação entre os grupos tenha apresentado algumas diferenças estatisticamente significativas, não foi possível determinar uma tendência evolutiva de maior ou menor comprometimento funcional com a classificação em estudo e os grupos formados. Como limitação, esta classificação só leva em consideração o plano sagital de movimento em sua avaliação.

O terceiro estudo validou e determinou a reprodutibilidade inter e intraobservador do Sistema de Classificação das Alterações da Marcha em Crianças com Paralisia Cerebral (GDCS-CP)¹⁰⁷. Com uso da GDCS-CP, mais de 96% dos casos da amostra avaliada foram classificados. Por avaliar mais de um plano de movimento, ser categorizada de maneira hierárquica e possibilitar ao avaliador um

número maior de opções para a categorização da marcha deste grupo de pacientes, a sua utilidade clínica foi considerada significativa. Entretanto, a reprodutibilidade interobservador foi moderada por conta da significativa sobreposição cinemática dos padrões.

No quarto estudo foi construída uma nova classificação, a partir de elementos de classificações anteriores, para preencher as lacunas observadas. A classificação teve o objetivo de determinar níveis de comprometimento da marcha nas crianças com PC, sem categorizar de maneira estática as alterações. Foi utilizado na construção desta nova classificação o conceito de que a função básica dos membros inferiores durante a marcha é resistir ao colapso em flexão e apresentar extensão eficiente para a produção de potência no final do apoio. A classificação avalia mais de um plano de movimento e incorporou, quando necessário, a utilização de tutores externos durante a marcha (muletas/andadores/bengalas). A reprodutibilidade da classificação foi substancial interobservadores e substancial a quase perfeita intraobservadores. A reprodutibilidade foi quase perfeita, quando calculada entre cada observador e o resultado de um consenso entre os autores da classificação. Quando a reprodutibilidade foi testada com os observadores utilizando a A3DM ou somente análise observacional do vídeo, os resultados foram similares em ambas as situações. Desta forma, a classificação proposta mostrou utilidade na prática clínica diária.

A marcha de pacientes com PC apresenta grande variabilidade e seu estudo continua desafiador. A utilização da A3DM auxiliou, na presente tese, a verificação das alterações do andar possibilitando determinar a aplicabilidade de classificações nesses indivíduos, assim como, na determinação do resultado do uso de OSP.

Além disso, as fragilidades observadas nas classificações existentes, impulsionaram a criação de uma nova classificação da marcha pelos autores deste estudo, lembrando que elas se destinam à: classificar adequadamente a marcha dessa população, servir de guia para a tomada de decisões terapêuticas (cirúrgicas e/ou conservadoras), auxiliar nos estudos de responsividade aos tratamentos propostos e melhorar a comunicação entre a equipe de reabilitação.

Novas pesquisas são incentivadas para melhorar ainda mais a compreensão da marcha e suas classificações em crianças com PC. No futuro, estudos que explorem a relação entre a estrutura cerebral e os padrões observados nas classificações da marcha poderiam prever a evolução clínica e as necessidades de tratamentos desta população.

9 REFERÊNCIAS

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ANEXOS

ANEXO A: Autorização Da Direção Do Centro Hospitalar De Reabilitação Ana Carolina De Moura Xavier – Curitiba – Paraná, Para Utilização Dos Dados Para A Pesquisa.

AUTORIZAÇÃO DE USO DE DADOS

Declaramos para os devidos fins, que cederemos ao pesquisador Alessandro Giurizatto Melanda, CPF 746831799-20, o acesso aos dados de prontuários do Laboratório de Marcha do Centro Hospitalar de Reabilitação Ana Carolina de Moura Xavier – Curitiba – Paraná, para serem utilizados na pesquisa: **Classificação dos Desvios da Marcha de Pacientes com Paralisia Cerebral Utilizando a Análise Tridimensional da Marcha**, que está sob a orientação da Profa. Dra. Suhaila M. Smaili Santos e co-orientado pela Profa Dra. Dirce Shizuko Fujisawa no programa de doutorado em Ciências da Reabilitação na Universidade Estadual de Londrina – Paraná.

Esta autorização está condicionada ao cumprimento do pesquisador aos requisitos da Resolução 466/12 e suas complementares, comprometendo-se o mesmo a utilizar os dados pessoais dos sujeitos da pesquisa, exclusivamente para os fins científicos, mantendo o sigilo e garantindo a não utilização das informações em prejuízo das pessoas e/ou das comunidades.


Antes de iniciar a coleta de dados o pesquisador deverá apresentar o Parecer Consubstanciado devidamente aprovado, emitido por Comitê de Ética em Pesquisa Envolvendo Seres Humanos, credenciado ao Sistema CEP/CONEP.

Marcos Takimura

Nome/assinatura e carimbo do responsável pela Instituição ou pessoa por ele delegada

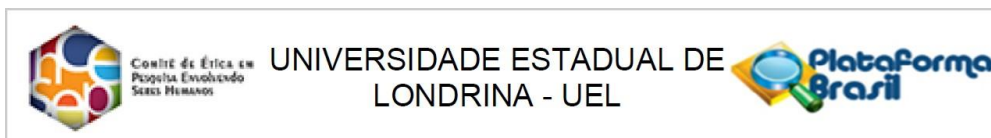
Dr. Marcos Takimura
Genética e Otorrinolaringologia
CRM-PR 13102

MARCOS TAKIMURA
Centro Hospitalar de Reabilitação
Ana Carolina Moura Xavier
DIRETOR TÉCNICO - CRM-PR 13102



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ANEXO B: Parecer Consubstanciado do Comitê de Ética em Pesquisa.



PARECER CONSUBSTANCIADO DO CEP

DADOS DO PROJETO DE PESQUISA

Título da Pesquisa: Classificação dos Desvios da Marcha de Pacientes com Paralisia Cerebral Utilizando a Análise Tridimensional da Marcha

Pesquisador: ALESSANDRO GIURIZATTO MELANDA

Área Temática:

Versão: 2

CAAE: 79599517.9.0000.5231

Instituição Proponente: CCS - Progr. de Pós-Grad. em Ciências da Reabilitação

Patrocinador Principal: Financiamento Próprio

DADOS DO PARECER

Número do Parecer: 2.447.001

Apresentação do Projeto:

Resumo:

Segundo o pesquisador, o projeto sobre classificação da marcha de sujeitos com diagnóstico clínico de paralisia cerebral (PC). Será realizada revisão sistemática da literatura e elaboração de nova classificação dos desvios da marcha deste grupo de sujeitos. Serão pesquisadas eletronicamente bases de dados (Medline, Embase, Lilacs, Cochrane Controlled Trials Database, SciSearch) nas línguas portuguesa e inglesa. As palavras chaves usadas para a estratégia de pesquisas incluirão paralisia cerebral (cerebral palsy), marcha, andar (gait), análise da marcha, análise do andar (gait analysis), classificação (classification), padrão da marcha, padrão do andar (gait pattern). Serão avaliadas a validade externa com determinação do método de amostragem, características dos sujeitos e validade interna com avaliação da construção da classificação e propriedades psicométricas da classificação. Na segunda etapa do projeto será elaborada classificação dos desvios da marcha de pacientes com paralisia cerebral que deverá conter desvios da marcha clinicamente significativos nos 3 planos de movimento (sagital, coronal e transversal) e ser reprodutível. Para construção da classificação serão avaliados os exames tridimensionais da marcha de sujeitos com diagnóstico de paralisia cerebral realizados no Laboratório de Marcha do Centro Hospitalar de Reabilitação Ana Carolina de Moura Xavier de Curitiba Paraná, durante o período de 2010 a 2017. A direção do Centro Hospitalar de Reabilitação Ana Carolina de Moura Xavier (CHR) liberou a utilização dos dados requeridos pelos autores. A revisão sistemática da

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Bairro: Campus Universitário

UF: PR

Município: LONDRINA

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CEP: 86.057-970

E-mail: cep268@uel.br



Continuação do Parecer: 2.447.001

02. Documento de autorização expedido pela Direção do Centro Hospitalar de Reabilitação Ana Carolina de Moura Xavier, em Curitiba.
03. Folha de rosto devidamente preenchida e assinada pela Coordenadora do Programa de Pós Graduação em Ciências da Reabilitação/uel - CCB
04. Termo de sigilo e confidencialidade encaminhado por e-mail para o parecerista, mediante autorização da coordenadora do Comitê.

Recomendações:

Não existem recomendações.

Conclusões ou Pendências e Lista de Inadequações:

O pesquisador atendeu os pedidos encaminhados no primeiro parecer, ou seja, apresentação do termo de sigilo, alteração no cronograma principalmente e apresentação dos gastos com o projeto, no valor total de R\$286,00.

Considerações Finais a critério do CEP:

Não existem pendências.

Este parecer foi elaborado baseado nos documentos abaixo relacionados:

Tipo Documento	Arquivo	Postagem	Autor	Situação
Informações Básicas do Projeto	PB_INFORMAÇÕES_BÁSICAS_DO_PROJETO_1009386.pdf	14/12/2017 10:55:13		Aceito
Projeto Detalhado / Brochura Investigador	brochura.docx	31/10/2017 22:18:54	ALESSANDRO GIURIZATTO MELANDA	Aceito
Declaração de Instituição e Infraestrutura	Liberacao.pdf	31/10/2017 21:59:17	ALESSANDRO GIURIZATTO MELANDA	Aceito
Folha de Rosto	rosto.pdf	31/10/2017 21:54:15	ALESSANDRO GIURIZATTO MELANDA	Aceito

Situação do Parecer:

Aprovado

Necessita Apreciação da CONEP:

Não

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UF: PR	Município: LONDRINA
Telefone: (43)3371-5455	E-mail: cep268@uel.br



Conselho de Ética em
Psicologia Evoluindo
Serres Humanos

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LONDRINA - UEL



Continuação do Parecer: 2.447.001

LONDRINA, 19 de Dezembro de 2017

Assinado por:
Rosana Lopes
(Coordenador)

Endereço: LABESC - Sala 14

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ANEXO C: Normas de formatação do periódico Acta Ortopédica Brasileira Instruções para Autores

O periódico Acta Ortopédica Brasileira, órgão oficial do Departamento de Ortopedia e Traumatologia da Faculdade de Medicina da Universidade de São Paulo (DOT/ FMUSP é publicado bimestralmente em seis edições ao ano (jan/ fev, mar/ abr, maio/ jun, jul/ ago, set/ out e nov/ dez) com versão em inglês. Os títulos, resumos e descritores são publicados em inglês e português. A Acta é distribuída para médicos ortopedistas e principais instituições de ensino e pesquisa do Brasil. A publicação segue integralmente o padrão internacional do International Committee of Medical Journal Editors (ICMJE) ou Convenção de Vancouver e seus requisitos de uniformização [[http:// www. icmje. org/](http://www.icmje.org/)]. Os artigos submetidos são enviados para avaliação por pareceristas (peer review) que recebem o texto de forma anônima (modalidade duplo- cego) e decidem ou não por sua publicação, sugerem modificações, requisitam esclarecimentos aos autores e efetuam recomendações ao Editor- Chefe. Os conceitos e declarações contidos nos trabalhos são de total responsabilidade dos autores. Solicitamos aos autores a atenção às seguintes instruções para publicação.

FORMATAÇÃO DE ARTIGOS

Número de palavras recomendadas por tipo de publicação: Os critérios abaixo especificados devem ser observados para cada tipo de publicação. A contagem eletrônica de palavras deve começar na Introdução e terminar na Conclusão.

PREPARAÇÃO DE MANUSCRITO: A Revista Acta Ortopédica Brasileira recebe para publicação os seguintes tipos de manuscritos: Artigo Original, Artigo de Atualização e Revisão. Os artigos de

Atualização e Revisão, somente serão aceitos a convite do Corpo Editorial.

Os manuscritos enviados deverão estar em arquivos .txt ou .doc, em espaço duplo, com margem larga. Os artigos deverão ser submetidos idealmente em inglês e português. As medidas deverão ser expressas no Sistema Internacional (Système International, SI), disponível em [http:// physics. nist. gov/ cuu/ Units](http://physics.nist.gov/cuu/Units) e unidades padrão quando aplicável. A revista adota o sistema Writecheck de detecção de plágio, porém todo conteúdo publicado nos artigos é de inteira responsabilidade dos autores. Recomenda-se aos autores não usar abreviações no título e limitar a sua utilização no resumo e ao longo do texto. Os nomes genéricos devem ser usados para todas as drogas. Os fármacos podem ser referidos pelo nome comercial, porém, deve constar o nome, cidade e país ou endereço eletrônico do fabricante entre parênteses na seção Materiais e Métodos.

ABREVIATURAS: O uso de abreviaturas deve ser minimizado. As abreviaturas deverão ser definidas por ocasião de sua primeira utilização no resumo e também no texto. Abreviaturas fora do padrão não devem ser utilizadas, a menos que essas apareçam pelo menos três vezes no texto. Unidades de medida (3 ml ou 3 mL, e não 3 mililitros) ou símbolos científicos padrão (elementos químicos, por exemplo, Na, e não sódio) não são consideradas abreviaturas, e portanto, não devem ser definidos. Abreviar nomes longos ou substâncias químicas e termos utilizados para combinações terapêuticas. Abreviaturas em figuras e tabelas podem ser utilizadas por razões de espaço, porém devem ser definidas na legenda, mesmo que tenham sido definidas no texto do artigo.

CARTA DE APRESENTAÇÃO: A carta de apresentação que acompanha a submissão do manuscrito deve ser assinada pelo autor correspondente, contendo as seguintes informações: Título do artigo, Nome (s) de todo (s) autor (es), texto autorizando a publicação do artigo, declarando que o mesmo é inédito (publicação em outro idioma

é considerado como o mesmo artigo) e que não foi, ou está sendo submetido à publicação em outro periódico. Os autores devem se certificar que o manuscrito está inteiramente em conformidade com as instruções.

ENSAIOS CLÍNICOS: O periódico Acta Ortopédica Brasileira apoia a política de Registro de Ensaio Clínicos da Organização Mundial de Saúde (OMS) e do ICMJE, reconhecendo a importância destas iniciativas para o registro e divulgação internacional sobre estudos clínicos em acesso aberto. Desta forma, somente serão aceitos para publicação os artigos envolvendo pesquisas clínicas que tenham recebido um número de identificação em uma das plataformas de registros de ensaios clínicos validados pelos critérios da OMS e ICMJE. Os endereços eletrônicos destas plataformas de registro estão disponíveis na página do ICMJE [<http://www.icmje.org/about-icmje/faqs/clinical-trials-registration/>].

CONFLITO DE INTERESSES: Conforme recomendação do ICMJE e resolução do Conselho Federal de Medicina nº 1595 / 2000 os autores têm a responsabilidade de reconhecer e declarar potenciais conflitos de interesse financeiros e outros (comercial, pessoal, político, etc.) envolvidos no desenvolvimento do trabalho apresentado para publicação.

AGRADECIMENTOS: Os autores podem agradecer o apoio financeiro ao trabalho, na forma de auxílios à pesquisa, bolsas de estudo e outros, bem como profissionais que não qualificam como co-autores do artigo e que contribuíram para o seu desenvolvimento.

CORREÇÃO DE PROVAS GRÁFICAS: Logo que prontas, as provas gráficas em formato eletrônico serão enviadas por e-mail para o autor correspondente. Os autores deverão devolver, também por e-mail, a prova gráfica com as devidas correções em no máximo, 48h após o seu

recebimento. A medida visa agilizar o processo de revisão e publicação do artigo.

DIREITOS AUTORAIS: Todas as declarações publicadas nos artigos são de inteira responsabilidade dos autores. Entretanto, todo material publicado torna-se propriedade da Editora, que passa a reservar os direitos autorais. Portanto, nenhum material publicado na ACTA ORTOPÉDICA BRASILEIRA poderá ser comercializado sem a permissão por escrito da Editora. Todos os autores de artigos submetidos deverão assinar um Termo de Transferência de Direitos Autorais, que entrará em vigor a partir da data de aceite do trabalho.

ORGANIZAÇÃO DO ARQUIVO ELETRÔNICO: Todas as partes do manuscrito devem ser incluídas em um único arquivo. O mesmo deverá ser organizado com a página de rosto, a seguir o texto, referências, figuras (com respectivas legendas) e ao final, as tabelas e quadros (com as respectivas legendas).

PÁGINA DE ROSTO: A página de rosto deve conter:

- a) O tipo do artigo (artigo original, de revisão ou atualização);
- b) O título completo em português e inglês com até 80 caracteres. O título deve ser conciso, porém informativo;
- c) O nome completo de cada autor (sem abreviações); e sua afiliação institucional (as unidades hierárquicas devem ser apresentadas em ordem decrescente, por exemplo, universidade, faculdade/ instituto e departamento. Os nomes das instituições e programas deverão ser apresentados preferencialmente por extenso e na língua original da instituição ou na versão em inglês quando a escrita não é latina (p. ex. árabe, mandarim, grego);
- d) Local onde o trabalho foi desenvolvido;
- e) Nome, endereço completo, telefone e e-mail do autor correspondente.

RESUMO: O resumo em português e inglês deve ser estruturado em caso de artigo original e deve apresentar os objetivos do estudo com clareza, métodos, resultados e as principais conclusões, não devendo ultrapassar 200 palavras (não incluir quaisquer citações de referência). Ademais, o resumo deve incluir o Nível de Evidência, e o tipo de Estudo, conforme tabela de classificação anexada ao final deste texto.

DESCRITORES: O artigo deve incluir no mínimo três e no máximo seis descritores em português e em inglês, baseados nos Descritores de Ciências da Saúde (DeCS) ou no Medical Subject Headings (MeSH) da National Library of Medicine, disponível em

INTRODUÇÃO: A introdução do artigo deve apresentar o assunto e objetivo do estudo, incluindo citações, sem, no entanto, fazer uma revisão extensa da matéria.

MATERIAIS E MÉTODOS: Esta seção deve descrever os experimentos (quantitativa e qualitativamente) e os procedimentos em detalhes suficientes que permitam que outros pesquisadores reproduzam os resultados ou deem continuidade ao estudo.

Ao relatar experimentos com seres humanos ou animais, indicar se os procedimentos seguiram as normas do Comitê Ético sobre Experiências Humanas da instituição na qual a pesquisa foi realizada, e se os procedimentos estão de acordo com a declaração de Helsinki de 1995 e a Animal Experimentation Ethics, respectivamente. Os autores devem incluir uma declaração indicando que o protocolo foi aprovado pelo Comitê de Ética da Instituição (instituição de afiliação de pelo menos um dos autores), com o respectivo número de identificação. Também deve incluir que o Termo de Consentimento Livre e Esclarecido foi assinado por todos os participantes.

Identificar precisamente todas as drogas e substâncias químicas utilizadas, incluindo os nomes genéricos, dosagens e formas de administração. Não citar nomes dos pacientes, iniciais, ou registros de

hospitais. Citar referências para o emprego de procedimentos estatísticos.

RESULTADOS: Apresentar os resultados em sequência lógica no texto, usando tabelas e ilustrações. Não repetir no texto todos os dados constantes das tabelas e ou ilustrações, porém enfatizar ou resumir somente as descobertas mais relevantes.

DISCUSSÃO: Enfatizar aspectos novos e importantes do estudo e as conclusões que decorrem destes no contexto da melhor evidência disponível. Não repetir em detalhes dados ou outras informações mencionadas em outras partes do manuscrito, como na Introdução ou Resultados. Para estudos experimentais, é recomendável iniciar a discussão resumindo brevemente os principais achados, depois explorar os possíveis mecanismos ou explicações para esses achados, comparar e contrastar os resultados com outros estudos relevantes, declarar as limitações do estudo e explorar as implicações destes resultados para pesquisas futuras e para a prática clínica.

Relacionar as conclusões com os objetivos do estudo, mas evitar afirmações e conclusões que não sejam suportadas pelos dados, em particular, a distinção entre relevância clínica e estatística. Evitar fazer afirmações sobre benefícios econômicos e custos, a menos que o manuscrito inclua dados e análises econômicas adequadas. Evitar reivindicação de prioridade (“este é o primeiro estudo sobre...”) ou se referir a trabalho que não tenha sido concluído.

CONCLUSÃO: A conclusão deve ser clara e concisa, estabelecendo uma ligação entre a conclusão e os objetivos do estudo. Evitar conclusões não baseadas nos dados do estudo em questão. Evitar sugerir que estudos com amostras maiores são necessários para confirmar os resultados do trabalho em questão.

AGRADECIMENTOS: Quando aplicável agradecer brevemente as pessoas que tenham colaborado intelectual ou tecnicamente com o

estudo, porém cuja contribuição não justifica coautoria. O autor deve garantir que as pessoas concordem em ter seus nomes e instituições divulgados. O apoio financeiro para a pesquisa e bolsas de estudo devem ser reconhecidos nesta seção (entidade de fomento e número do projeto).

IDENTIFICAÇÃO DOS AUTORES: O número ORCID (Open Researcher and Contributor ID, de cada um dos autores deve ser informado na declaração de contribuição dos autores, conforme modelo abaixo.

DECLARAÇÃO DA CONTRIBUIÇÃO DE AUTORES: A declaração da contribuição dos autores deverá ser incluída ao final do artigo com utilização de dois critérios mínimos de autoria, entre eles:

Contribuição substancial na concepção ou desenho do trabalho, ou aquisição, análise ou interpretação dos dados para o trabalho;

Redação do trabalho ou revisão crítica do seu conteúdo intelectual; Aprovação final da versão do manuscrito a ser publicado;

Estar de acordo em ser responsabilizado por todos os aspectos do trabalho, no sentido de garantir que qualquer questão relacionada à integridade ou exatidão de qualquer de suas partes sejam devidamente investigadas e resolvidas;

a) Participar ativamente da discussão dos resultados; b) Revisão e aprovação da versão final do trabalho.

Todos os artigos deverão incluir a descrição da contribuição dos autores, conforme modelo:

“ Cada autor contribuiu individual e significativamente para o desenvolvimento deste artigo. MJ (0000 - 0000 - 0000 - 0000)*: redação do artigo, revisão e realização das cirurgias; CPV (0000 - 0002 - 3904 - 2836)*: cirurgias, análise dos dados e redação dos artigos; JVC (0000 - 0003 - 3910 - 714 x(0000 - 0000 - 0000 - 0000)*: análise estatística, cirurgias e revisão do artigo; OMA (0000 - 0000 - 0000 - 0000)*: análise das lâminas e revisão do artigo; MASP (0000 - 0000 - 0000 - 0000)*: redação e revisão do artigo e também em todo o conceito intelectual do artigo; ACA

(0000 - 0001 - 6891 - 5935)*: cirurgia, redação do artigo, análise estatística e conceito intelectual do artigo e confecção de todo o projeto de pesquisa. * Número ORCID (Open Researcher and Contributor ID).”

REFERÊNCIAS: Artigos originais podem incluir até cerca de 20 referências, restritas à bibliografia essencial ao conteúdo do artigo. Numerar as referências de forma consecutiva de acordo com a ordem em que forem mencionadas pela primeira vez no texto, utilizando-se números arábicos sobrescritos, no seguinte formato: (p. ex., Redução das funções da placa terminal. 1).

Os autores devem se certificar de que todas as referências são citadas no texto. Várias citações dentro de um único conjunto de parênteses devem ser separadas por vírgulas, sem espaço (1 , 5 , 7) . Onde há 3 ou mais citações sequenciais, utilizar um intervalo numérico (4 - 9) . Incluir os seis primeiros autores seguidos de et al.

Os títulos de periódicos deverão ser abreviados de acordo com o Index Medicus.

a) Artigo: Autor(es). Título do artigo. Título do Periódico. ano; volume: página inicial - final

Ex.: Campbell CJ. The healing of cartilage defects. Clin Orthop Relat Res. 1969; (64) : 45- 63.

b) Livro: Autor(es) ou editor(es). Título do Livro. Edição, se não for a primeira. Tradutor(es), se for o caso. Local de publicação: editora; ano. Ex.: Diener HC, Wilkinson M, editors. Drug- induced headache. 2nd ed. New York: Spriger- Verlag; 1996 .

c) Capítulo de Livro: Autor(es) do capítulo. Título do capítulo Editor (es) do Livro e demais dados sobre este, conforme o item anterior. Ex.: Chapman MW, Olson SA. Open fractures. In: Rockwood CA, Green DP. Fractures in adults. 4 th ed. Philadelphia: Lippincott- Raven; 1996 . p.305-52.

d) Resumo: Autor(es). Título, seguido de [abstract]. Periódico ano; volume (suplemento e seu número, se for o caso): página(s) Ex.:

Enzensberger W, Fisher PA. Metronome in Parkinson's disease [abstract]. Lancet. 1996;34:1337.

e) Comunicações pessoais: só devem ser mencionadas no texto entre parênteses.

f) Tese: Autor, título nível (mestrado, doutorado etc.), cidade: instituição; ano. Ex.: Kaplan SJ. Post-hospital home health care: the elderly's access and utilization [dissertation]. St. Louis: Washington Univ.; 1995.

g) Material eletrônico: Autor(es). Título do artigo. Título do periódico abreviado [suporte]. Data de publicação [data de acesso com a expressão "acesso em"]; volume (número): páginas inicial-final ou [número de páginas aproximado]. Endereço eletrônico com a expressão "Disponível em:"

Exemplo: Pavezi N, Flores D, Perez CB. Proposição de um conjunto de metadados para descrição de arquivos fotográficos considerando a Nobrade e a Sepiades. Transinf. [Internet]. 2009 [acesso em 2010 nov 8];21(3):197-205. Disponível em:

TABELAS: As tabelas devem ser numeradas por ordem de aparecimento no texto com números arábicos. Cada tabela deve ter um título e, se necessário, uma legenda explicativa. Os quadros e tabelas deverão ser enviados através dos arquivos originais editáveis (Word, Excel) e não como imagem. Tabelas e quadros que ocupem mais de uma página devem ser evitados. Não usar elementos de imagem, caixas de texto, ou tabulações.

FIGURAS (FOTOGRAFIAS E ILUSTRAÇÕES): As figuras devem ser apresentadas em páginas separadas e numeradas sequencialmente, em algarismos arábicos, conforme a ordem de aparecimento no texto. Para evitar problemas que comprometam o padrão da revista, o envio do material deve obedecer aos seguintes parâmetros: todas as figuras, fotografias e ilustrações devem ter qualidade gráfica adequada (300 dpi de resolução) e apresentar título e legenda. Em todos os casos, os arquivos devem ter extensão .tif e/ou .jpg. Também são aceitos arquivos

com extensão . xls, . xlsx (Excel), . eps, . psd para ilustrações em curva (gráficos, desenhos e esquemas). As figuras incluem todas as ilustrações, tais como fotografias, desenhos, mapas, gráficos, etc. Figuras em preto e branco serão reproduzidas gratuitamente, mas o editor reserva o direito de estabelecer o limite razoável, quanto ao número delas ou cobrar do autor, a despesa decorrente do excesso. Fotos coloridas serão cobradas do autor.

Por favor, note que é de responsabilidade do autor (s) obter permissão do detentor dos direitos autorais para reproduzir figuras (ou tabelas) que tenham sido previamente publicados em outras fontes. Para todos os valores de acesso aberto, os autores devem ter permissão do detentor dos direitos, caso desejem incluir imagens que tenham sido publicados em outros periódicos de acesso não- aberto. A permissão deve ser indicada na legenda da figura, e a fonte original deve ser incluída na lista de referências.

LEGENDAS: Digitar as legendas usando espaço duplo, acompanhando as respectivas figuras (gráficos, fotos e ilustrações). Cada legenda deve ser numerada em algarismos arábicos, correspondendo a cada figura, e na ordem em que foram citadas no trabalho. Abreviaturas e siglas: Devem ser precedidas do nome completo quando citadas pela primeira vez no texto. No rodapé das figuras e tabelas deve ser discriminado o significado das abreviaturas, símbolos, outros sinais e informada fonte: local onde a pesquisa foi realizada. Se as ilustrações já tiverem sido publicadas, deverão vir acompanhadas de autorização por escrito do autor ou editor, constando a fonte de referência onde foi publicada.

SUBMISSÃO DE ARTIGOS: A partir de janeiro de 2008 a Acta Ortopédica Brasileira adota o Sistema SciELO de Publicação e Submissão online disponível. Os autores deverão seguir as instruções de cadastro e inclusão de artigo no próprio sistema.

Caso ocorra a necessidade de esclarecimentos adicionais, favor entrar em contato com a Atha Comunicação e Editora - Rua: Machado Bittencourt, 190 , 4º andar - Vila Mariana - São Paulo Capital CEP 04044 - 000 - E-mail: - telefone 55 - 11 - 5087 - 9502 com Ana Carolina de Assis/ Arthur T. Assis.

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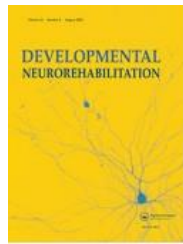
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ANEXO D: Normas de formatação do periódico Developmental Neurorehabilitation.

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Updated 22-04-2020

ANEXO E: Normas de formatação do periódico Journal of the American Academy of Orthopaedic Surgeons (JAAOS).

Instructions for Authors


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The mission of the *Journal of the American Academy of Orthopaedic Surgeons (JAAOS)* is dissemination of knowledge to improve the care of orthopaedic patients.

MANUSCRIPT AND AUTHORSHIP POLICY

- Presubmission approval of a proposal is required for review manuscripts (the Standard Review, Orthopaedic Advances, and Surgical Techniques article types). See page 2. Invited authors and research manuscripts do not need a presubmission proposal.
- JAAOS uses Editorial Manager[®] (www.editorialmanager.com/jaaos) for all proposal and manuscript submissions.
- Note: Please submit your fully written research manuscripts (the research article type) directly to Editorial Manager. A proposal is not required. Case Reports should be submitted to *JAAOS Global Research & Reviews* (<http://www.editorialmanager.com/jaaosglobal/default.aspx>).
- Invited authors: Please log in to the Editorial Manager website, click “My New Invitations” in your author main menu, click “Agree to Submit,” and follow the on-screen directions.

- Video:  You are encouraged to submit video with audio to accompany your manuscript. See tables 1 through 3 below and the section on videos in the Checklists (page 9).
- Authorship: We require that the senior author take an active role in manuscript preparation and development. *Standard Review, Orthopaedic Advances, and Surgical Techniques manuscripts are limited to 4 authors.*
- If a contributor to your manuscript does not meet the criteria for authorship listed below, that author should be credited in an acknowledgment.
- No simultaneous submissions (to more than one publisher) or multi-part articles will be considered.

Authorship policy: Research (the Research Section of the *Journal* and *JAAOS Global Research & Reviews*) and Case Report (*JAAOS Global Research & Reviews*)

(No limit to the number of authors, and authorship restrictions do not apply)

Order of Authors	MD (or equivalent / above, eg, DO, MBBS, PhD)	Resident or in Fellowship Training ^a	Post- Residency Fellow of the AAOS	Other
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First/Lead Author^a 2nd etc., Author Senior Author Corresponding Author^a We do not permit dual first-author status.

Authorship policy: Standard Review, Orthopaedic Advances, and Surgical Techniques (the Review Section of the *Journal*)

(The number of authors is limited to no more than four, and authorship restrictions apply)

Order of Authors	MD (or equivalent / above, eg, DO, MBBS, PhD)	Resident or in Fellowship Training ^a	Post- Residency Fellow of the AAOS	Other
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First/Lead Author ^a 2nd, 3rd, 4th Author Senior Author Corresponding Author ^a We do not permit dual first-author status.

♣ Authors who will complete residency or training fellowship within 6 months following submission may serve as corresponding authors and first authors.

- ♣ No more than one resident can serve as coauthor, and medical students are not allowed as coauthors.
- ♣ No more than two accepted proposals or manuscripts within a 1-year period will be allowed from any author.
- *JAAOS* requires all authors to meet the International Committee of Medical Journal Editors (ICMJE) criteria for authorship: <http://www.icmje.org/icmje-recommendations.pdf>
- The lead author (listed first) may claim 10 *AMA PRA Category 1 Credits* directly from the American Medical Association (AMA) for publishing an article in *JAAOS*. The AMA requires a copy of a page from the published article that shows the name of the author listed first, the name of the journal, and the date published: www.ama-assn.org/education/claim-cme-credit-ama

PRESUBMISSION APPROVAL

Authors of Research manuscripts may submit fully written manuscripts at any time, without an invitation. Prospective authors of Standard Review, Orthopaedic Advances, and Surgical Techniques manuscripts *must* first submit a proposal, which will be reviewed by the *JAAOS* Editorial Board. If your proposal is approved, you will receive an invitation to submit the *blinded* manuscript. Acceptance of your proposal DOES NOT guarantee acceptance of your manuscript. It means only that your manuscript will be reviewed.

Submit all proposals for Standard Review, Orthopaedic Advances, or Surgical Techniques manuscripts to the *JAAOS* Editorial Manager website at www.editorialmanager.com/jaaos by following these steps:

1. Prepare your proposal on the topic using this template.

2. Register in Editorial Manager or log in to your existing author account and click “Submit New Manuscript.”

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MANUSCRIPT SPECIFICATIONS AND COMPONENTS

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- Do not include any identifying information, including author names and affiliations in the body of the text.
- Remove references to funding sources from the body of the text.
- Do not include clinical trial or Institutional Review Board numbers in the body of the text.
- Remove any affiliation related identifier from all figures and tables.

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If you have not received an invitation, select the article type most appropriate for your content.

All manuscript submissions must include a Title Page, uploaded to Editorial Manager as a separate file. The Title Page should not be included in the word count. The title page should include the following information:

- Title of paper including a description of the type of study conducted.
- Full name of each author (first name, middle initial and last name) followed by each author's highest academic degree(s). Name of department(s) and institution(s) with which each author is affiliated and to which work should be attributed.
- Name, address, telephone number, fax number, and E-mail (if available) of author responsible for correspondence concerning the manuscript.
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- Cite all sources of support for the work being reported, including grants, equipment, and drugs.
- A short running head of no more than 40 characters, including spaces, placed at the bottom of the title page.

Manuscripts that do not meet the specifications outlined in Table 1 will be returned to the corresponding author through Editorial Manager for changes.

Table 1: Manuscript Specifications

Article Type	Description	Abstract Word Limit	Text Word Limit ^a	Illustrative Material Limit ^b	Reference Limit	Format
Research Section: Manuscript	Present retrospective or prospective studies that are clinical observational, interventional, or experimental. Format: Introduction, Methods, Results, Discussion	300	4,000	16 panels	40	Keywords (list 5 to 8) Title page ^c Abstract (use structured headings: Introduction, Methods, Results, Discussion, Data Availability and Trial Registration numbers) Text with headings: Introduction, Methods, Results, Discussion References Figures and Figure legends (if

						applicable) Tables (if applicable) Video (if applicable)
Review Section: Standard Review	Present a balanced approach to the current state of knowledge on a topic of interest to the practicing orthopaedic surgeon	200	4,000	16 panels	40 (≥25% from past 5 years)	Keywords Title page ^C Abstract Text (including Introduction and Summary) References Figures Figure legends (if applicable) Tables (if applicable) Video (if applicable)
Review Section: Orthopaedic Advances	Provide current information on recent developments in orthopaedic surgery, technology, pharmacotherapeutics, and diagnostic modalities. Topics are not yet well represented in the literature.	150	2,250	6 panels	20	Keywords Title page ^C Abstract Text References Figures and Figure legends (if applicable) Tables (if applicable) Video (if applicable)

Review Section: Surgical Techniques	Provide step-by-step details of new/innovative surgical procedures or substantial modifications of	150	4,000	8 panels	30	Keywords Title page ^C Abstract Text (Use headings: Introduction, Indications, Contraindications, Pearls, Pitfalls, Summary)
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previously reported techniques. Provide video with audio to demonstrate specific steps.	References Figures and Figure legends (if applicable) Table (if applicable) Video
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^a Excludes abstract, references, and figure legend ^b Add the number of figure and table panels together to get the total. Count each multi-part figure separately, and multiply number of tables by 2 (eg, Figure 1A and 1B = 2 panels; one table = 2 panels; count appendices as tables). Note that a single illustration would not be broken up into multiple panels. ^c Upload as a separate file. The Title Page should not be included in the word count. The title page should contain the following information:

Title of paper including a description of the type of study conducted. Full name of each author (first name, middle initial and last name) followed by each author's highest academic degree(s). Name of department(s) and institution(s) with which each author is affiliated and to which work should be attributed. Name, address, telephone number, fax number, and E-mail (if available) of author responsible for correspondence concerning the manuscript. Name, address, and telephone number of author to who requests for reprints should be addressed, or a statement that reprints will not be available from the author(s). Cite all sources of support for the work being reported, including grants, equipment,

and drugs. A short running head of no more than 40 characters, including spaces, placed at the bottom of the title page.

Table 2: Parts of a Manuscript: Research

Article

Type Abstract Introduction

Figures, Tables, Body, References Videos

<p>Research Section: Manuscript</p>	<p>State essential principles and information</p> <p>Provide facts, conclusions, and outcomes; avoid “we discuss”</p> <p>Be certain data agree with numbers and values in the text</p> <p>Use structured headings:</p>	<p>State hypothesis and purpose of study, setting, population, and primary outcome measure</p> <p>Any clinical study in which patients are randomized into two treatment groups or are followed prospectively to compare two different treatments must have been registered in a public trial registry, eg, www.clinicaltrials.gov (approved registries for clinical trials need to meet all of ICJME guidelines: http://www.icmje.org/recommendations/browse/publishing-and-</p>	<p>Use structured headings: Introduction, Methods, Results, Discussion</p> <p>Include approval for human studies by IRB or animal utilization study committee</p> <p>In the Discussion, note whether hypothesis was validated or refuted, and discuss</p>	<p>Figures</p> <p>Line drawings, radiographs/other imaging scans, photos, algorithms</p> <p>A succinct legend is required for each figure panel</p> <p>Number each figure in order of citation in text</p> <p>Include signed photo consent or remove/blur patient faces, names, institution identifiers, and manufacturer logos</p> <p>Authors must obtain permission</p>
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	Introduction, Methods, Results, Discussion	editorial- issues/clinical-trial- registration.html)	relative significance, strengths, and limitations of your study Limit 40 references Include levels of evidence ^a	to reuse published figures and tables. Digital manipulation must not result in misrepresentation of the original image Preferred image file formats: TIFF, EPS, or MS Office (DOC, PPT, XLS) files. High resolution PDF files are also acceptable. Include a title for each table and a heading for each column If possible, use no more than 6 columns and 10 rows per table. Larger tables will be placed online as supplemental material.
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				Place each table on a separate page in Word or Excel Tables
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Videos

Include as appropriate

Preferred video format: .mp4.

For SDC, video over 10 MB (up to 100MB): .wmv, .swf, .flv, mpg., .mpeg, m4v, .mov, .mp4. For video up to 10 MB.qt and .avi will also be accepted.

^a Level I. Diagnostic study = randomized controlled trial; testing of previously developed diagnostic criteria. Prognostic study = inception cohort study. Therapeutic study = randomized controlled trial. Economic study = computer simulation model. Level II. Diagnostic study = prospective cohort study; development of diagnostic criteria. Prognostic study = prospective cohort study; control arm of randomized trial. Therapeutic study = prospective cohort study; observational study with dramatic effect. Economic study = computer simulation model. Level III. Diagnostic study = retrospective cohort study; case-control study; nonconsecutive patients; no consistently applied reference standard. Prognostic study = retrospective cohort study; case-control study. Therapeutic study = retrospective cohort study; case-control study. Economic study = computer simulation model. Level IV. Diagnostic study = case series; poor or nonindependent reference standard. Prognostic study = case series. Therapeutic study = case series; historically controlled study. Economic study = decision tree over the short time horizon with input data from original level II and III studies and uncertainty examined by univariate sensitivity analyses. Level V. Diagnostic, prognostic, and therapeutic studies = mechanism-based reasoning. Economic study = decision tree over the short time horizon with input data informed by

prior economic evaluation and uncertainty examined by univariate sensitivity analyses.

Table 3: Parts of a Manuscript: Standard Review, Orthopaedic Advances, Surgical Techniques

Article

Type Abstract Introduction

Body, References Figures, Tables, Videos

<p>Review Section: Standard Review</p>	<p>Reflect essential principles and information</p> <p>Provide facts, conclusions, and outcomes; avoid “we discuss”</p> <p>Be certain data agree with numbers and values in the text</p>	<p>Present brief overview, background information, statistics, and history</p> <p>Include rationale for importance, main points, information deficiencies, and/or differences of opinion</p>	<p>Review pertinent literature</p> <p>Use section headings (eg, Indications, Contraindications)</p> <p>Include, as applicable: controversy, treatment methods, basic science, authors’ preferred treatment, complications</p> <p>Use generic names for drugs and devices</p> <p>Include <i>P</i> values and correlation coefficients</p>	<p>Figures</p> <p>Line drawings, radiographs/ other imaging scans, photos, algorithms</p> <p>A succinct legend is required for each figure panel</p> <p>Number each figure in order of citation in text</p> <p>Include signed photo consent or remove/blur patient faces, institution identifiers, and manufacturer logos</p> <p>Authors must obtain permission to reuse</p>
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			<p>Reiterate nature of problem, provide clear conclusion based on literature and author experience, suggest role for ongoing study and future directions</p> <p>Limit 40 references ($\geq 25\%$ published within past 5 years)</p> <p>Include levels of evidence^a</p>	<p>published figures and tables.</p> <p>Digital manipulation must not result in misrepresentation of the original image</p> <p>Preferred image file</p> <p>TIFF, EPS, or MS Office (DOC, PPT, XLS) files. High-resolution PDF files are also acceptable.</p> <p>Tables</p> <p>Include a title for each table and a heading for each column</p> <p>Use no more than 6 columns and 10 rows per table</p> <p>Place each table on a separate page in Word</p> <p>formats:</p> <p>or Excel</p> <p>Videos</p>
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				<p>Include as appropriate</p> <p>Preferred video format: .mp4 For SDC video over 10 MB (up to 100MB): .wmv, .swf, .flv, mpg., .mpeg, .m4v, .mov, .mp4. For video up to 10 MB, .qt and .avi will also be accepted.</p>
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<p>Review Section: Orthopaedic Advances</p>	<p>See above</p>	<p>Present objective appraisals of recent or controversial techniques and new developments in orthopaedic surgery</p> <p>Address current trends or advances of brief clinical experience and few documented studies</p>	<p>See above</p> <p>Limit 20 references</p> <p>Include levels of evidence^a</p>	<p>See above</p>
<p>Review Section:</p>	<p>None</p>	<p>Present brief overview, background</p>	<p>Use headings: Introduction, Indications, Contraindications, Surgical</p>	<p>See above</p>

Surgical Techniques		information, statistics, and history Include rationale for importance, main points, information deficiencies, and/or differences of opinion, surgical technique	Technique, Pearls and Pitfalls, Outcomes In the Surgical Technique section, use subheads Setup, Exposure/Approach, Technique, Closure, Postoperative Care/Considerations Discuss anatomic and biomechanical considerations Provide pearls and pitfalls in two bulleted lists Limit 30 references Include levels of evidence ^a	Video is strongly recommended Describe indications and contraindications of technique No more than 5 to 10 minutes Audio narration is required Include title screen without identifying author, patient, or institution Adhere to safety precautions and FDA guidelines for off-label use
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^a Level I. Diagnostic study = randomized controlled trial; testing of previously developed diagnostic criteria. Prognostic study = inception cohort study. Therapeutic study = randomized controlled trial. Economic study = computer simulation model. Level II. Diagnostic study = prospective cohort study; development of diagnostic criteria. Prognostic study = prospective cohort study; control arm of randomized trial. Therapeutic study = prospective cohort study; observational study with dramatic effect. Economic study = computer simulation model. Level III. Diagnostic study = retrospective cohort study; case-control study; nonconsecutive patients; no consistently applied reference standard. Prognostic study = retrospective cohort study; case-control study. Therapeutic study = retrospective cohort study; case-control study. Economic study = computer simulation model. Level IV. Diagnostic study = case

series; poor or nonindependent reference standard. Prognostic study = case series. Therapeutic study = case series; historically controlled study. Economic study = decision tree over the short time horizon with input data from original level II and III studies and uncertainty examined by univariate sensitivity analyses. Level V. Diagnostic, prognostic, and therapeutic studies = mechanism- based reasoning. Economic study = decision tree over the short time horizon with input data informed by prior economic evaluation and uncertainty examined by univariate sensitivity analyses.

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2. From your Author Main Menu, click “My Accepted Invitations” and “Submit Invited Manuscript.” Proceed through the remaining screens, attaching your text/references/figure legends, figures, tables, videos, and author forms as separate files. All figures must be submitted as image files. Please do not embed figures in the body of your text or in a separate Word document.
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3. From the Article Type drop-down menu, select “Research Section: Manuscript” and proceed through the remaining screens.

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POLICIES AND GUIDELINES

Authors must read the Academy's guidelines and policies on:

AAOS Clinical Practice Guidelines AAOS Appropriate Use Criteria

Table 4: Intellectual Property, Public Funding, and JAAOS Article Citation Topic Description

<p>Duplicative publishing and copyright</p>	<p>Text</p> <p>JAAOS uses iThenticate® to detect matching text across published works. If the similarity percentage of your manuscript is excessive, it will be returned to you.</p> <p>Images and Tables</p> <p>Provide complete bibliographic information for any previously published material you are submitting. Authors are responsible for obtaining permission to use previously published material. Be aware that images contained in a “free use” database may be copyrighted.</p> <p>When your material is published in JAAOS, it becomes the copyrighted property of the AAOS. You may still use this material for certain purposes. Please see the Rights and Permissions link on the online version of your article for more information.</p>
<p>Intellectual property</p>	<p>Prior to submitting your paper, see copyright resources from the U.S. Copyright Office here: https://www.copyright.gov/learning-engine/</p> <p>The AAOS is currently updating a comprehensive Intellectual Property Primer with Intellectual Property Learning Modules. Links will be added here as soon as these become available.</p>

Funding from public entities	<p>NIH</p> <p>The corresponding author of a study prepared with funding from the National Institutes of Health is responsible for submitting the final peer-reviewed manuscript to the digital archive PubMed Central upon acceptance for publication.</p> <p>Such manuscripts are to be made accessible to the public on PubMed Central no more than 12 months after publication.</p>
JAAOS article citation	<p>To cite an article that you have published in <i>JAAOS</i>, use the format below:</p> <p>Last name + initials: Title. <i>J Am Acad Orthop Surg</i> Year;Volume(Issue):starting page no. - ending page no.</p>

Figures

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Figures must meet the professional standards of the journal (ie, sufficient resolution and appropriate file format).

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Line art must be vector or have a resolution of at least 1200 dpi (dots per inch), and electronic photographs- radiographs, CT scans, and so on- and scanned images must have a resolution of at least 300 dpi. Photographs containing text must have a resolution of at least 600 dpi. If fonts are used in the artwork, they must be converted to paths or outlines or they must be embedded in the files. Cite figures consecutively on the site, and number them in the order in which they are discussed.

For additional assistance, please refer to the journal's Creating Digital Artwork file. Each figure should be uploaded into Editorial Manager as a separate item, one file per figure. Do not embed

figures in the manuscript. Color figures are encouraged and are published at no charge to the author.

A Figure Legend should be included in the manuscript, beginning on a new page after the References. Cover the following in the figure legend:

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If a figure contains a human subject that is identifiable, written consent from the patient or guardian must accompany the submission.

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Lettering should be the same font throughout all figures in the manuscript in the sans-serif typeface Helvetica, Medium, 8pt, sharp. Units, capitalization, etc, should follow *JAAOS* style (see www.jaaos.org) and refer to issues of the *Journal* published in 2015 through 2017. Arrows, arrowheads, and other symbols should be black or white, depending which is most visible against the image in question and sized to be visible but not to obscure or overwhelm the image. Leaders and rules should be 2.25 px.

Avoid headings on the figure. Heading information should appear in the figure legend. Label units of measure consistently with the text and legend. Follow the *AMA Manual of Style* for unit abbreviations.

For multi-panel figures, submit each part individually (eg, Figure 1A, Figure 1B, Figure 1C, Figure 1D), rather than as one block (eg, Figure 1ABCD). Similar panels should be consistent in size and uniformly set.

Supply a scale bar with photomicrographs.

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Algorithms

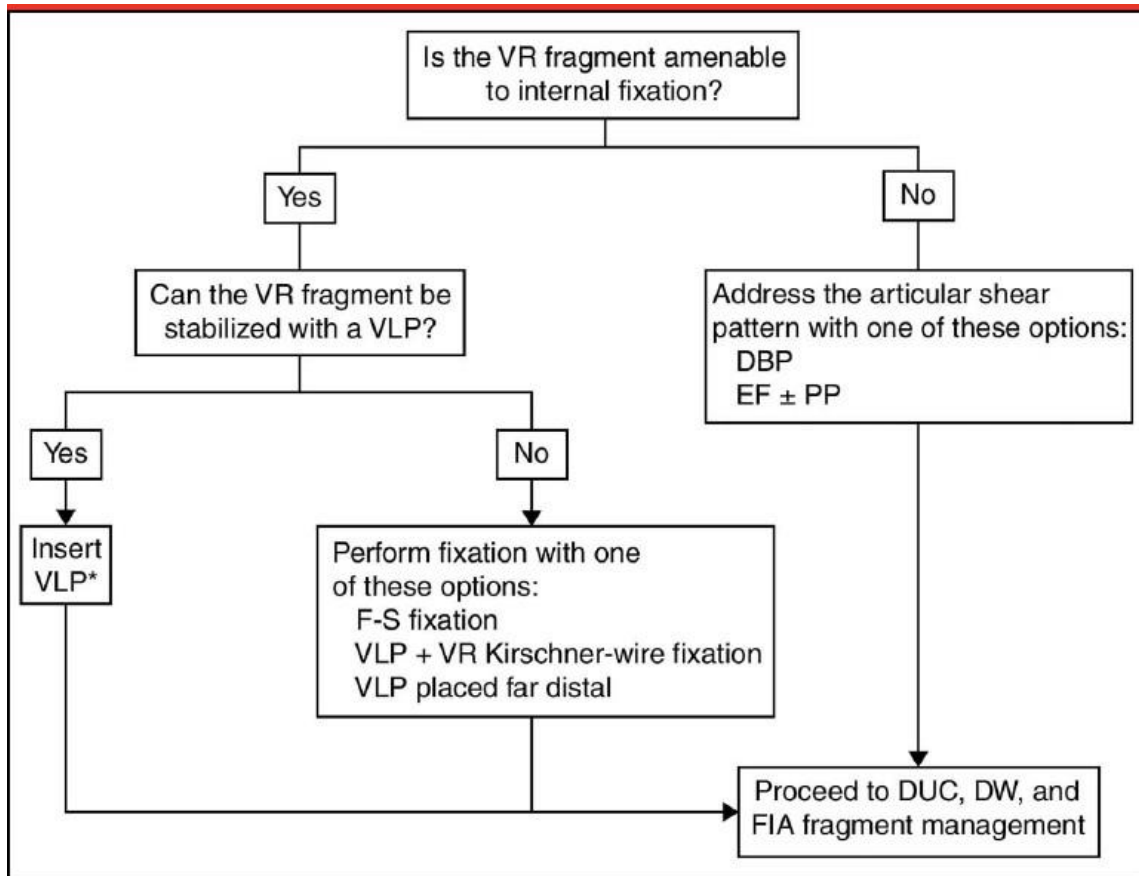
The flow should be logical and complete. Text is centered in boxes with one idea or point. Hanging indents are used for boxes with more than one idea or option (eg, treatment option).

Label leaders and algorithm leaders (rules) to boxes should be 10 px when the document DPI is 1200. Arrowheads are inserted only when a rule leads to a box with an action, such as a surgical procedure. Arrowheads for algorithm rules are to be created with 800% width, 650% length at 10 px. If a need arises to have an "algorithm box" in an image at 300 DPI the box should be created with a 3 px contraction in Photoshop. Label leaders (rules) should be 2.25 at 300 DPI.

Example: Figure 5 from Rhee PC, Medoff RJ, Shin AY: Complex distal radius fractures: An anatomic algorithm for surgical management. *J Am Acad Orthop Surg* 2017;25(2):77-88.

https://journals.lww.com/jaaos/Fulltext/2017/02000/Complex_Distal_Radius_Fractures___An_Anatomic.1.aspx

1. Data should neither be added to, nor removed from, an image by digital manipulation. Images gathered at different times or from different locations should not be combined into a single image, unless it is stated that the resultant image is a product of time-averaged data or a time-lapse sequence. Figures assembled from multiple images must indicate the separation of the parts by lines and described in the legend.
2. The use of touch-up tools, such as cloning and healing tools in Photoshop, or any feature that deliberately obscures manipulations, is unacceptable.



Algorithm depicting the management of a volar rim (VR) fragment. The asterisk (*) indicates insertion of distal locking screws through the volar locking plate (VLP) into the intermediate column only (not the radial column). DBP = distraction bridge plate, DUC = dorsal ulnar corner, DW = dorsal wall, EF ± PP = external fixation with or without percutaneous pins, FIA = free intra-articular, F-S = fragment-specific

The use of digital media for image acquisition and processing introduces the potential for inadvertent distortion of data. To prevent such distortion, the following guiding principles should be used:

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4. When submitting revised final figures upon conditional acceptance, authors may be asked to submit original, unprocessed images.

5. All image acquisition tools and image processing software packages used should be listed. Deviations from the above, including nonlinear adjustments, must be indicated in the figure legend along with a description of the processing software used.

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Footnotes: Place explanatory matter in footnotes rather than in the table title or column heading. Please define all abbreviations used in the table in the footnotes. If italics are used, specify the meaning of the italics in the footnotes.

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Book Chapter Reference Example

Henry MH: Hand fractures and dislocations, in Court-Brown CM, Heckman JD, McQueen MM, Ricci WM, Tornetta III P, McKee M, eds: *Rockwood and Green's Fractures in Adults*, ed 8. Philadelphia, PA, Wolters Kluwer Health/Lippincott Williams & Wilkins, 2014, vol 1, pp 915-990.

Online Resource Reference Example

The American Board of Surgery: ABS to require ACLS, ATLS and FLS for general surgery certification.

https://www.absurgery.org/default.jsp?news_newreqs. Accessed April 7, 2016.

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- From the Article Type drop-down, select “Review Section: Letter to the Editor” (for review articles) or “Research Section: Letter to the Editor” (for research articles) and proceed through the remaining screens.

TIPS FOR SEARCH ENGINE OPTIMIZATION

Search engine optimization (SEO) is the process of affecting the visibility of a website or web page on a search engine’s results page. Authors can play a decisive role in optimizing search results to make their articles more discoverable online.

Below are some useful writing tips to ensure that your article is visible and high-ranking in the search results of Google and other engines.

1. Make the title of your article SEO-friendly

The title of your article should be descriptive of its content and include keywords. Because only the first 65 characters (including spaces) are shown in Google search results, it is important to put your keywords within the first 65 characters of the title.

2. Use headings

Headings help readers as well as search engines like Google to better understand the structure and organization of your article. Be sure to include keywords and phrases in section headings where appropriate.

3. Choose good keywords

Appropriate keywords will help improve the visibility of your article via search engines. Keywords should accurately reflect the content of the paper. In crafting good keywords, think about your audience. Which words or phrases might a reader use to find the information in your article online using a search engine? You might also consider using sites such as Google Trends or Google Adwords to find out which search terms are most popular.

4. Optimize the abstract

In most cases, only the abstract of the paper will be “visible” to search engines. It is therefore important that the abstract accurately reflect the content of the entire paper by incorporating appropriate keywords and phrases throughout in a natural, contextual way.

5. Stay consistent in your language

In writing your paper, be sure to use terms and keywords in a consistent manner. Wherever possible, try to refer to these key terms in the same way they’ve been referred to in past online publications.

6. Cite previous publications

When appropriate, cite your own or your co-authors’ previous publications. Such citations will factor into how search engines will rank your current and future work.

7. Promote your article through social media

Another important way to ensure that your article is visible and discoverable online is to promote it through academic and social networking sites. Google and other search engines regard links as “votes” for web pages. Therefore, by creating inbound and

outbound links to your article, you can help improve the ranking of your article in the search results. Recommended academic and social networking platforms include:

- LinkedIn, •Facebook, •Twitter, • Mendeley, If you are interested in promoting your article via Twitter or Facebook, you will have the opportunity to enter your Twitter handle and/or your Facebook username when you complete the author questionnaire during the submission process.

ANEXO F: Normas de formatação do periódico Gait and Posture.

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GAIT & POSTURE

Official Journal of: Gait and Clinical Movement Analysis Society (GCMAS), European Society of Movement Analysis in Adults and Children (ESMAC), Società Italiana di Analisi del Movimento in Clinica (SIAMOC), and the International Society for Posture and Gait Research (ISPGR)

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- Guide for Authors

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ISSN: 0966-6362

DESCRIPTION

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Gait & Posture is a vehicle for the publication of up-to-date basic and clinical research on all aspects of locomotion and balance. The topics covered include: Techniques for the measurement of gait and posture, and the standardization of results presentation; Studies of normal and pathological gait; Treatment of gait and postural abnormalities; Biomechanical and theoretical approaches to gait and posture; Mathematical models of joint and muscle mechanics; Neurological and musculoskeletal function in gait and

posture; The evolution of upright posture and bipedal locomotion; Adaptations of carrying loads, walking on uneven surfaces, climbing stairs etc; spinal biomechanics only if they are directly related to gait and/or posture and are of general interest to our readers; The effect of aging and development on gait and posture; Psychological and cultural aspects of gait; Patient education.

Index bound in last issue of year.

For details of the GCMAS, ESMAC, SIAMOC, ISPGR please visit their web sites through these links.

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IMPACT FACTOR

2018: 2.414 © Clarivate Analytics Journal Citation Reports 2019

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ABSTRACTING AND INDEXING

OT Bibsys (The Reliable SOURCE)

PubMed/Medline

Embase

Current Contents - Clinical Medicine

Journal of Rehabilitation Research and Development

Scopus

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GUIDE FOR AUTHORS.

JOURNAL DESCRIPTION

Gait and Posture publishes new and innovative basic and clinical research on all aspects of human movement, locomotion and balance.

The topics covered include: Techniques for the measurement of gait and posture, and the standardization of results presentation; Studies of normal and pathological gait; Treatment of gait and postural abnormalities; Biomechanical and theoretical approaches to gait and posture; Mathematical models of joint and muscle mechanics; Neurological and musculoskeletal function in gait and posture; The evolution of upright posture and bipedal locomotion; Adaptations of carrying loads, walking on uneven surfaces, climbing stairs, running and performing other movements. Spinal biomechanics only if they are directly related to gait and/or posture and are of general interest to our readers; The effect of aging and development on gait and posture; Psychological and cultural aspects of gait; Patient education.

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